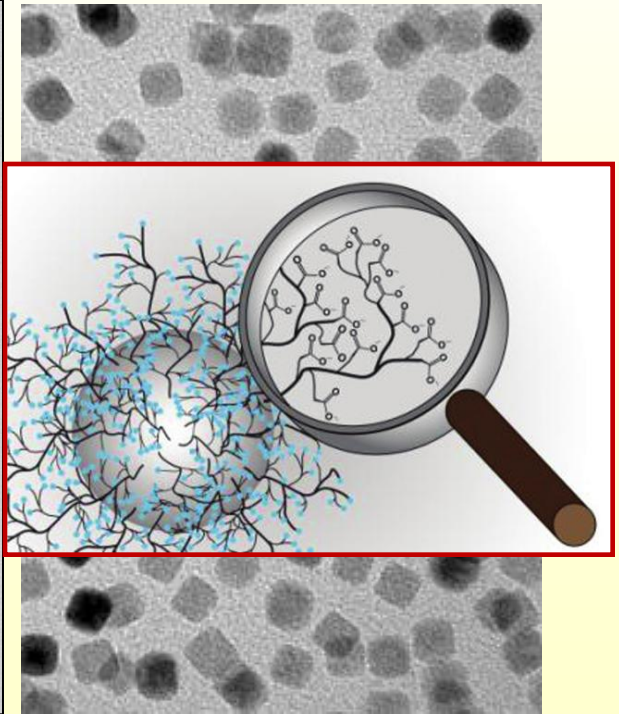
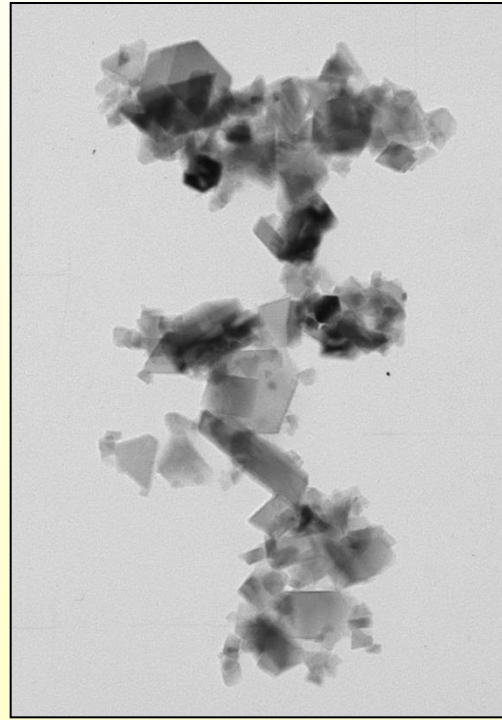
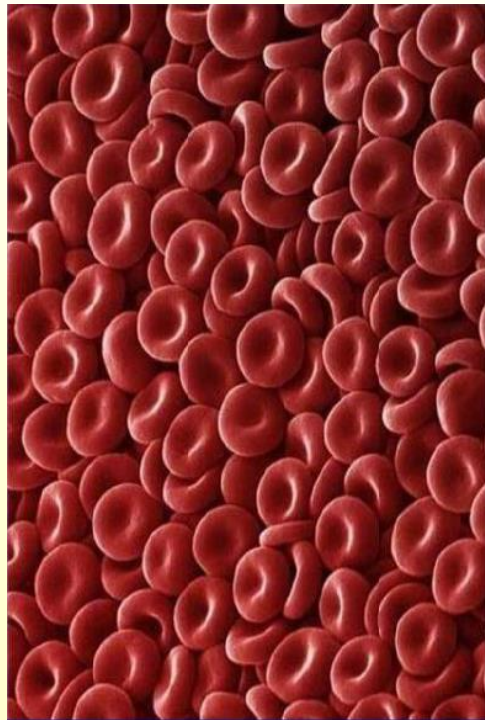


Preparation and Biomedical Applications of Magnetic Nanoparticles

Dra. M^a del Puerto Morales Herrero

Departamento de Biomateriales y Materiales Bioinspirados
Instituto de Ciencia de Materiales de Madrid, CSIC

<http://www.icmm.csic.es/csc>



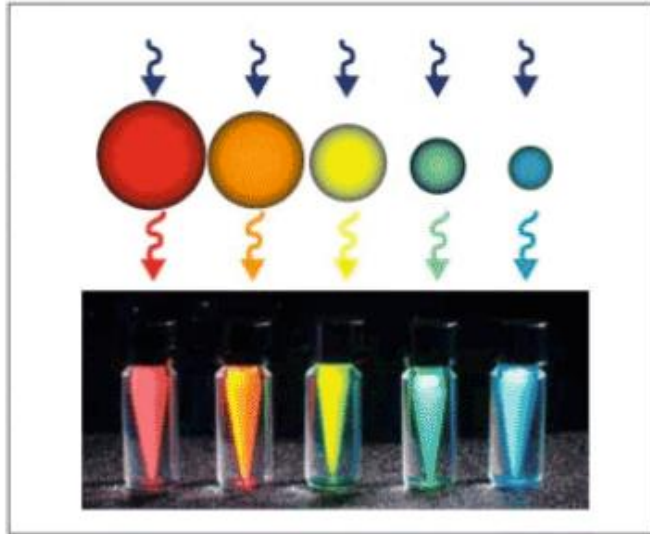
Preparation and Biomedical Applications of Magnetic Nanoparticles

Summary

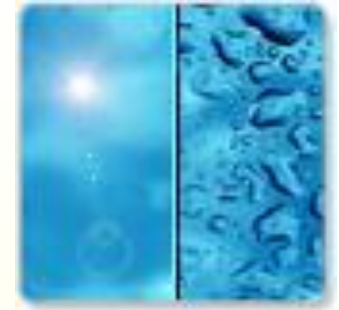
- 1- What are magnetic nanoparticles?
 - 2- Requirements for biomedical applications
 - 3- Basic principles in magnetism
 - 4- Biomedical applications
 - in vitro
 - in vivo
-
- 5- Synthesis routes
 - in solution
 - aerosol
 - 6-Example
-

Nanotechnology

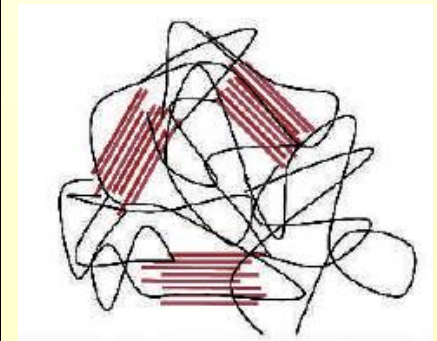
Particles



Films



Composites



Improving Smelly Socks

ARC Outdoors, ArcticShield Socks

Incorporate 19-nanometer antimicrobial **silver** particles within their fibers.

A comfortable synthetic fiber sock with permanent resistance to odor and fungus.



Magnetic nanoparticles



Magnetic nanoparticles



Inks



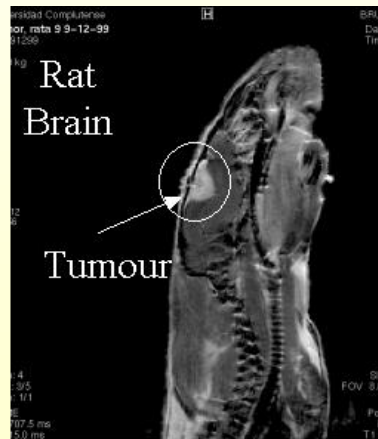
Loud speakers



Barcodes



Magnetic recording media



NMR Contrast agents



2004

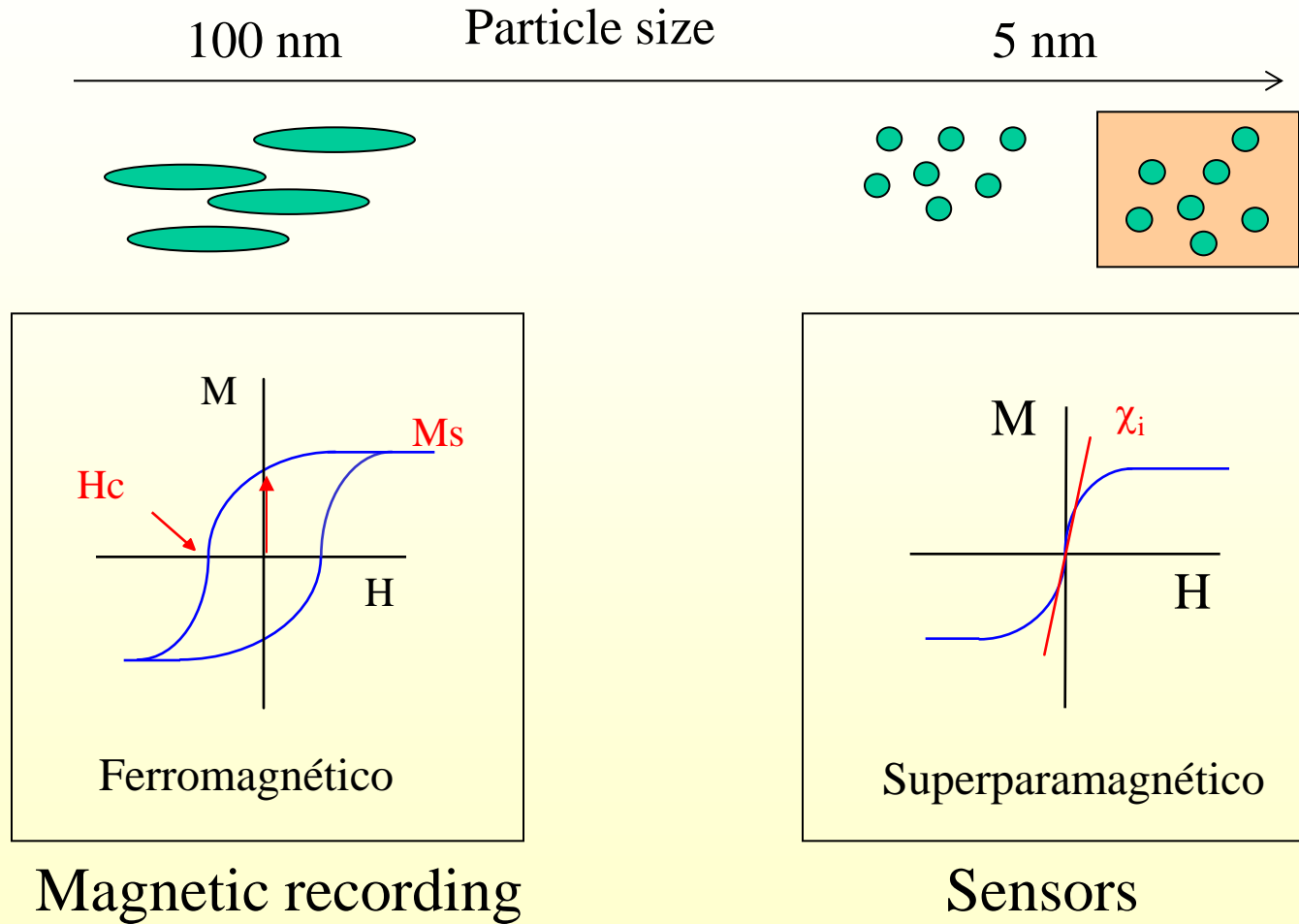
Formulaciones aprobadas por las diferentes agencias regulatorias.

Producto	Nanosistema	Indicación	Status	Compañía
Doxil (Barenholz, 2012)	Doxorrubicina encapsulada en liposomas PEGilados	Cáncer de ovarios	Aprobado 11/17/1995 FDA50718	Ortho Biotech (adquirida por JNJ)
Myocet (Waterhouse et al., 2001)	Doxorrubicina encapsulada en liposomas No PEGilados	Cáncer de mama metastásico	Aprobado en Europa y Canadá, en combinación con ciclofosfamida	Sopherion Therapeutics, LLC en América del Norte y Cephalon, Inc. en Europa
DaunoXome (Forssen, 1997)	Daunorrubicina encapsulada en liposomas	Tratamiento de sarcoma de Kaposi avanzado asociado al VIH	Aprobado en E.E.U.U	Galen Ltd.
ThermoDox (Dromi et al., 2007)	Doxorrubicina encapsulada en liposomas (liberación mediada por calor)	Cáncer de mama y primeras etapas de cáncer de hígado	Aprobación esperada para el año 2013	Celsion
Abraxane (Guarneri et al., 2012)	Nanopartículas de albúmina-paclitaxel	Diferentes tipos de cáncer	Aprobado 1/7/2005 FDA21660	Celgene
Rexin-G (Gordon and Hall, 2010)	MicroRNA-122 encapsulado en liposomas	Sarcoma, osteosarcoma, cáncer de páncreas, y otros tumores sólidos	Aprobado en Filipinas, Fase II y III en E.E.U.U	Epeius Biotechnologies Corp.
Oncaspar (Avramis and Tiwari, 2006)	Asparaginasa PEGilada	Leucemia linfoblástica aguda	Aprobado 24/06/2006	Enzon Pharmaceuticals, Inc.
Resovist (Hamm et al., 1994)	Nanopartículas de óxido de hierro recubiertas de carboxidextrano	Agentes de contraste para hígado y bazo	Aprobado en Europa en 2001	Bayer Schering Pharma AG
Feridex (Weissleder et al., 1989)	Nanopartículas de óxido de hierro recubiertas de dextrano	Agentes de contraste para hígado y bazo	Aprobado por la FDA en E.E.U.U en 1996	Berlex Laboratories
Endorem (Weissleder et al., 1989)	Nanopartículas de óxido de hierro recubiertas de dextrano	Agentes de contraste para hígado y bazo	Aprobado en Europa	Guerbet

Patrick Couvreur et al., Chem. Rev. 112, 5818, 2012

He was the first to develop nanometric capsules able to penetrate cells to deliver medicine

Magnetic nanoparticles

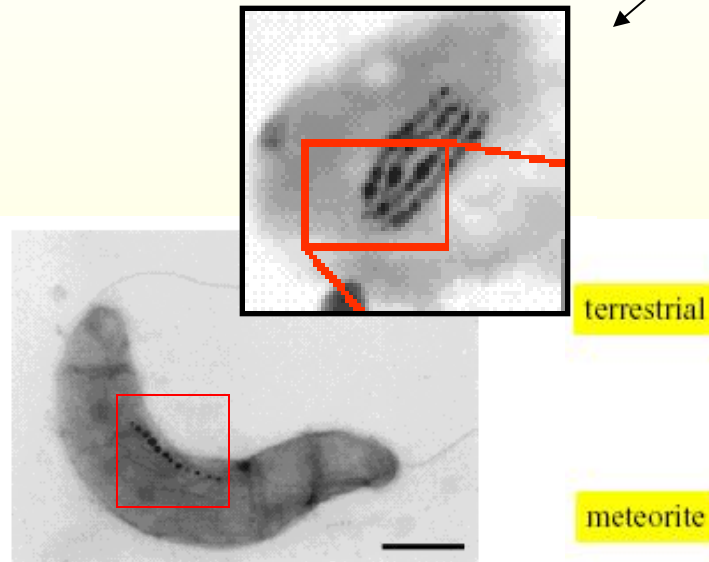
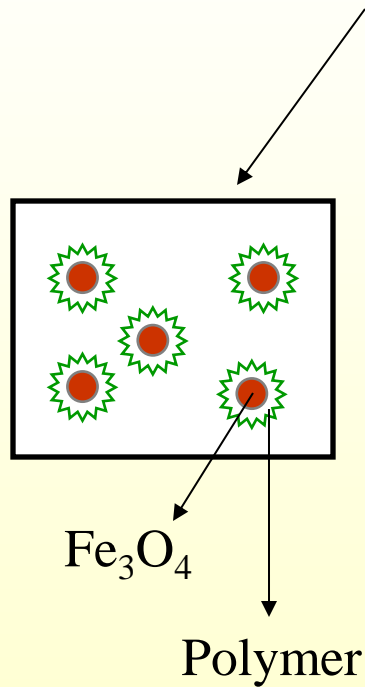


Magnetic nanoparticles

1 H																	2 He				
3 Li	4 Be	Red = Ferromagnetic Blue = Antiferromagnetic														5 B	6 C	7 N	8 O	9 F	10 Ne
11 Na	12 Mg															13 Al	14 Si	15 P	16 S	17 Cl	18 Ar
19 K	20 Ca	21 Sc	22 Ti	23 V	24 Cr 312 K	25 Mn 96 K	26 Fe 1043 K	27 Co 1390 K	28 Ni 629 K	29 Cu	30 Zn	31 Ga	32 Ge	33 As	34 Se	35 Br	36 Kr				
37 Rb	38 Sr	39 Y	40 Zr	41 Nb	42 Mo	43 Tc	44 Ru	45 Rh	46 Pd	47 Ag	48 Cd	49 In	50 Sn	51 Sb	52 Te	53 I	54 Xe				
55 Cs	56 Ba	57 La	72 Hf	73 Ta	74 W	75 Re	76 Os	77 Ir	78 Pt	79 Am	80 Hg	81 Tl	82 Pb	83 Bi	84 Po	85 At	86 Rn				
87 Fr	88 Ra	89 Ac																			
			58 Ce 13 K	59 Pr	60 Nd 19 K	61 Pm	62 Sm 105 K	63 Eu 90 K	64 Gd 293 K	65 Tb 229 221	66 Dy 179 85	67 Ho 132 20	68 Er 85 20	69 Tm 56 K	70 Yb	71 Lu					
			90 Th	91 Pa	92 U	93 Np	94 Pu	95 Am	96 Cm	97 Bk	98 Cf	99 Es	100 Fm	101 Md	102 No	103 Lr					

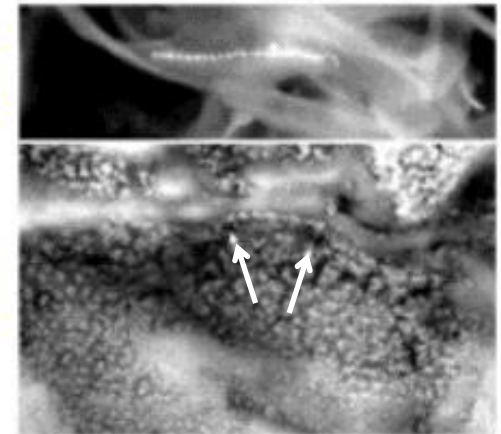
Magnetic nanoparticles

MAGNETIC NANOPARTICLES \Leftrightarrow LIVING SYSTEMS



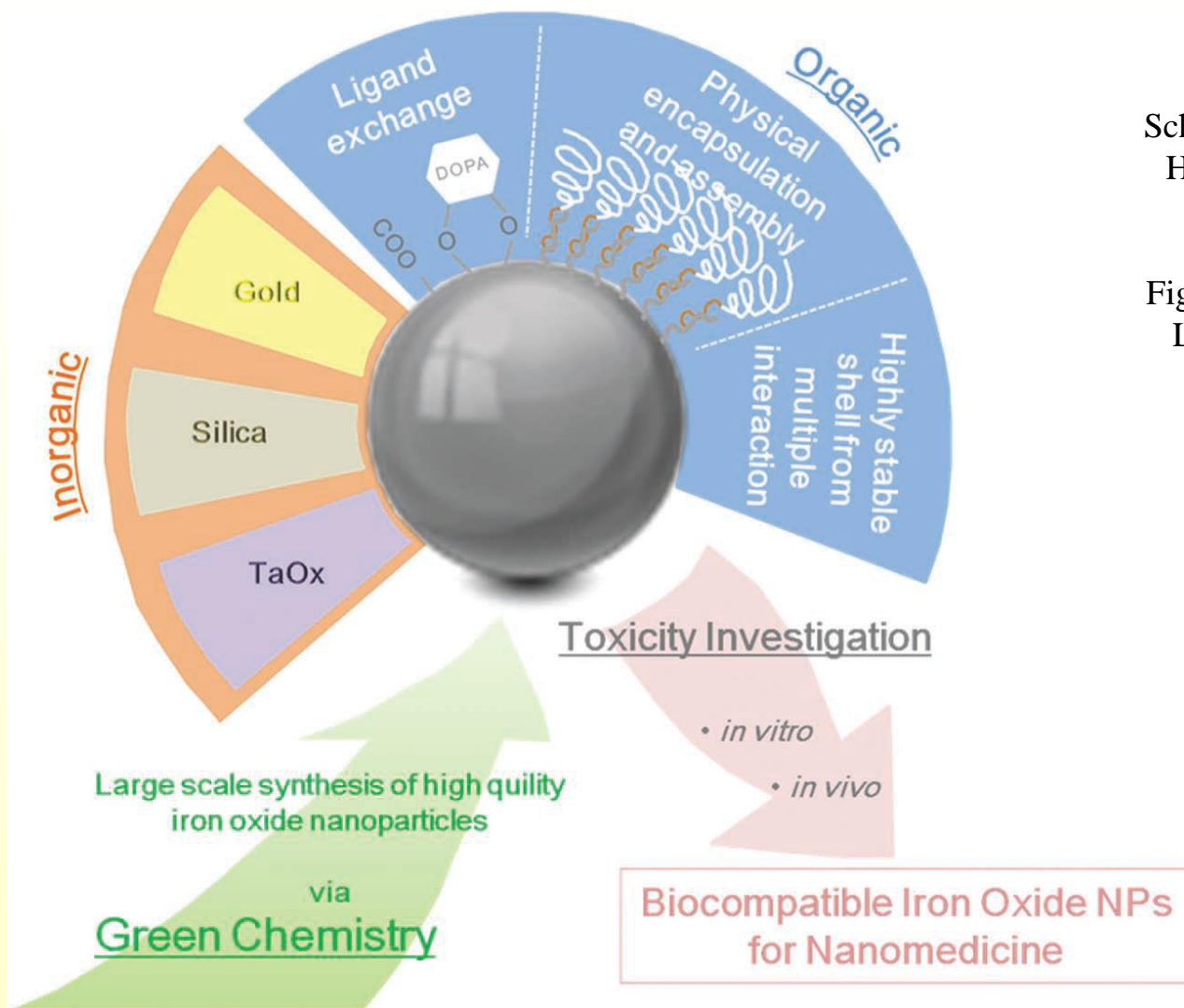
Magnetotactic bacteria

For orientation



Life in Mars?

Magnetic nanoparticles



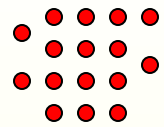
Chem. Soc. Rev., 2012, 41, 4306

Schladt, T. D.; Schneider, K.; Schild, H.; Tremel, W. *Dalton transactions* 2011, 40, 6315

Figuerola, A.; Corato, R. Di; Manna, L.; Pellegrino, T. *Pharmacological Research* 2010, 62, 126

Chemical Design of Biocompatible Iron Oxide Nanoparticles for Medical Applications,
Daishun Ling and Taeghwan Hyeon, Small 2013, 9, No. 9–10, 1450–1466,

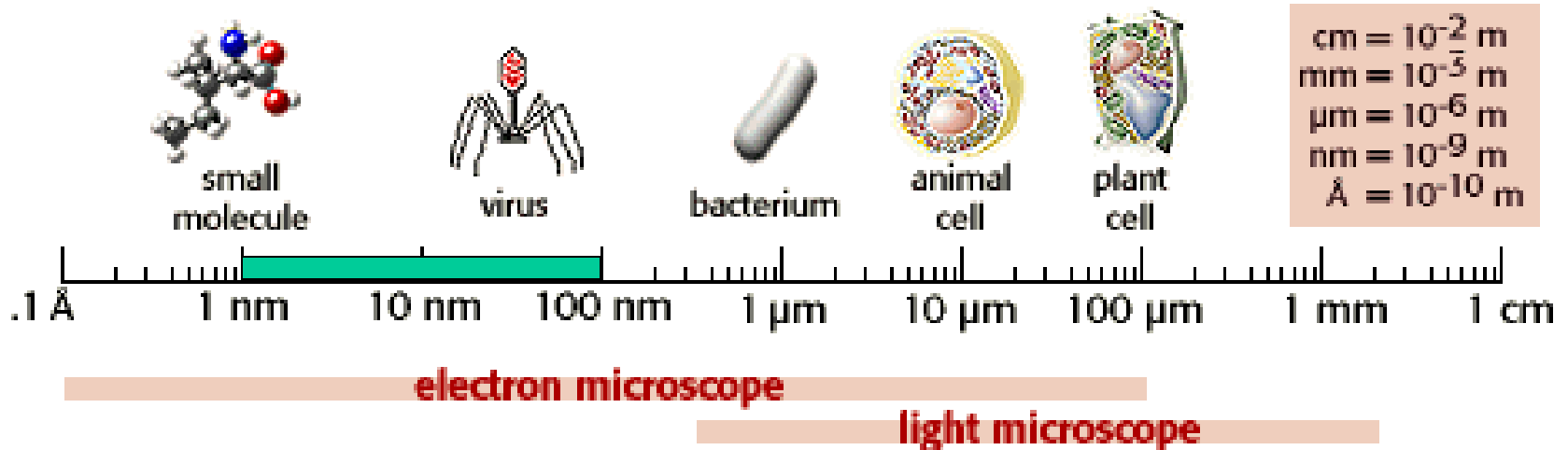
Magnetic nanoparticles



- Nanometer** => **Size:** Get close to a biological entity of interest
=> **Surface:** Bind a biological entity
=> **Properties:** Manipulated by a magnet

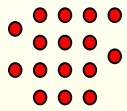


Relative sizes of cells and their components

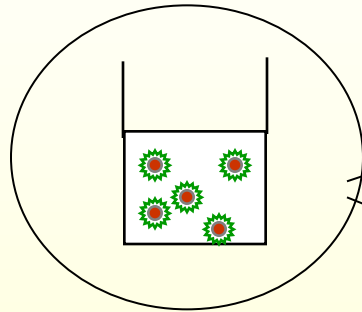


Requirements for biomedical applications

NANOPARTICLES



**COLLOIDAL
SUSPENSIONS**



APPLICATIONS

In vitro

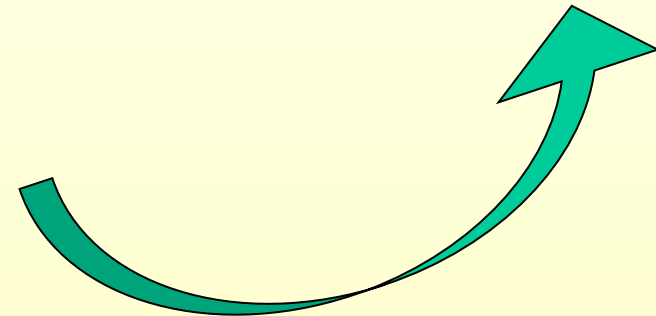
In vivo

REQUIREMENTS

- Size
- Surface
- Properties

No toxic!!

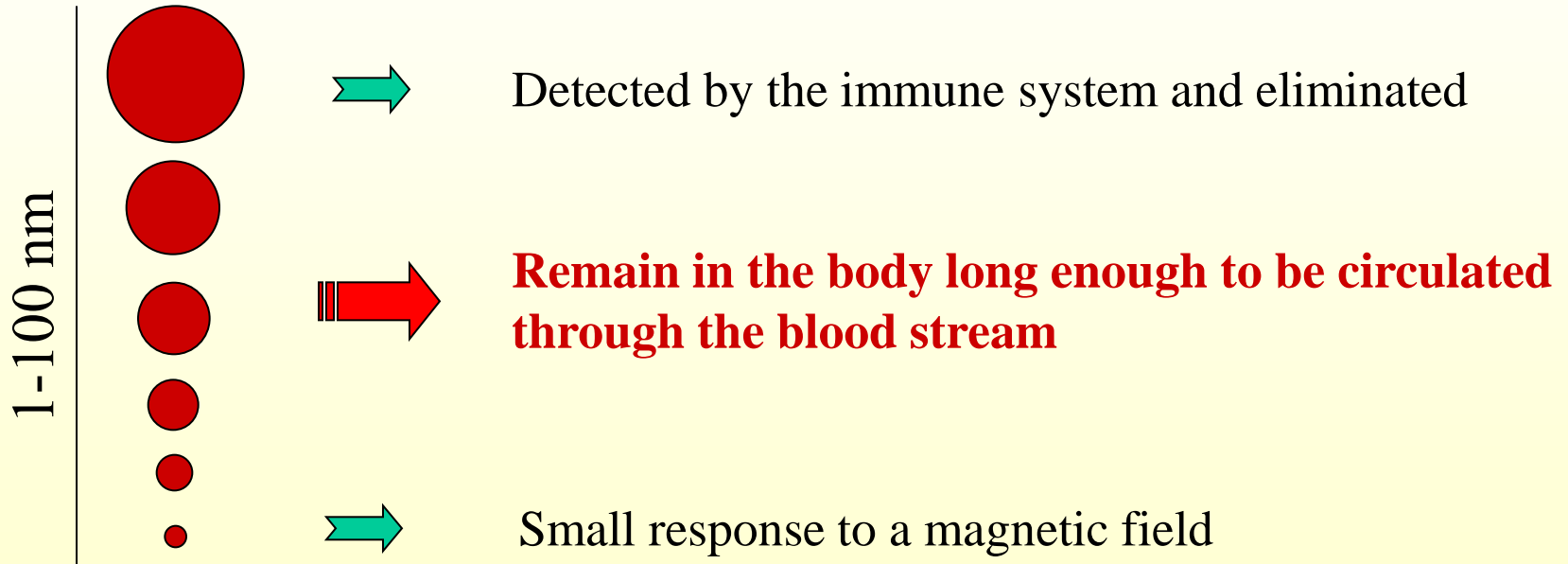
- Stable
- Biocompatible
- Reversible



Requirements for biomedical applications

Size

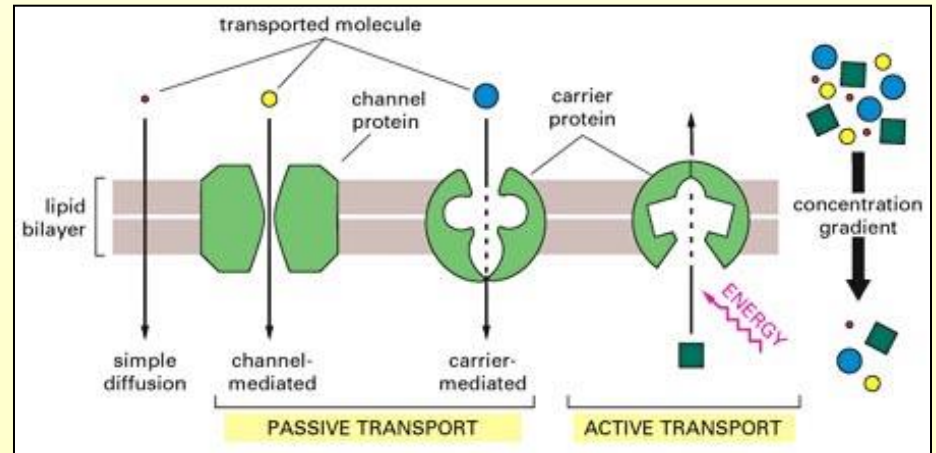
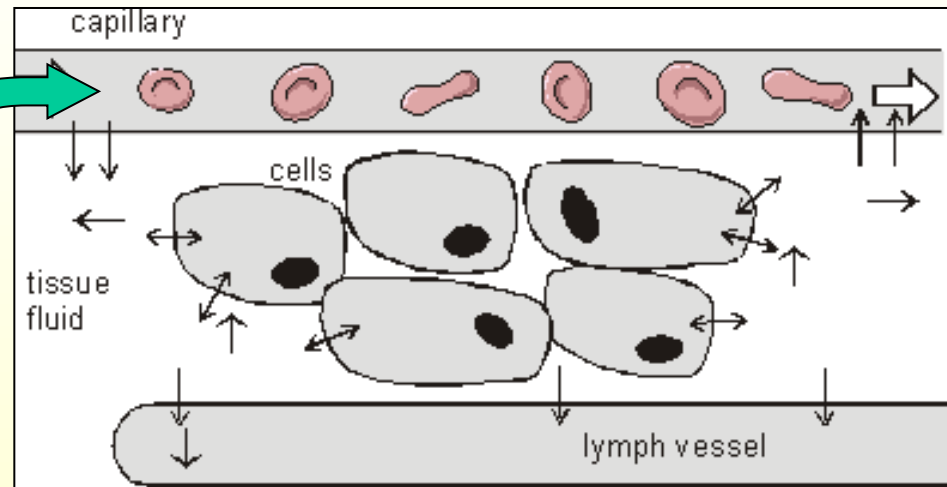
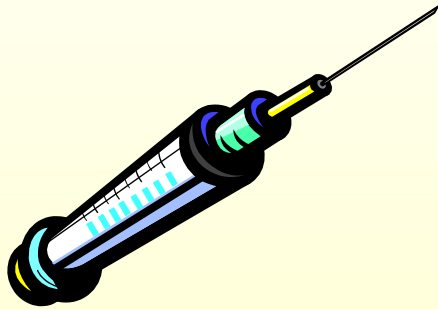
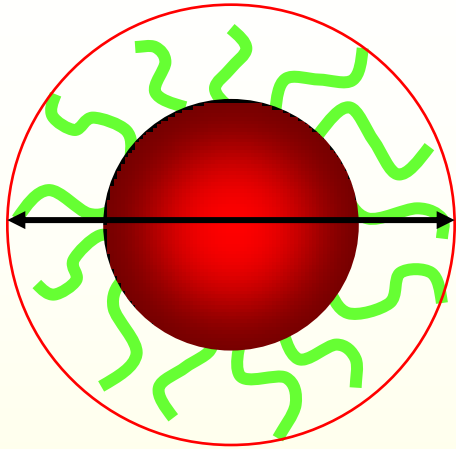
5-50 nm = Ideal diameter for most forms of therapy



Requirements for biomedical applications

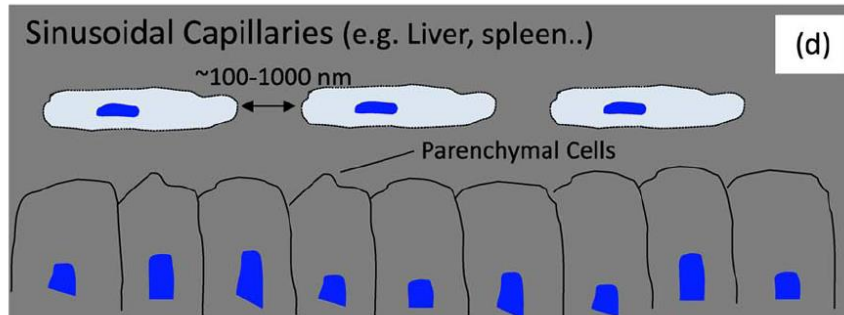
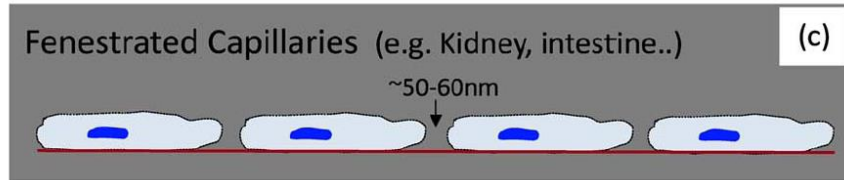
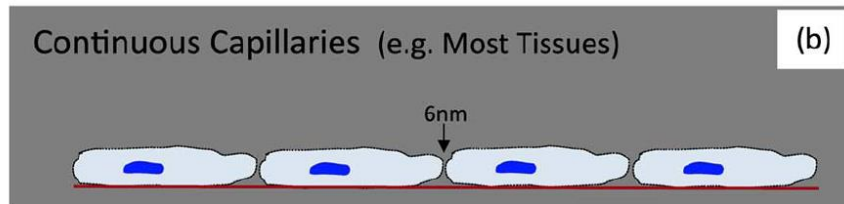
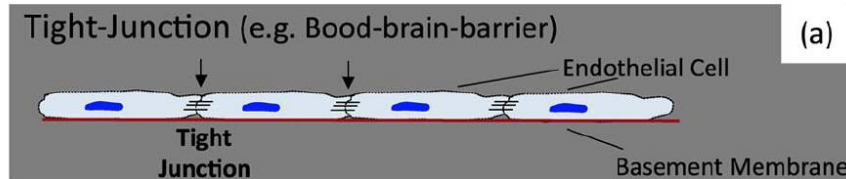
Hydrodynamic size

Core + Molecules around



Requirements for biomedical applications

Biology barriers



Gaps between endothelial cells

2 nm

6 nm

50 nm

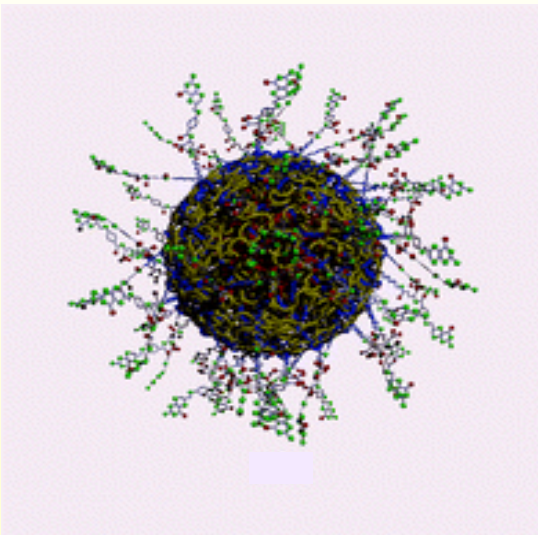
> 100 nm

Blood capillaries

Requirements for biomedical applications

Surface

Modification of the particle's surface to make it biocompatible and specific



=> **Biocompatible = Hydrophilic coating** make the particle look friendly to the immune system

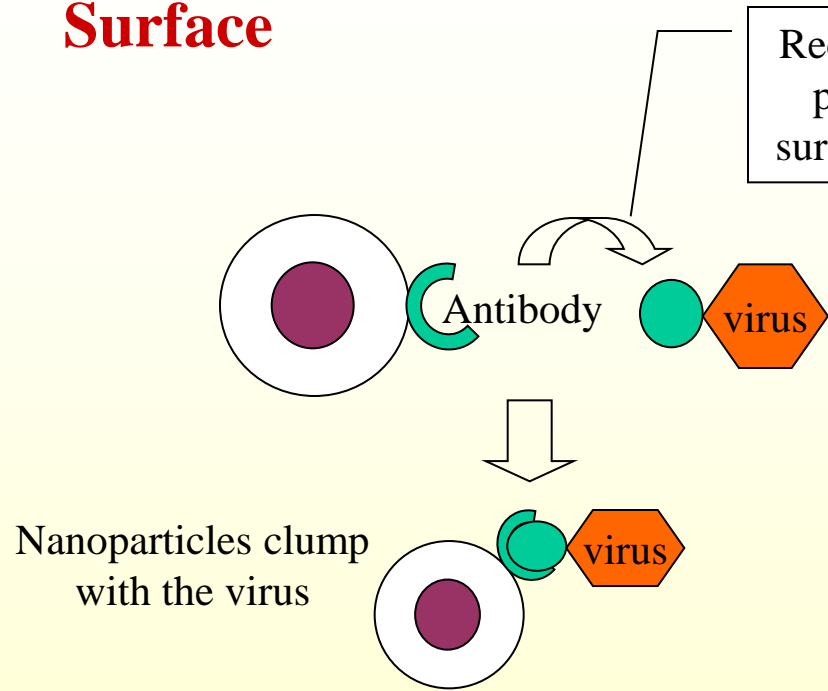
- Polymer
- Inorganic

=> **Specific = Coated with a biological entity** to make the particles function in a specific manner

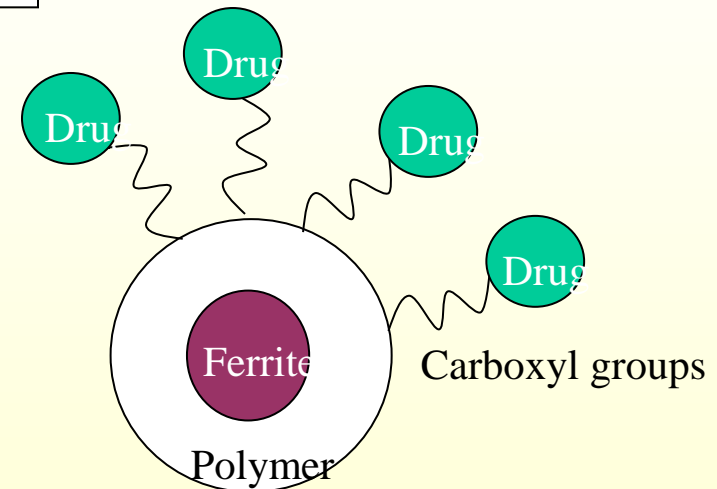
=> **Carrier =** to transport and deliver a biological active agent

Requirements for biomedical applications

Surface



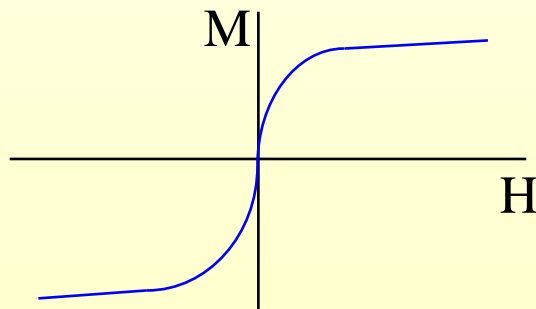
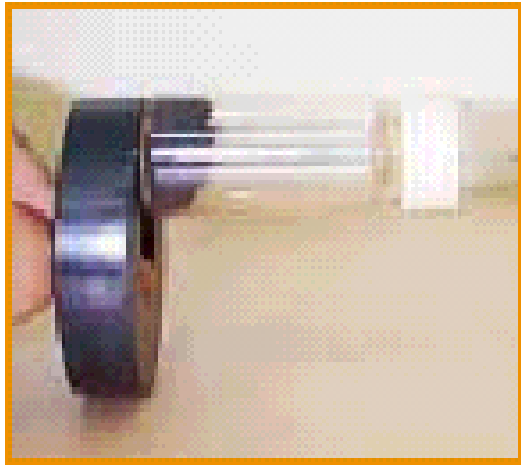
Detect virus in body fluids



Recognise and destroy a cancer cell

Requirements for biomedical applications

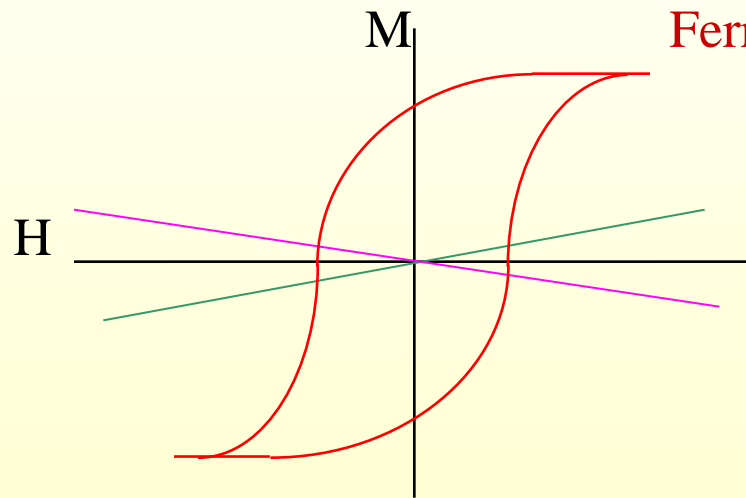
Magnetic properties



- They must **constantly and rapidly** “flip” magnetic states.
=> $M_r=0$
- **Saturation magnetisation** (M_s) should be **strong enough** to be manipulated by an external magnetic field
- **Resonant respond** to a time-varying magnetic field should be enough to heat up.

Basic principles in magnetism

All materials are magnetic to some extent with their magnetic response depending on their atomic structure and temperature



Ferromagnetic, ferrimagnetic and antiferromagnetic

Ordered magnetic states
 $M = 10^4$ times larger

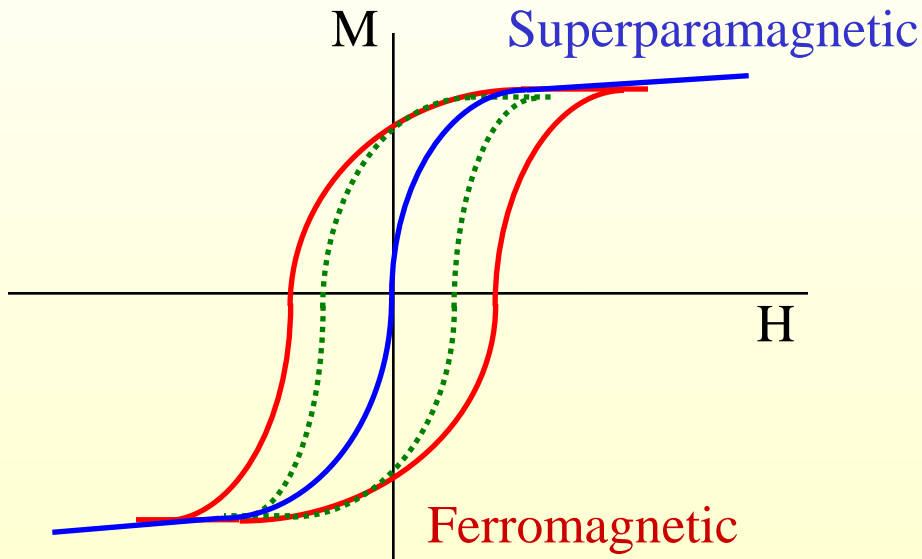
Paramagnetic

Diamagnetic

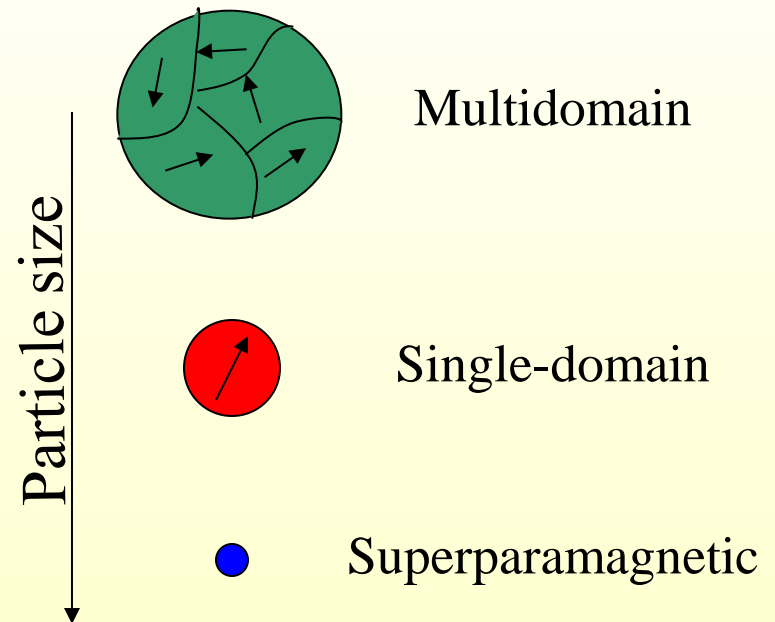
Little magnetism, only in the presence of a magnetic field

Basic principles in magnetism

The shape of the loops are determined in part by the particle size



Domain structure



Basic principles in magnetism

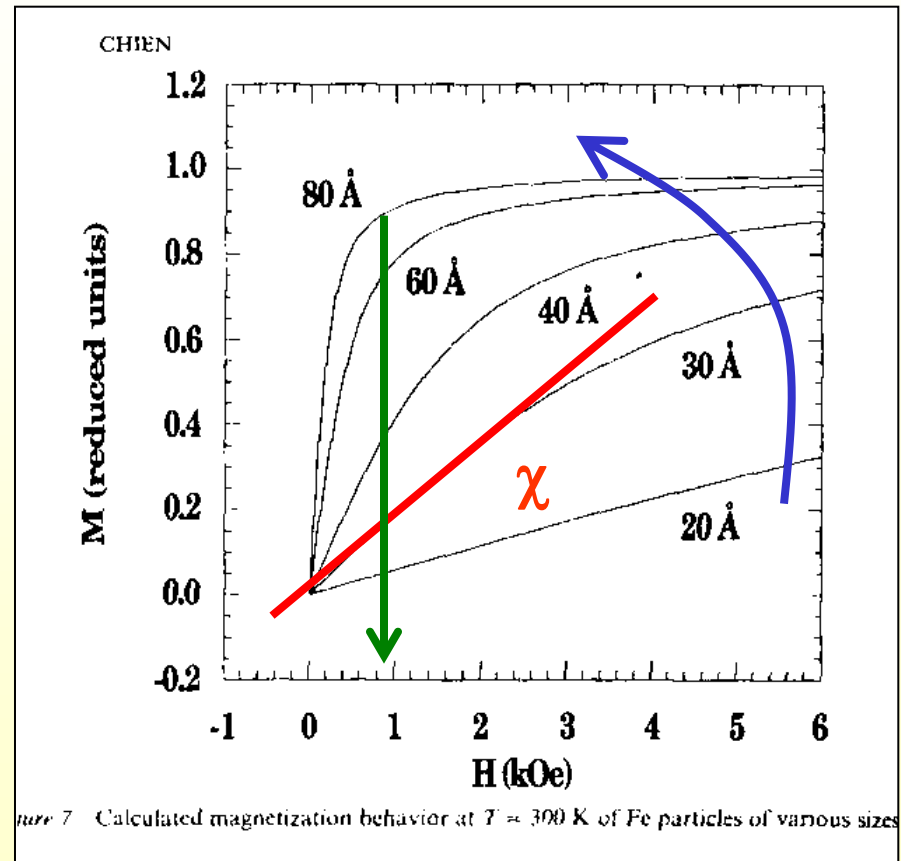
Superparamagnetism

Particle size

Magnetic behaviour

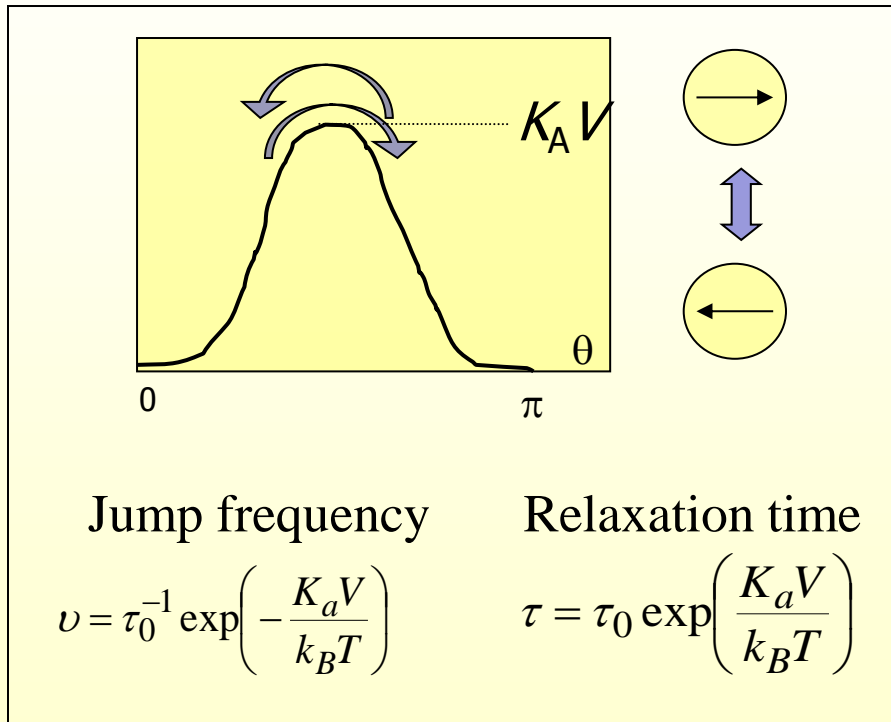
$$\chi \approx \frac{VM_s^2}{3k_B T}$$

Saturation field



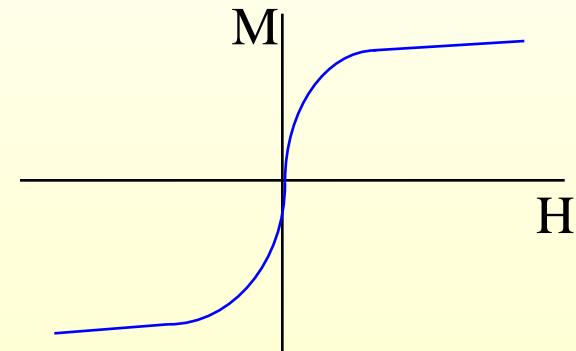
Basic principles in magnetism

Superparamagnetism



Small particle size

$$\Delta E = K_a V \approx k_B T$$

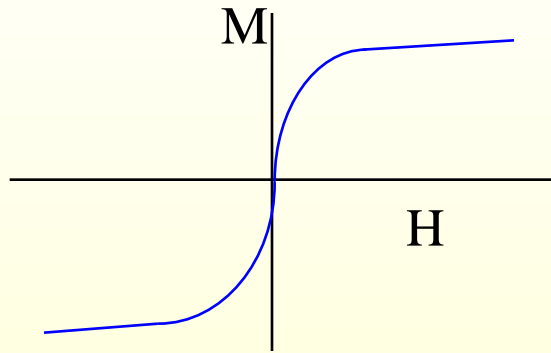


No particle aggregation

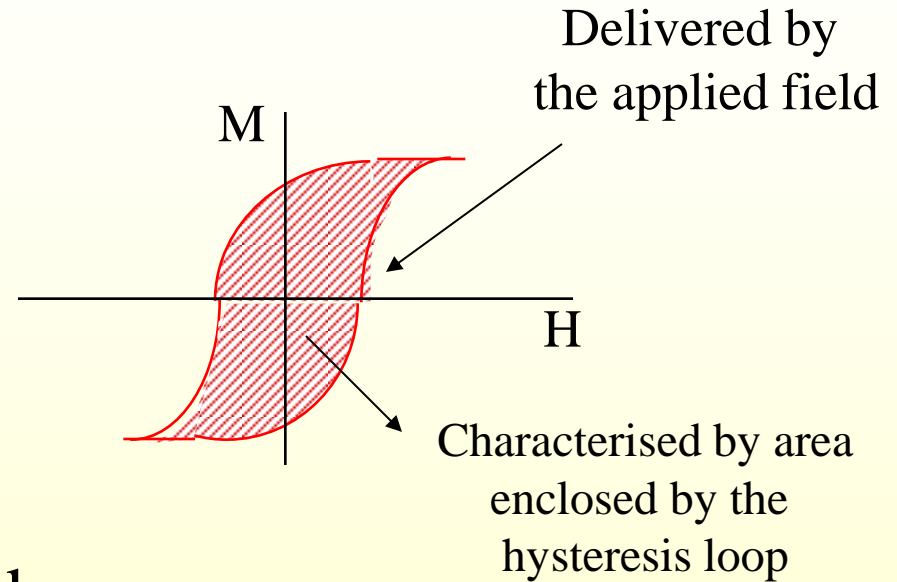
Reversible behaviour

Basic principles in magnetism

Ferromagnetism

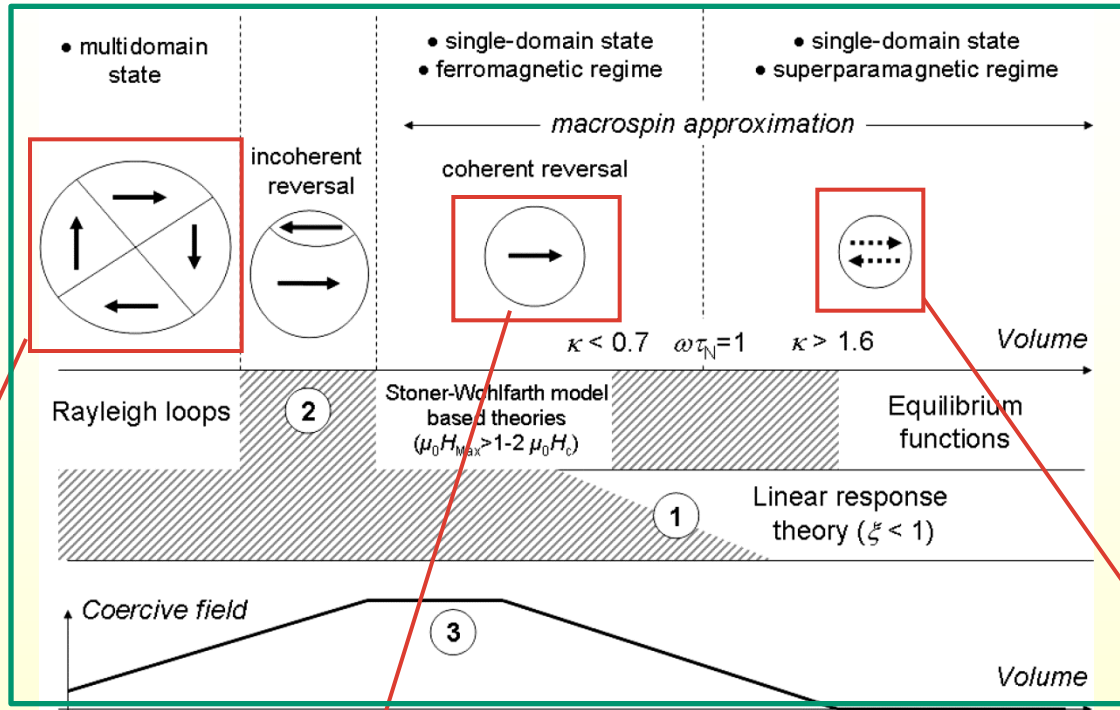


Alternating
magnetic field



Thermal
energy

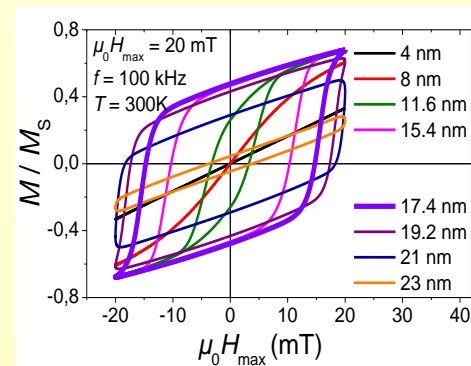
Basic principles in magnetism



- Drop of coercive field \rightarrow less efficient
- No prediction possible

- No hysteresis \rightarrow no interest
- Analytical calculation : Langevin..

- Open hysteresis loops \rightarrow **optimized nanoparticles**
- Analytical calculations : Stoner-Wohlfarth model



Biomedical applications

• In vitro → Diagnostic → **Separation/selection** ←

• In vivo → Diagnostic → **NMR imaging** ←

• In vivo

Therapeutic

Drug targeting

Hyperphermia

Gene delivery

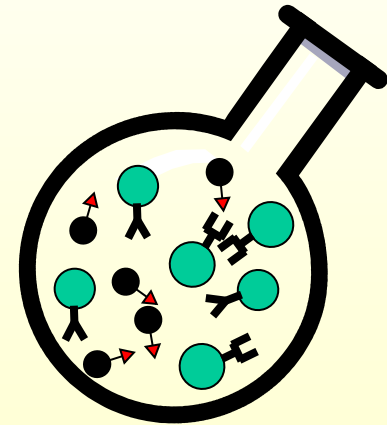
Tissue regeneration (cell labelling)

Separation/selection

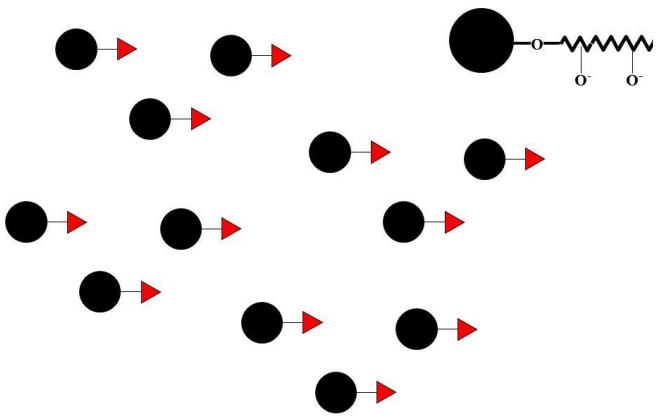
- Goal: Separate/detect/isolate one type of cell from others, often when the target is present in very small quantities



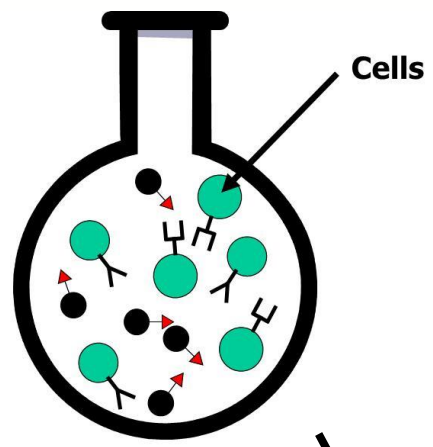
Reduce the time
Detect lower concentrations



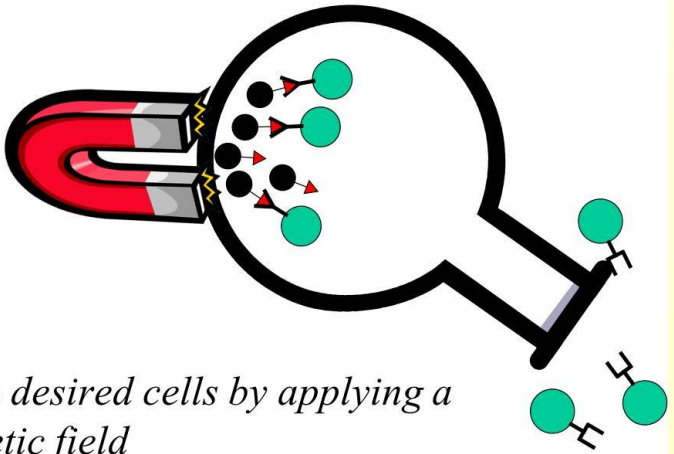
Separation/selection



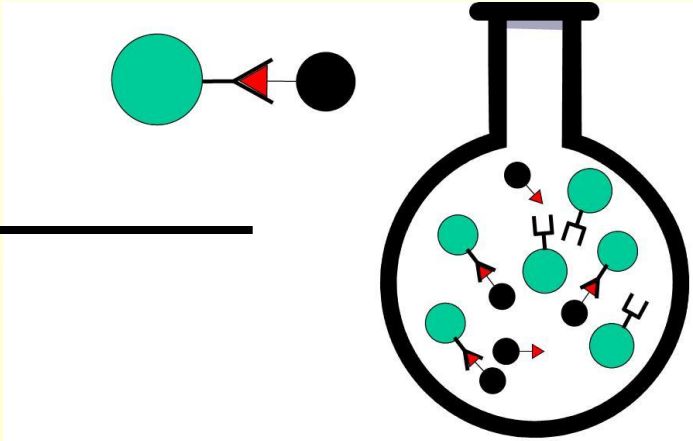
Functionalized nanoparticles



Add to sample

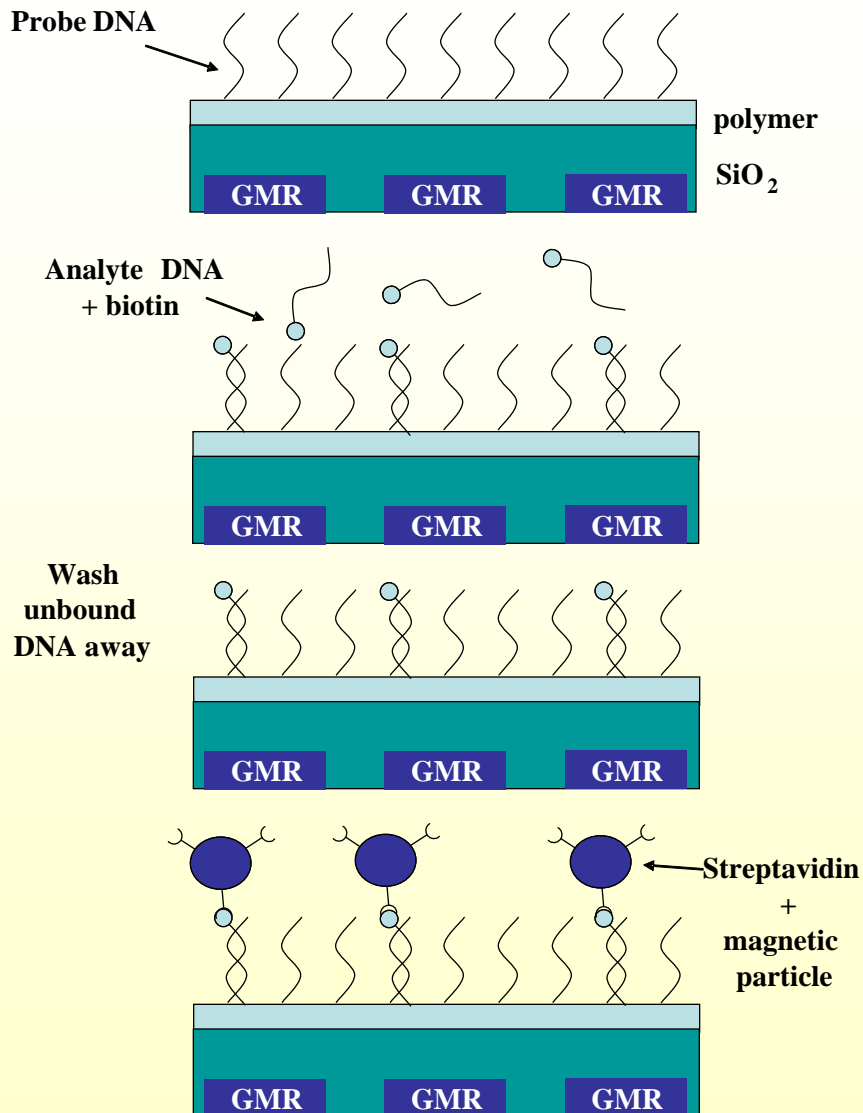


Retain desired cells by applying a magnetic field



Magnetic nanoparticles bond with targeted cells

Separation/selection

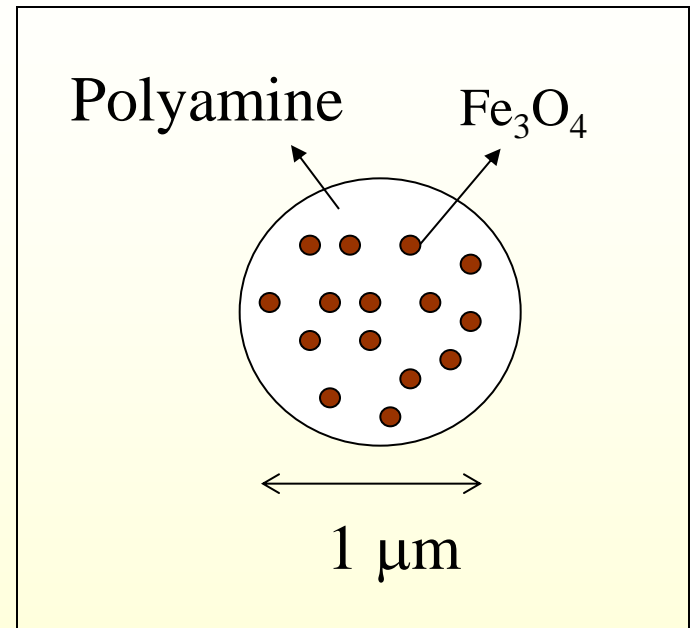
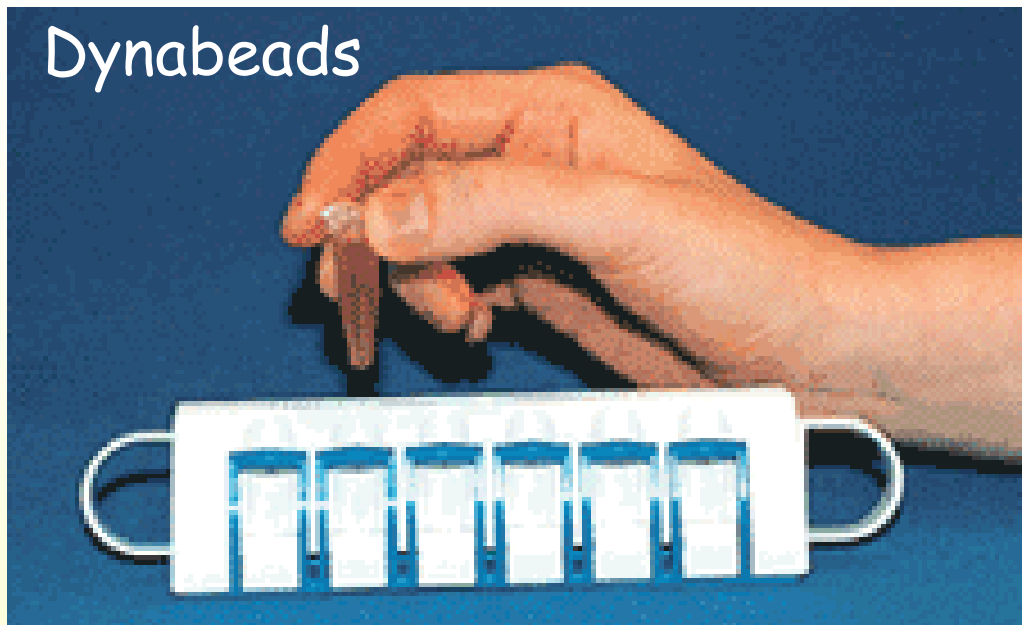


Magnetic Sorting/Detection

- **High sensitivity**
- **Multiple analytes at one time**
- **Hand-held**
- **Lightweight**
- **Fast**
- **Potential for single-bead detection**

Biomedical applications

Separation/selection

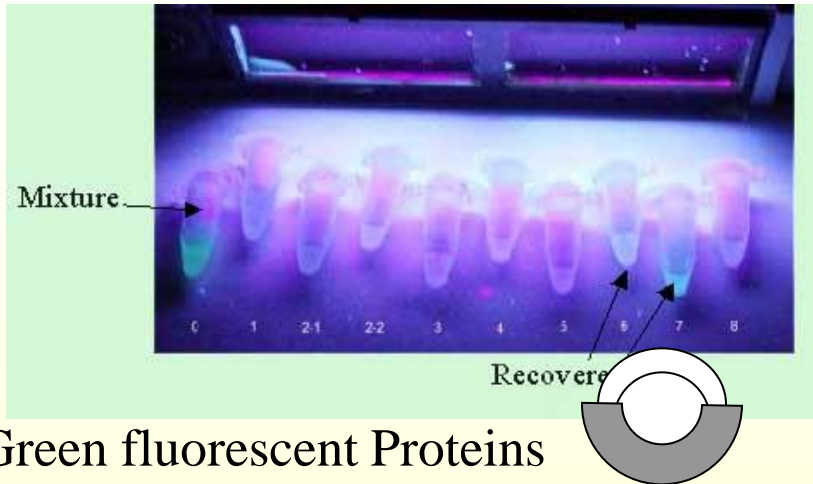


Separación y purificación

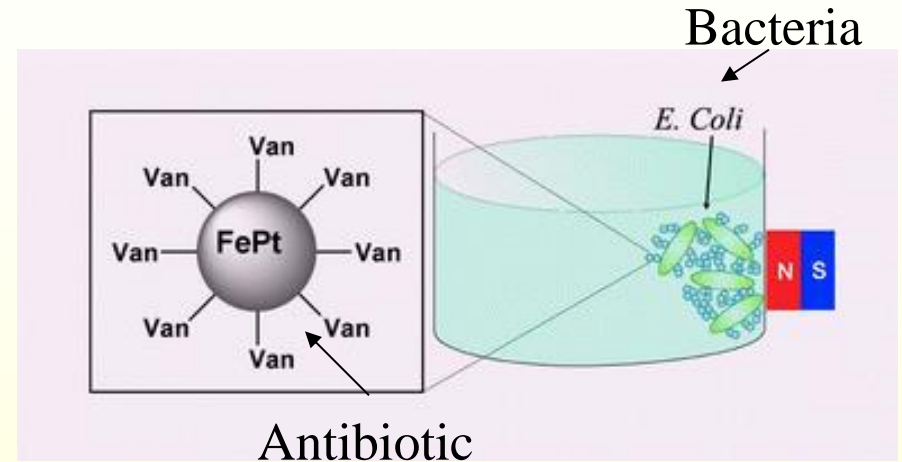
- ✓ Detection of proteins at 10^{-18} M = Prostate-specific antigen (PSA)
- ✓ Detection of DNA at 10^{-21} M **6 orders of magnitude more sensitive**

Biomedical applications

BIOMOLECULE SEPARATIONS



FOOD QUALITY CONTROL



WATER PURIFICATION (Ar, Pb...)

884 millones = Personas que carecen de acceso a fuentes de abastecimiento de agua potable (una de cada ocho)

Biomedical applications

NMR IMAGING



The most powerful technique for diagnosis

Nobel Prize 2003

Paul C. Lauterbur and Sir Peter Mansfield
"for their discoveries concerning magnetic resonance imaging"

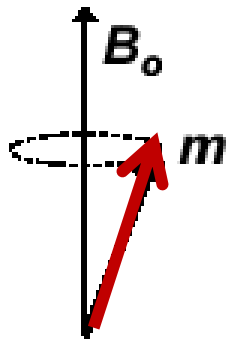
Advantage: not use X-Rays nor any other type of "ionizing" radiation

Instead: it is a technique that combines a large magnetic field and some radio frequency antennas

Measure the **relaxation** rate of **protons** in the atoms of **water** within the patient from their excited state to the ground state

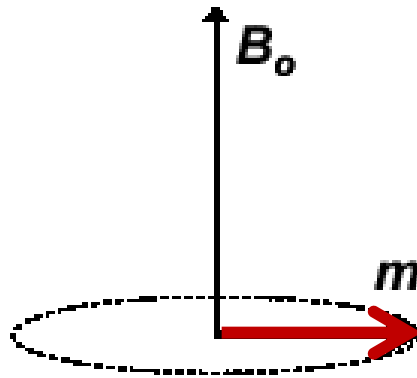
NMR imaging

magnetic field



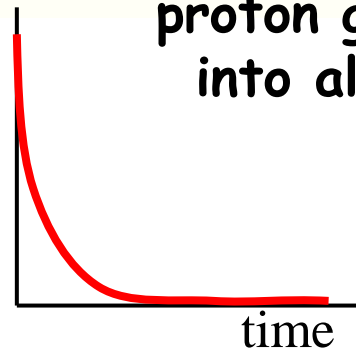
protons of water "line-up"

high-frequency electro-magnetic pulse



protons out of alignment

M



"resonance" signal as the proton goes back into alignment

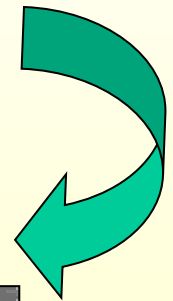


image reflects the water protons in the patient and their chemical association with proteins



NMR imaging

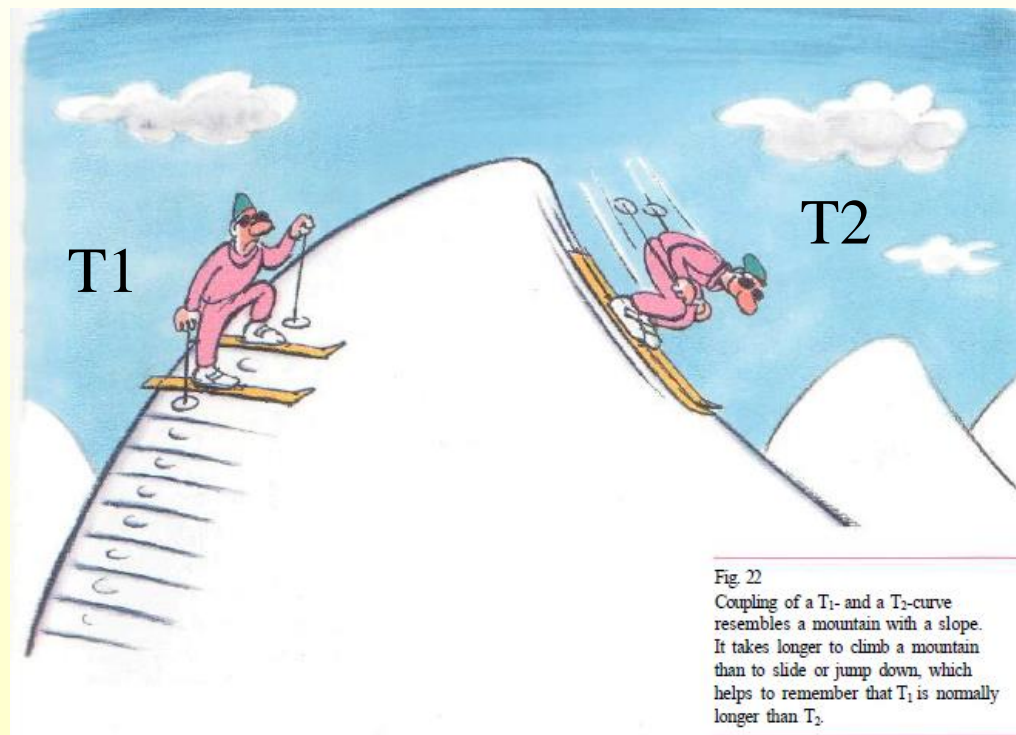
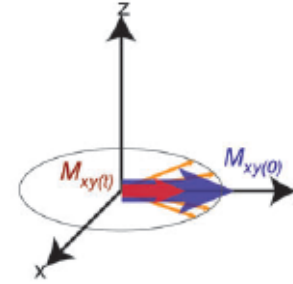
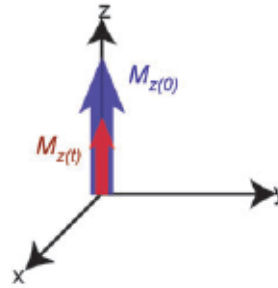
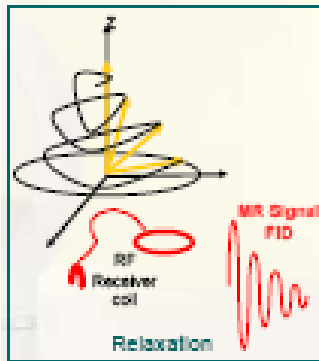


Fig. 22
Coupling of a T_1 - and a T_2 -curve resembles a mountain with a slope. It takes longer to climb a mountain than to slide or jump down, which helps to remember that T_1 is normally longer than T_2 .

MRI made easy

Instituto de Ciencia
de Materiales de Madrid

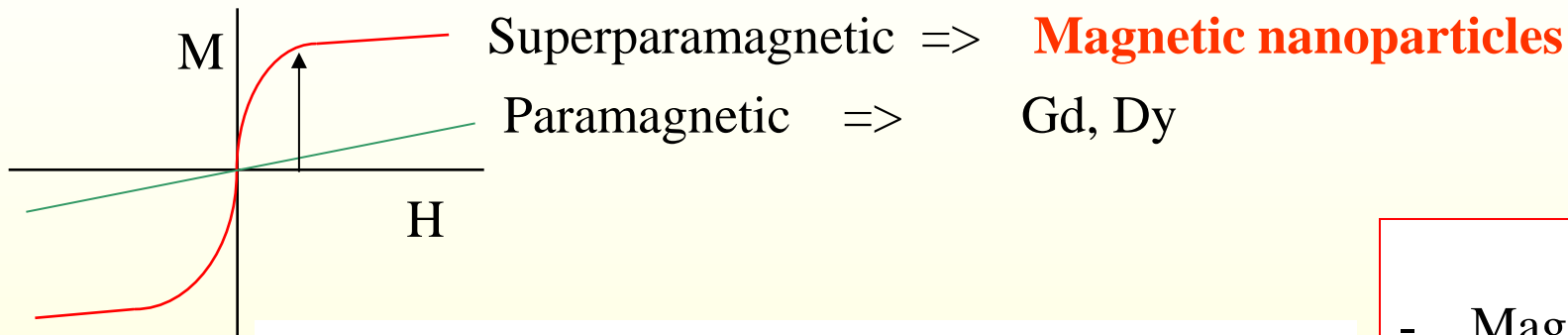


CSIC

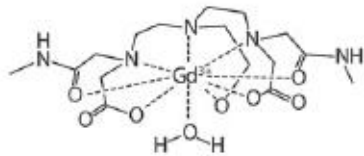
CONSEJO SUPERIOR DE INVESTIGACIONES CIENTÍFICAS

Contrast agents for NMR imaging

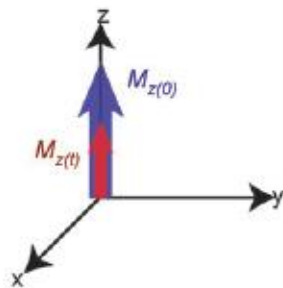
Enhance the contrast between normal and diseased tissues, indicate organ function or blood flow



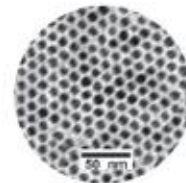
T_1 Agents



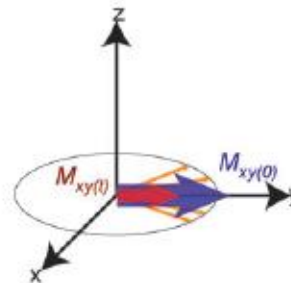
Omniscan™



T_2 Agents

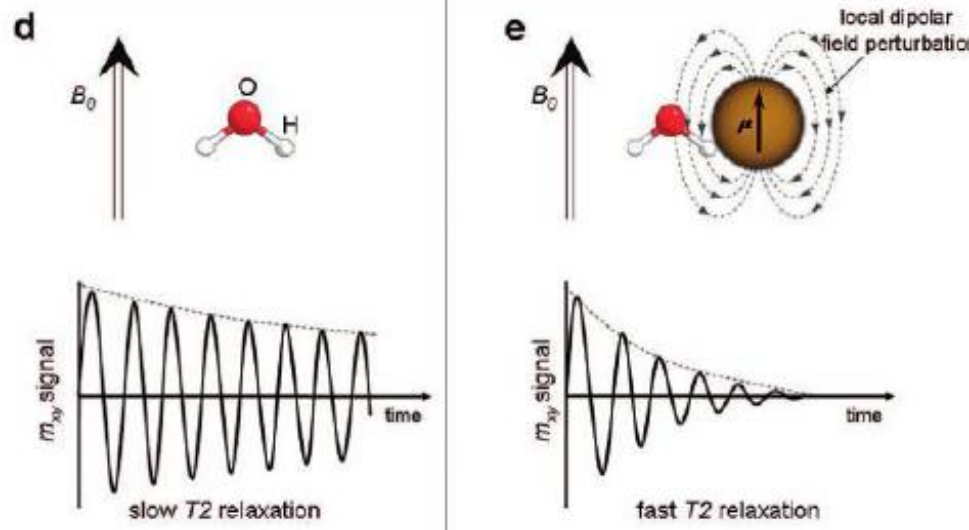


Fe₃O₄ Nanoparticles



- Magnetic moment 10^4 times larger
- 80-90% saturation at lower field

Contrast agents for NMR imaging



Cheon et al, ACCOUNTS OF CHEMICAL RESEARCH
1630-1640 December 2008 Vol. 41, No. 12

Shorter relaxation (T_2)
=> **Darker** in the MRI



$$\frac{1}{T_2} = R_2 = \frac{\left(\frac{64\pi}{135000}\right) \gamma^2 N_A M \mu^2}{r D}$$

NP radio

Diffusion coefficient
of water molecules

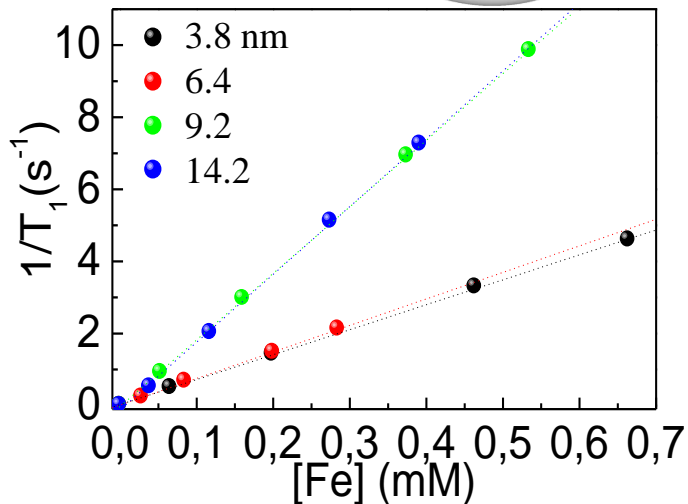
NP magnetic
moment

Concentration
(mole.L⁻¹)

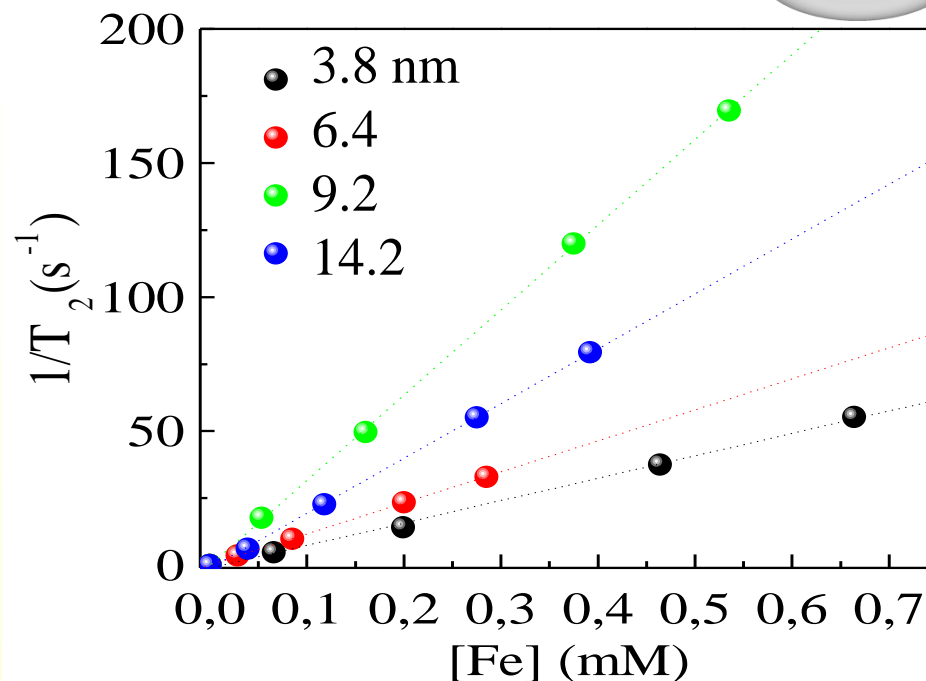
Contrast agents for NMR imaging

MINISPEC MQ60 (37 ° C, 1.5 T)

T1



T2



$$1/T_{1,2} = 1/T_{1,2}^0 + r_{1,2} [Fe]$$

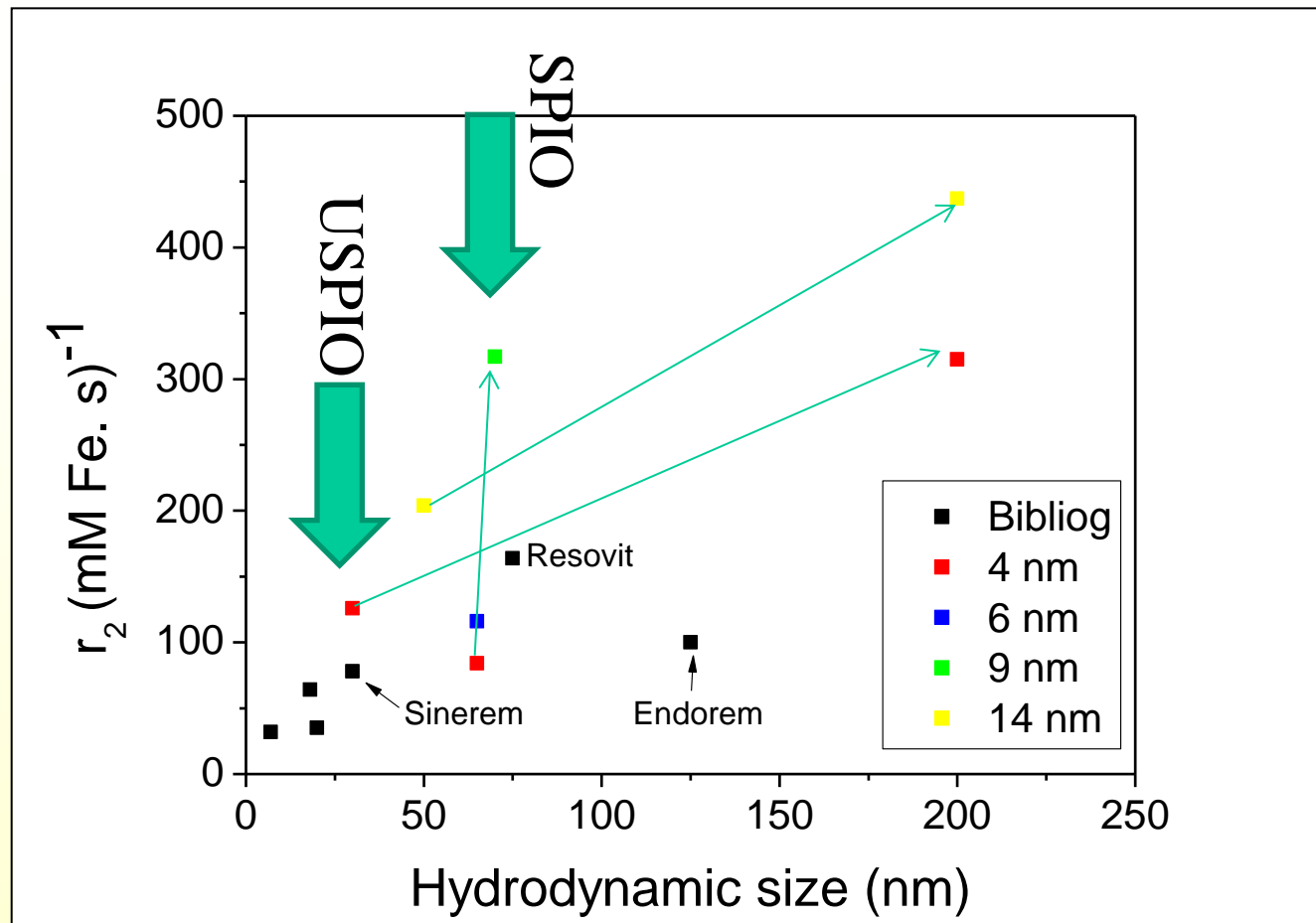
$r_{1,2}$ = Relaxivity constant

Measurement of the efficiency of the contrast agent

$1/T_2 = R_{1,2}$ = Inverse of the relaxation time
 $[Fe]$ = Concentration of iron in mmol l⁻¹

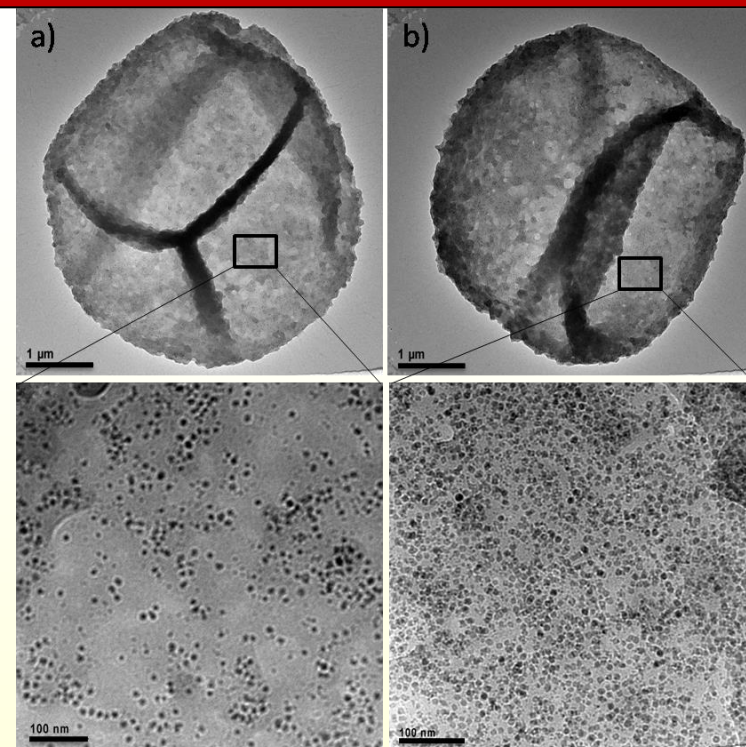
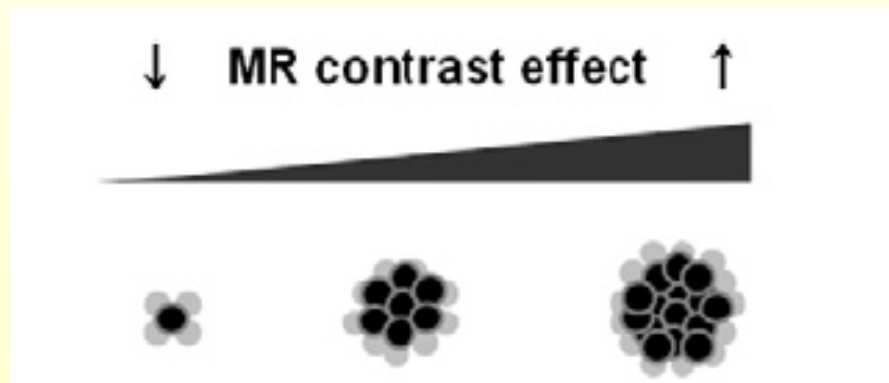
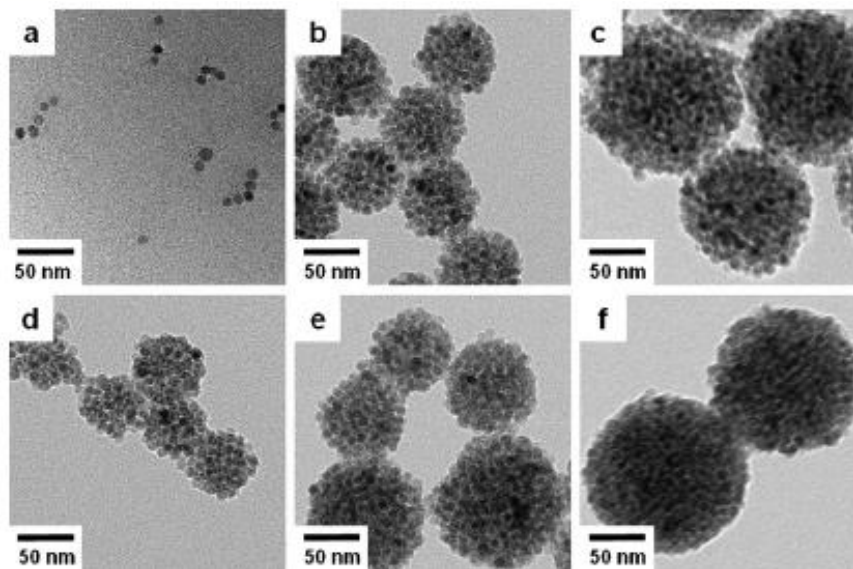
Contrast agents for NMR imaging

Commercial products = 5-10 nm



High crystalline particles lead to high relaxivity values

Contrast agents for NMR imaging



Azhar Zahoor Abbasi. *Phys. Chem. C* 2011, 115, 6257

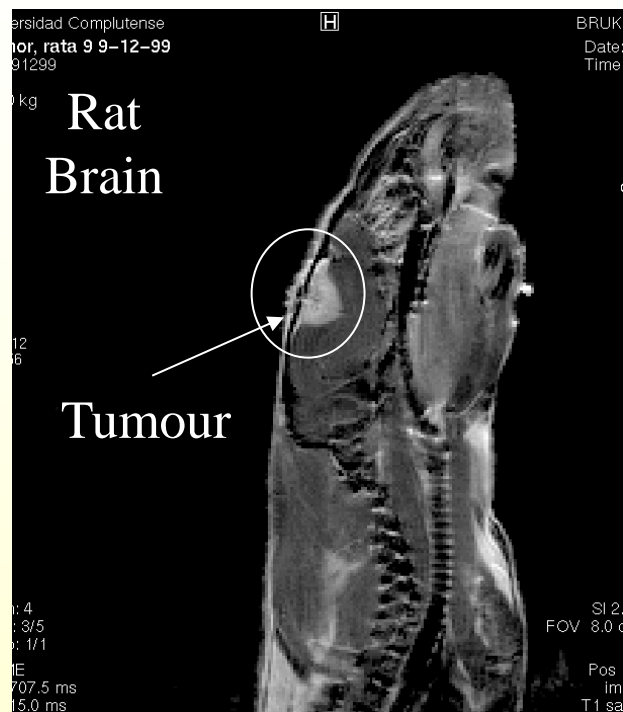
S.-B. Seo et al. / Journal of Colloid and Interface Science 319 (2008) 429–434

Instituto de Ciencia
de Materiales de Madrid



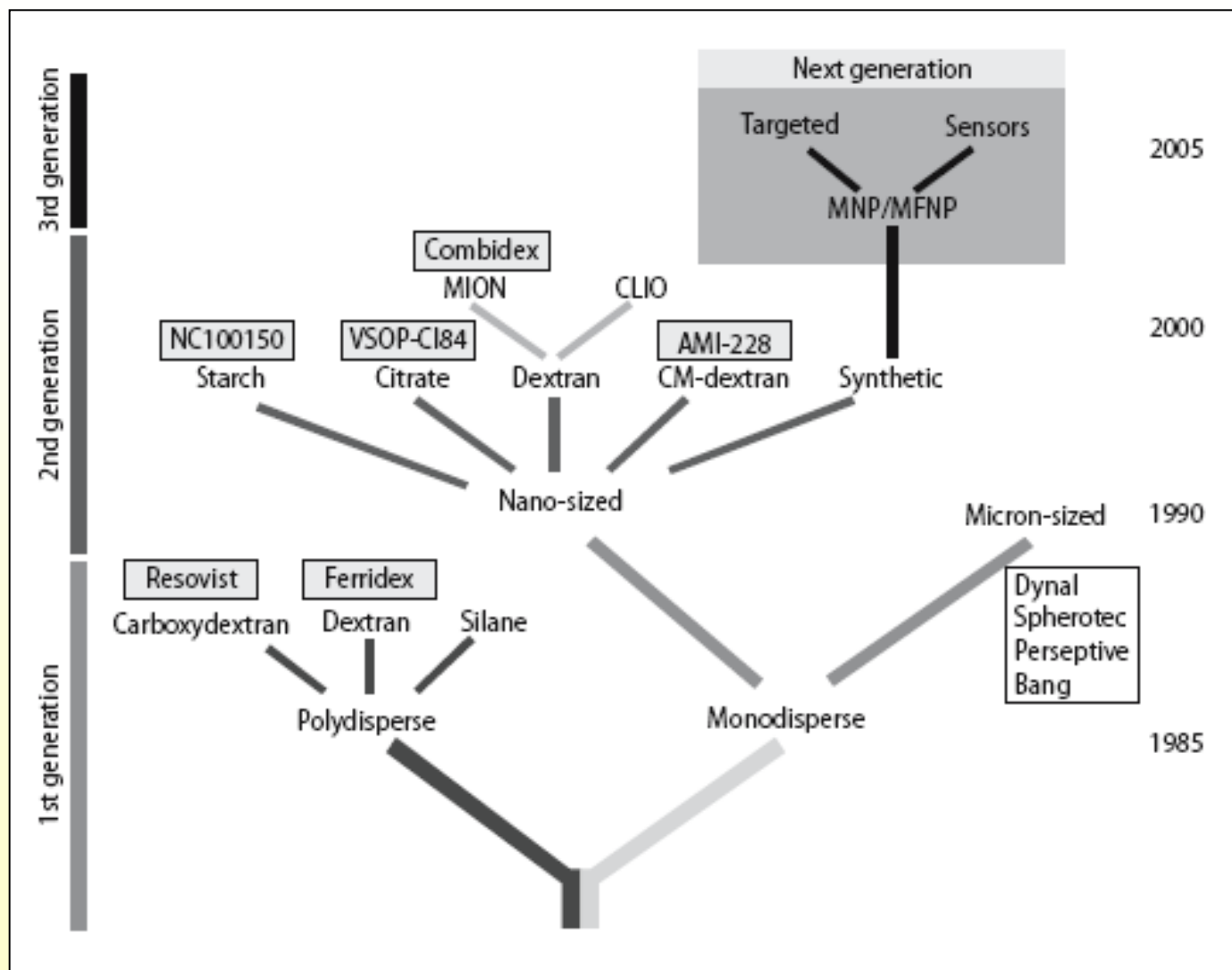
CONSEJO SUPERIOR DE INVESTIGACIONES CIENTÍFICAS

Contrast agents for NMR imaging



Tumour cells prevent the flow of macrophages and magnetic nanoparticles do not get to them
=> no decrease in signal intensity => appeared as **bright spots**

Contrast agents for NMR imaging

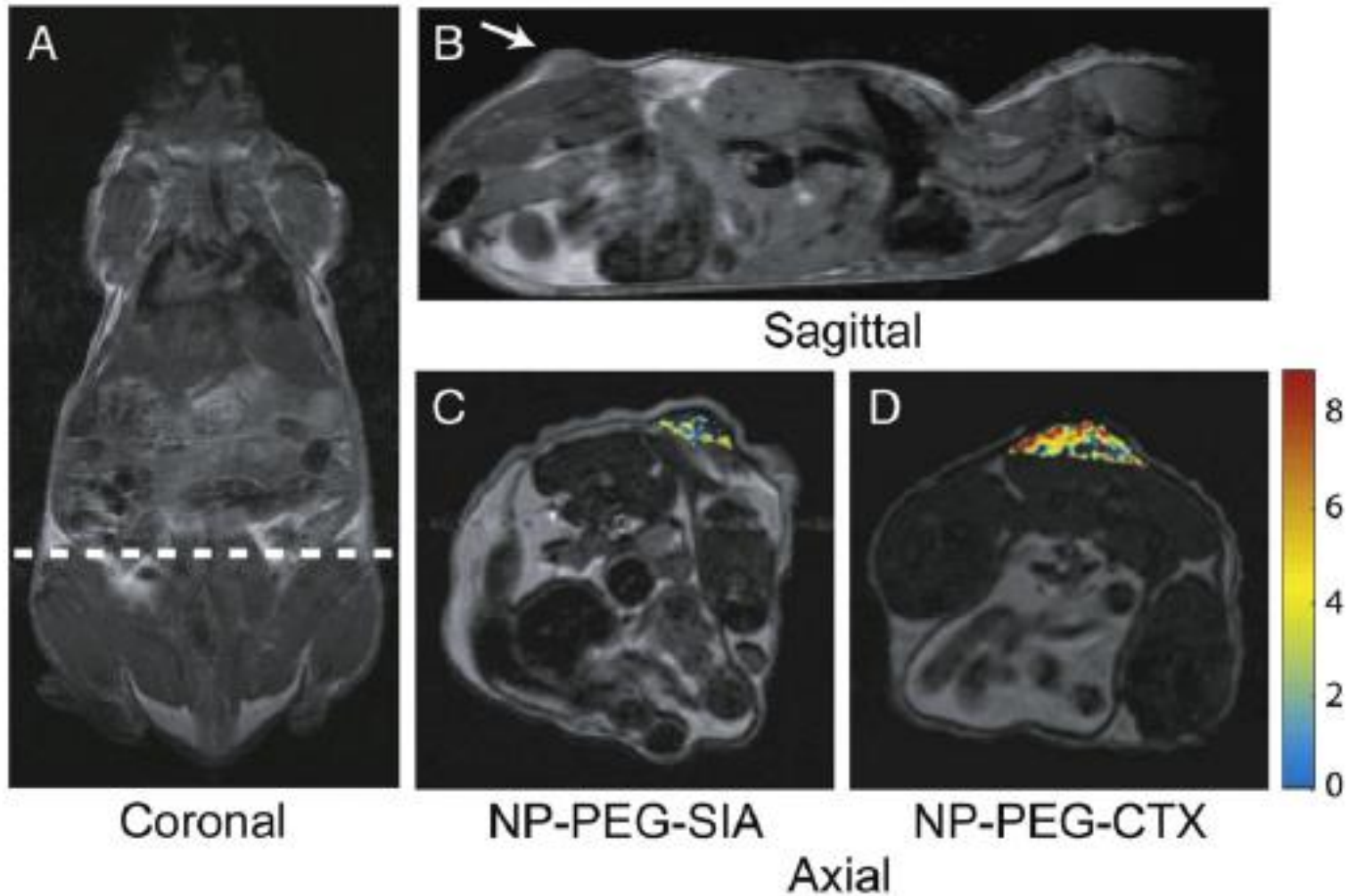


Ralph Weissleder

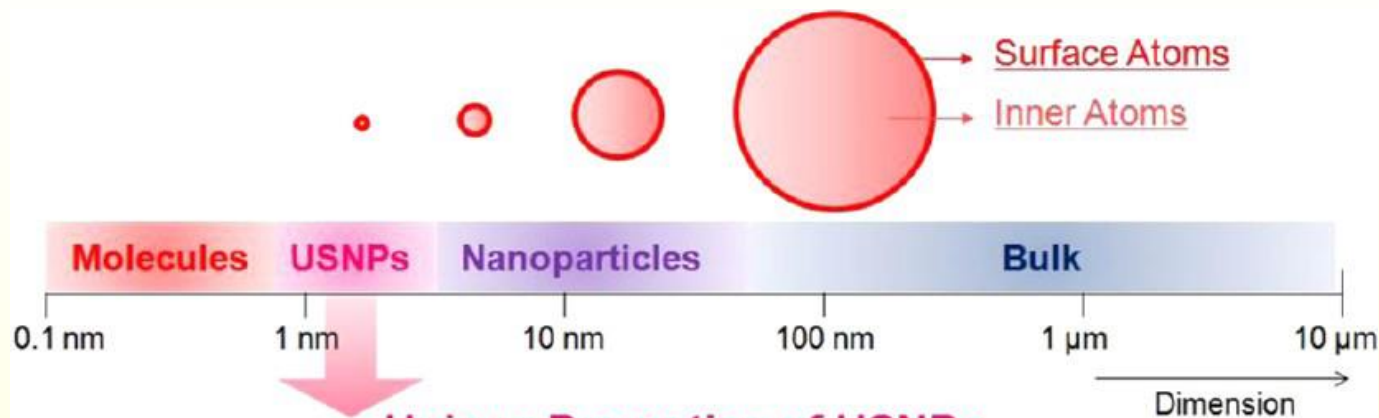
Basic Res Cardiol 103:122–130 (2008)

Contrast agents for NMR imaging

tumor



Contrast agents for NMR imaging



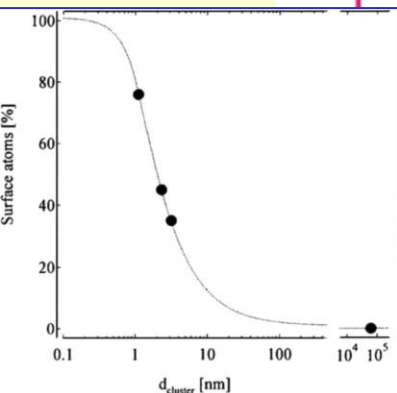
Unique Properties of USNPs

Extremely Small Volume

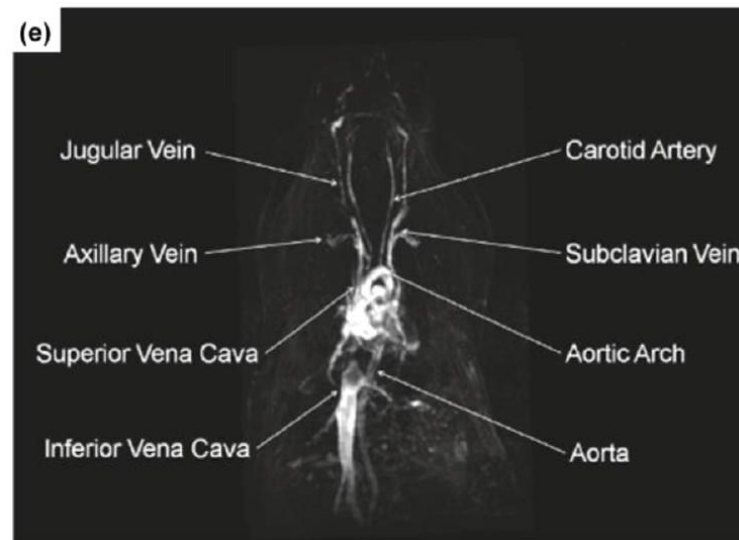
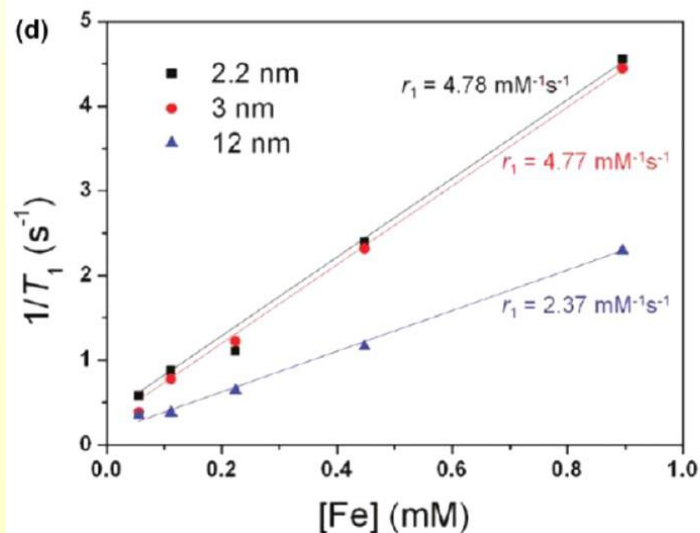
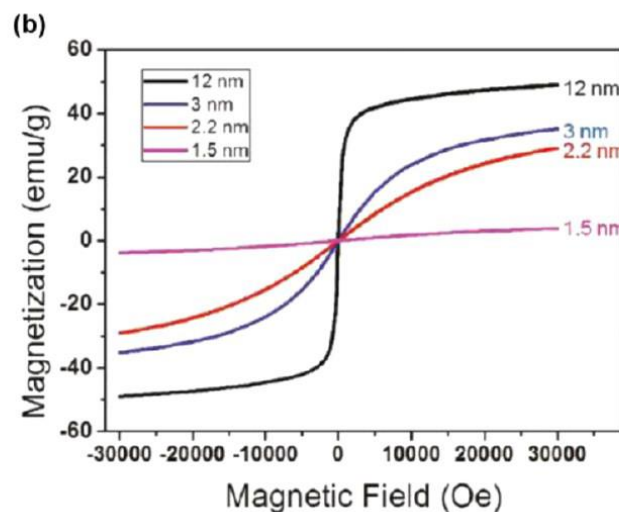
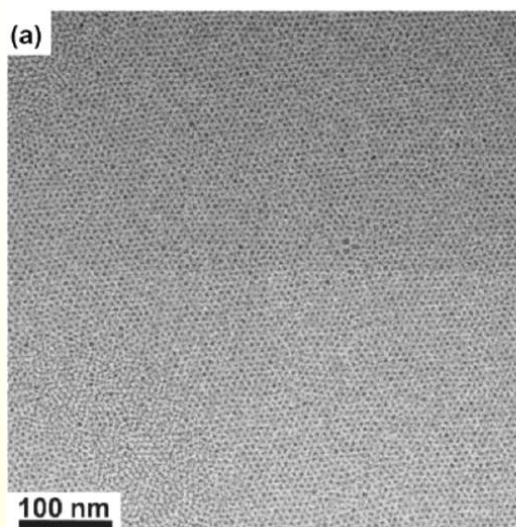
- Noble Metal USNPs
 - Fluorescence
 - Catalytic Activities
- Magnetic USNPs
 - Quantized Spin

Large Surface Area

- Noble Metal USNPs
 - Ferromagnetic
 - Catalytic Activities
- Magnetic USNPs
 - Nearly Paramagnetic
- Semiconductor USNPs
 - Pinned Emission



Contrast agents for NMR imaging



NMR imaging

Table 1. Imaging techniques and related contrast agents.

Imaging technology	Contrast agents	Spatial resolution	Toxicity	Sensitivity	Time Resolution
X-ray CT	Iodinated contrast material	sub-mm	Nephrotoxic	mM	1–2 s
MRI	Gadolinium-based	sub-mm	Nephrogenic systemic fibrosis	mM for Gd-based nM for Fe-based	1–2 s
PET/SPECT	Radioactively labelled agents	mm	Dosimetric exposure	pM	min

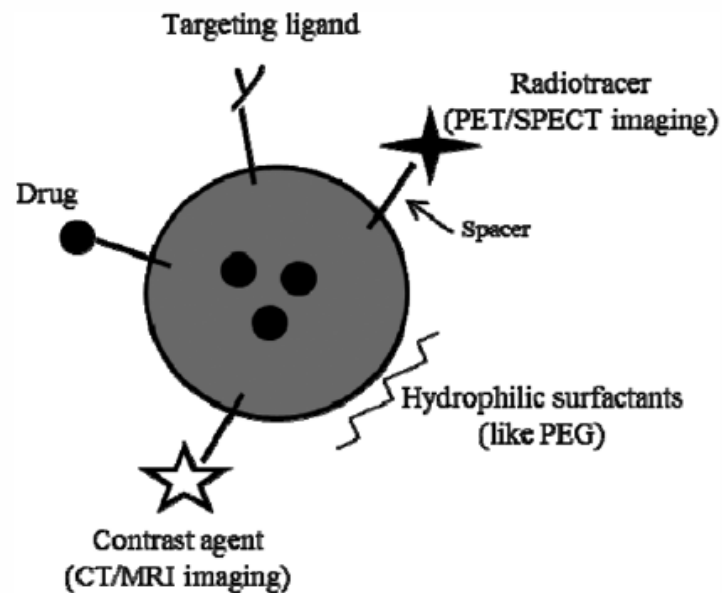


Figure 2. Multi-functionalized NPs. Graphical representation of multifunctional NP for molecular imaging (functionalized with contrast agents for CT/MRI, with radiotracer for PET/SPECT), for drug delivery (functionalized with drug molecules incorporated within the core of NP or conjugated to the surface), for specific targeting (functionalized with specific ligands) and for stealth (hydrophilic surfactants). Spacer/linker molecules are also indicated.

Biomedical applications

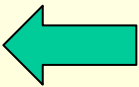
• In vitro → Diagnostic → **Separation/selection**

• In vivo → Diagnostic → **NMR imaging**

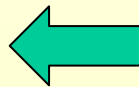
• In vivo

Therapeutic

Drug targeting



Hyperphermia



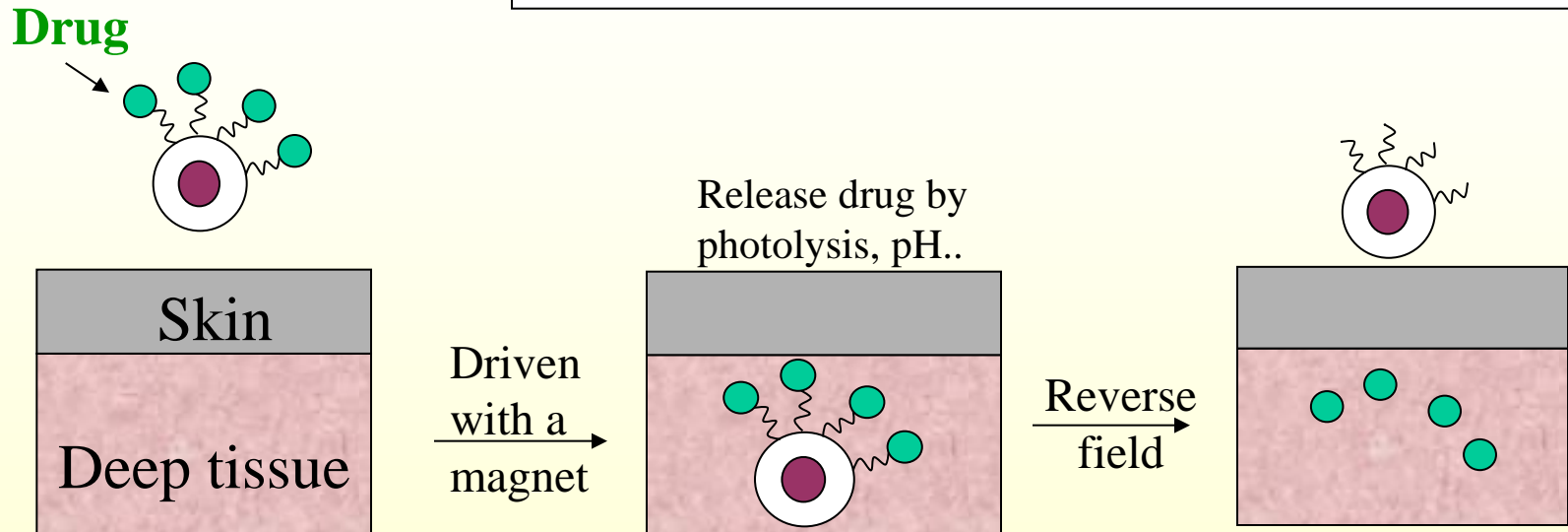
Gene delivery

Tissue regeneration (cell labelling)

Biomedical applications

DRUG DELIVERY

Targeting of a drug immobilised on magnetic nanoparticles under the action of an external magnetic field.



- **Specific** -> Reducing side effects
- **High local concentration** -> Reducing the dosage
- **Problem** -> Field strength

→ Human preliminary test

Cytokine **IFN- γ**

Cancer immunotherapy : Activating immune response to removal primary tumor and prevent metastases.

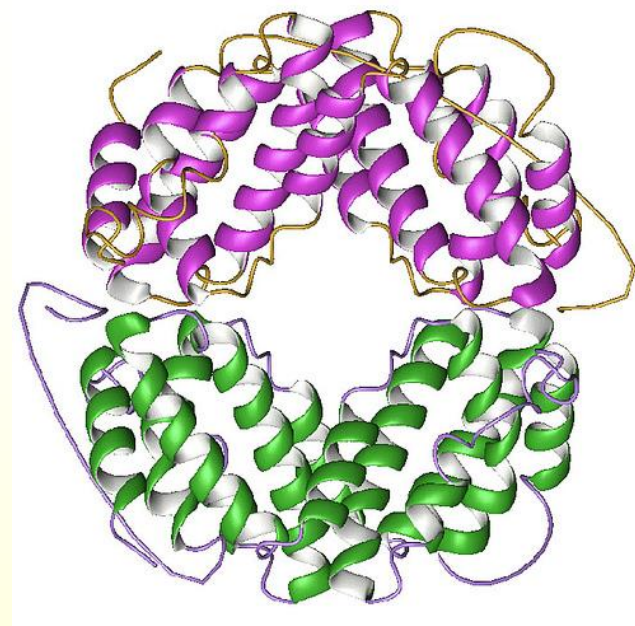
Cytokine: small protein produced by macrophages and T lymphocytes

Activity:

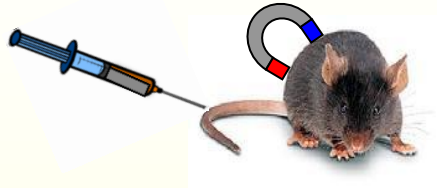
- Activate macrophages production
- Induce cancer cell apoptosis

IFN- γ the most effective cytokine in tumor elimination

Magnetic nanoparticles: Controlled local release of cytokines



Drug delivery



Inyección subcutánea de
 $2,5 \times 10^6$ células Pan02

Días: -7

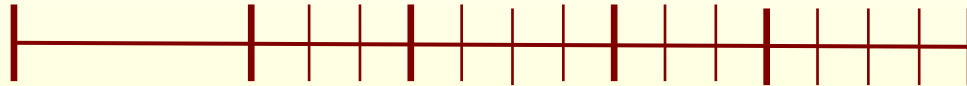
0

3

7

10

14



Eutanasia y extracción de tumores:

Tamaño

Presencia de nanopartículas

Niveles de IFN- γ

Inmunohistoquímica

PBS (Control) + campo magnético externo

DMSA-NP (300 μg Fe) + campo magnético externo

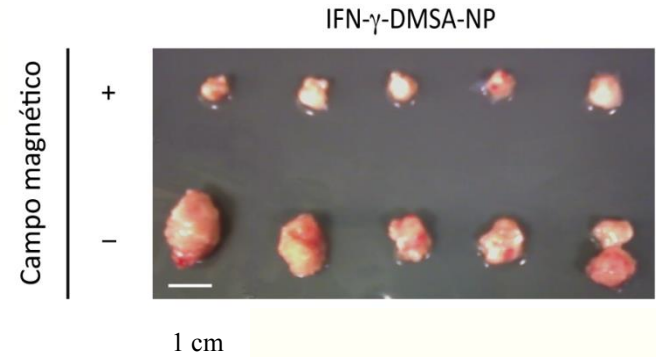
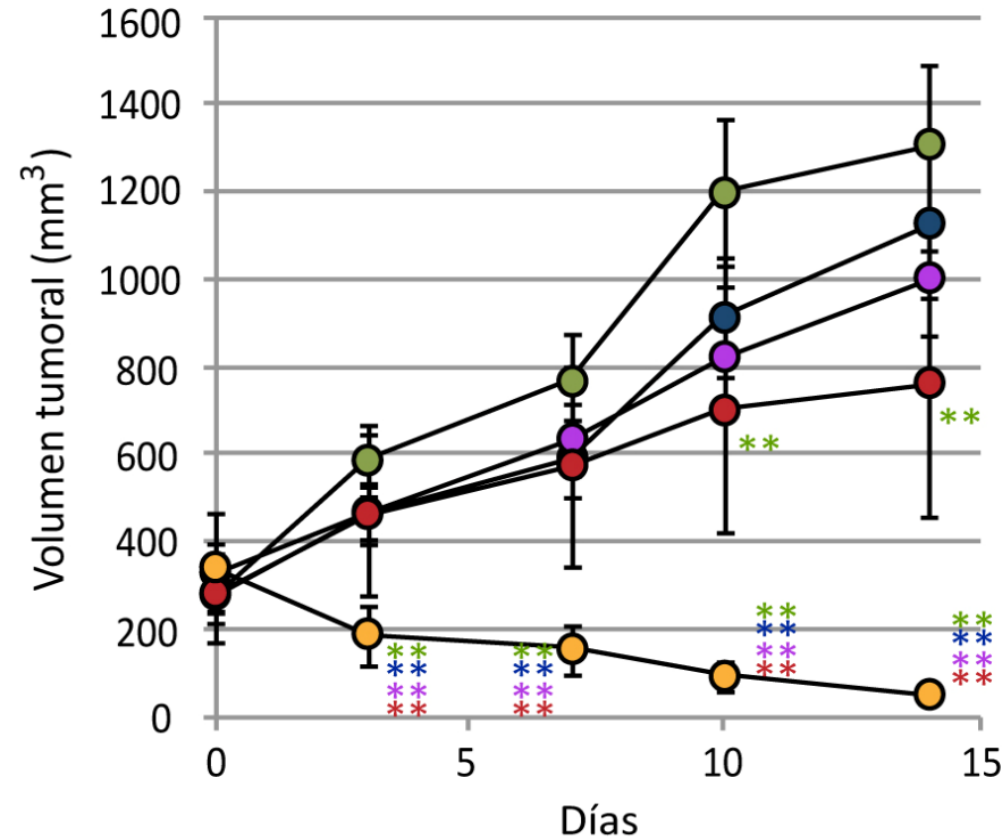
IFN- γ (10000 UI) + campo magnético externo

IFN- γ -DMSA-NP (300 μg Fe + 10000 UI) + campo magnético externo

IFN- γ -DMSA-NP (300 μg Fe + 10000 UI)

(0,4 T; 1 h)

Tumor size



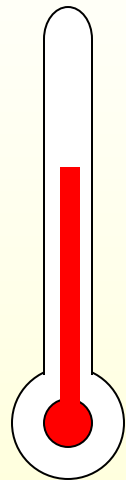
- PBS
- DMSA-NP
- IFN- γ
- IFN- γ -DMSA-NP
- IFN- γ -DMSA-NP + campo magnético

Also for induced tumours
with 3-methylcholanthrene (MCA)

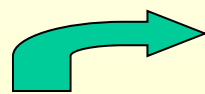
Biomedical applications

HYPERTHERMIA

Heating of a target tissue to the temperatures between 42-43 °C

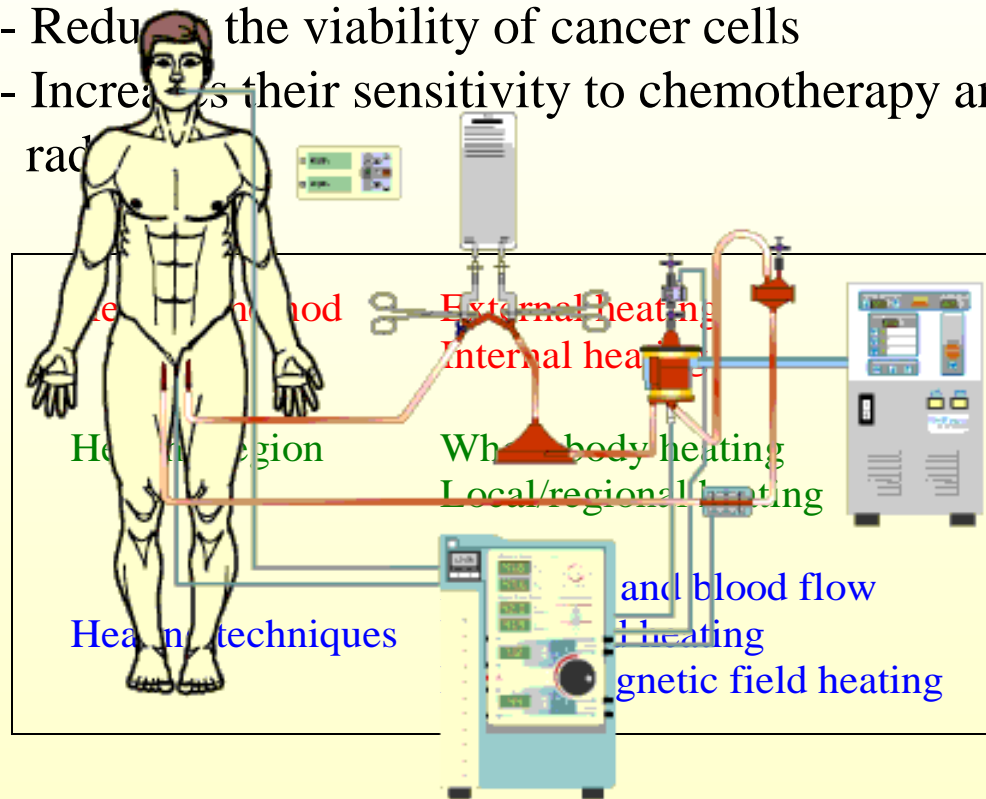


42-43°C



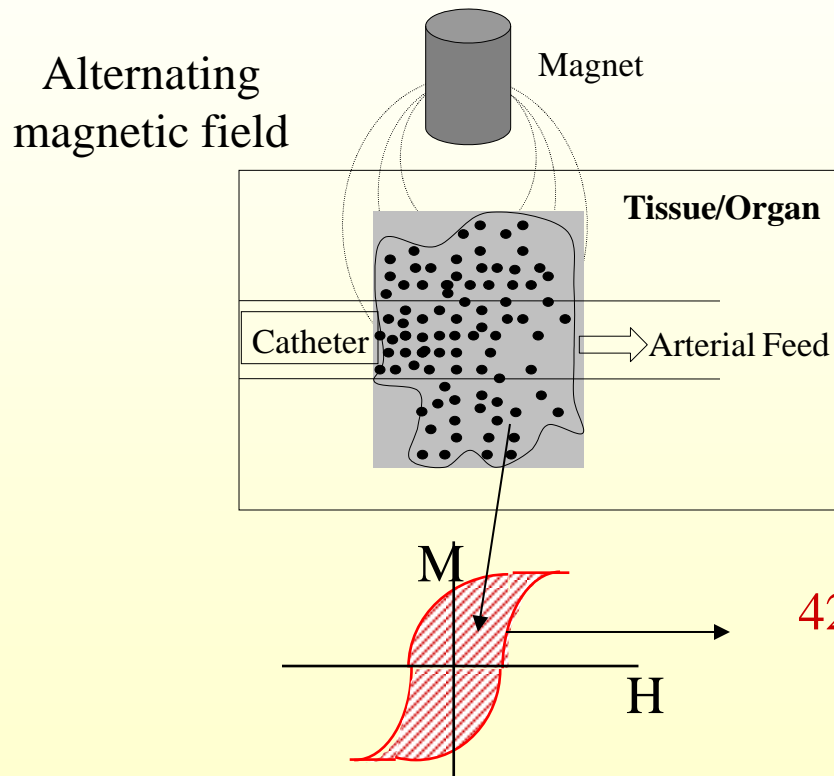
Conventional
Hyperthermia

- Reduces the viability of cancer cells
- Increases their sensitivity to chemotherapy and radiation



Biomedical applications

HYPERTHERMIA



Advantages of using magnetic nanoparticles

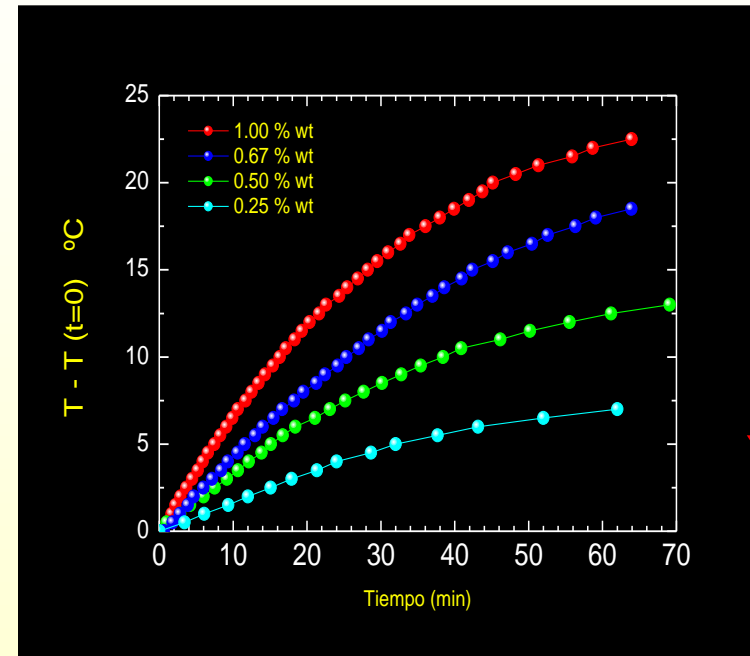
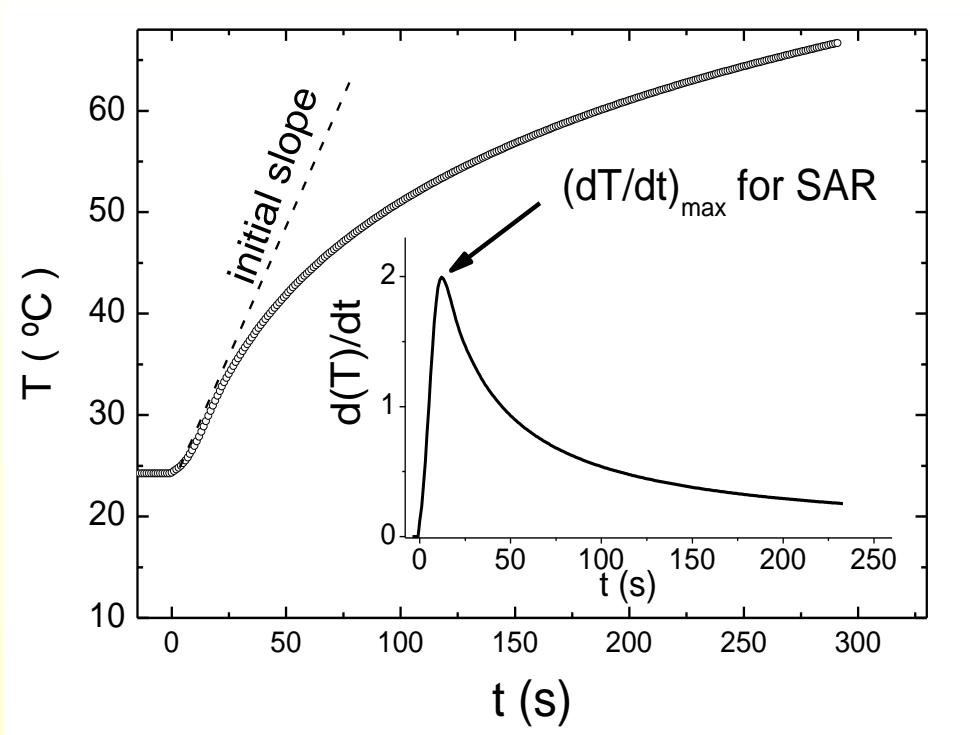
- Avoid heating healthy tissues
- Combining other therapies
Targeting radionuclides

42°C / 30 min → Cancer is destroyed

Goya et al, Current Nanoscience 2008, 4, 1-16

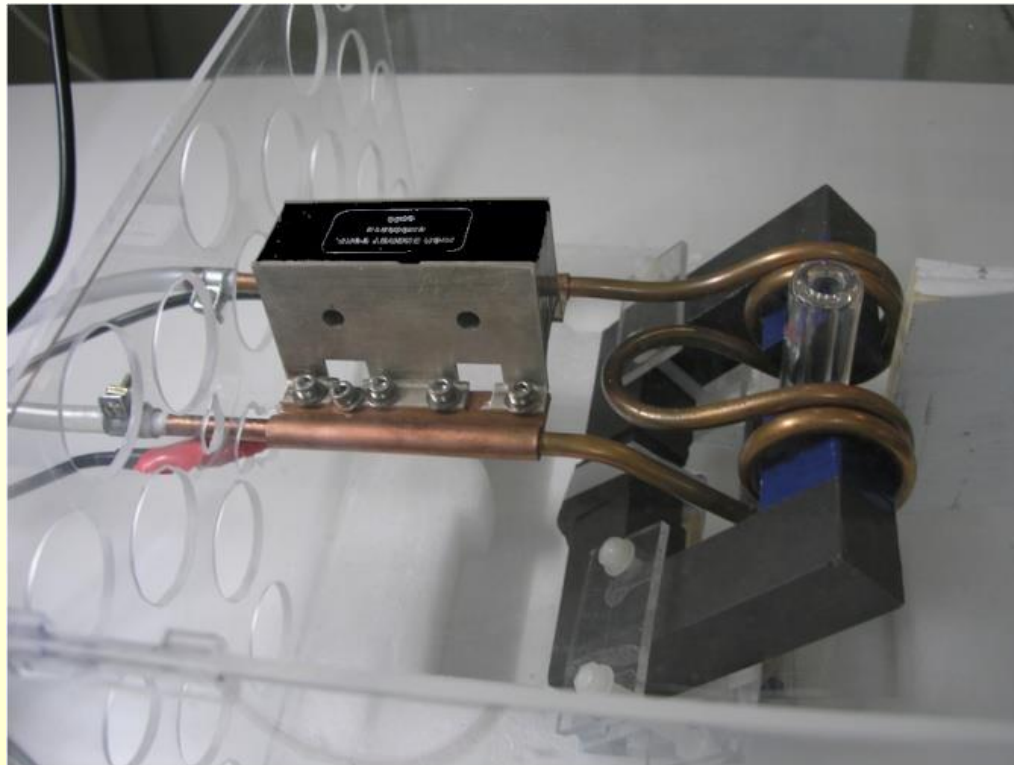
Nearly complete regression of tumors via collective behavior of magnetic nanoparticles in hyperthermia, C L Dennis et al., Nanotechnology 20 (2009)

WHAT WE ACTUALLY MEASURE...



Magnetite nanoparticles 30 nm in diameter

SAR = Specific Absorption Rate = Specific loss power
= Power absorbed by unit mass of the magnetic material



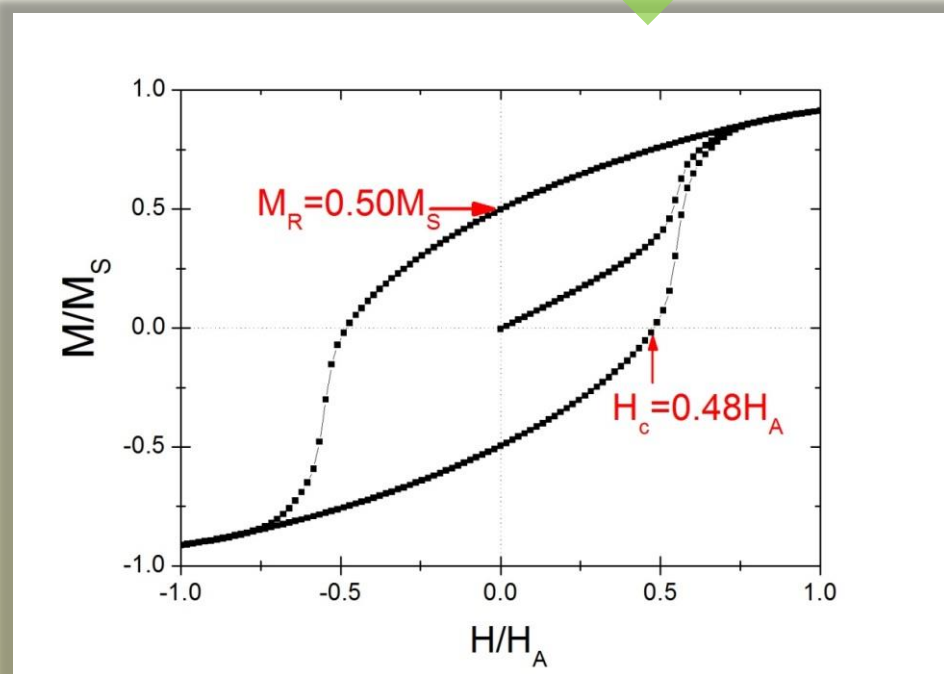
$$SAR = C_m \phi (\Delta T / \Delta t)$$

C_m = specific heat capacity of the sample

$$\phi = m_{ff} / m_{ox}$$

Field Amplitude = 10 kA/m
Frequency = 249 kHz

- Magnetic particles under an AC field will rise T
- Heat dissipated → area M(H) curve: Hysteresis Losses (HL)



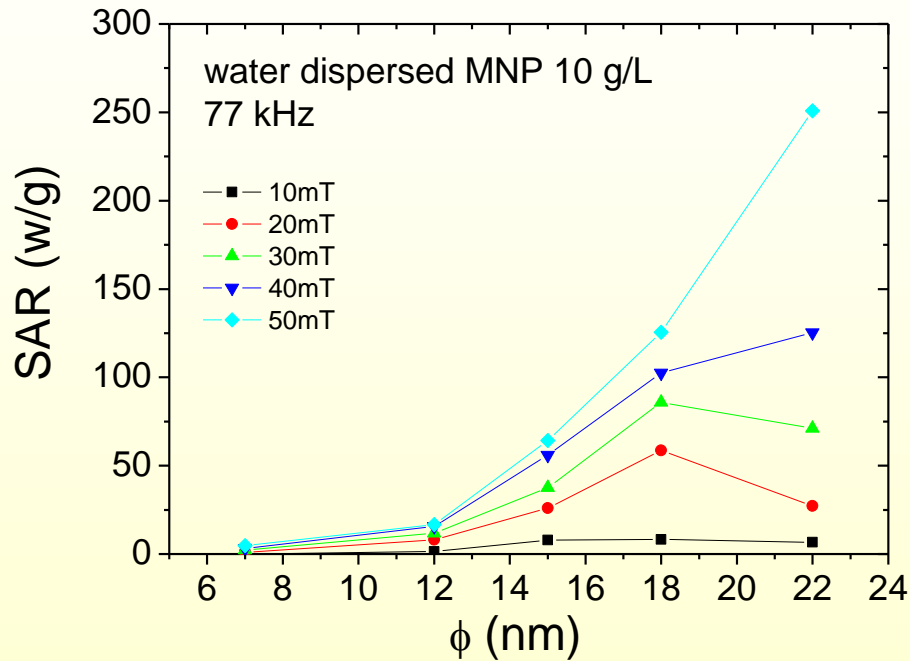
Serantes et al.

**Specific Absorption Rate
(SAR)**

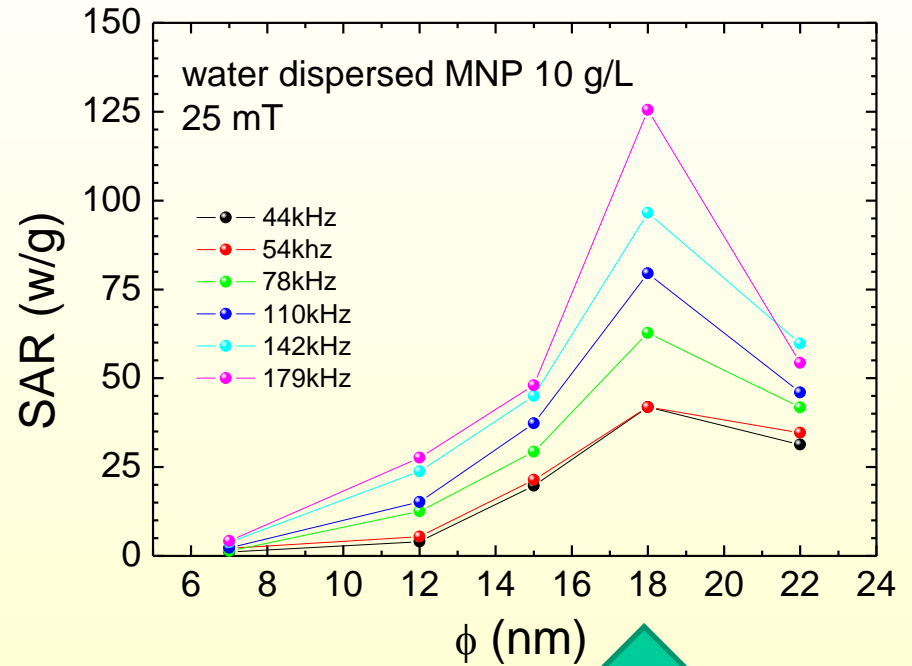
Heat can kill
the tumour!

EFFECT OF THE PARTICLE SIZE

Heating efficiency



Specific Absorption Rate (SAR)



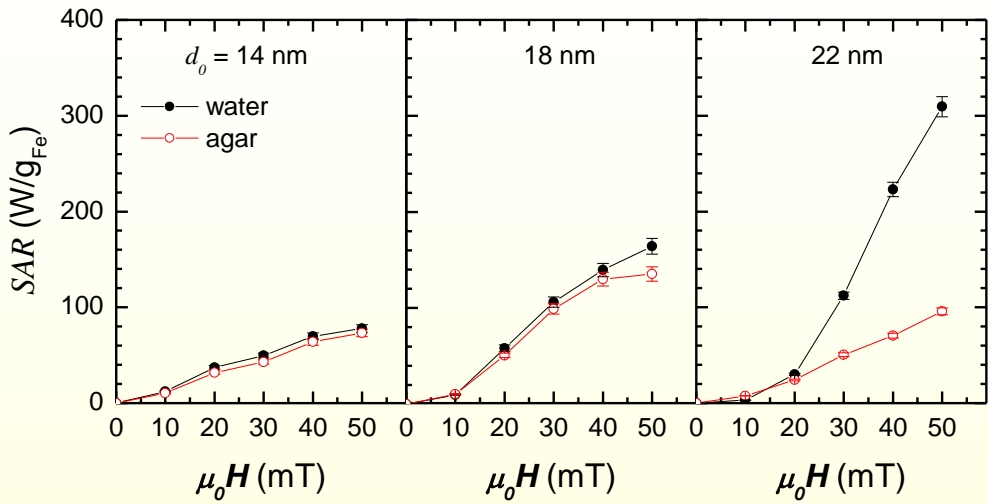
100 W/g, 250 Oe, 100 kHz

IMDEA Nanoscience (Madrid)



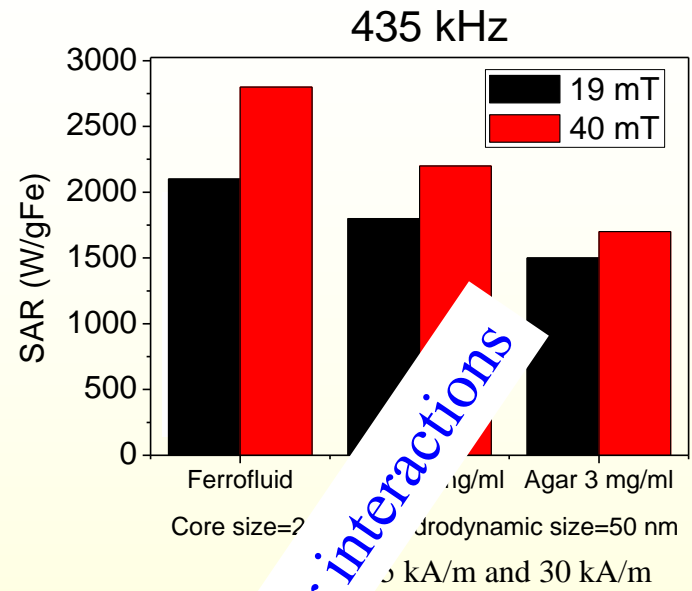
EFFECT OF THE MEDIA VISCOSITY

VISCOSITY



Frequency (77 kHz).

CONCENTRATION



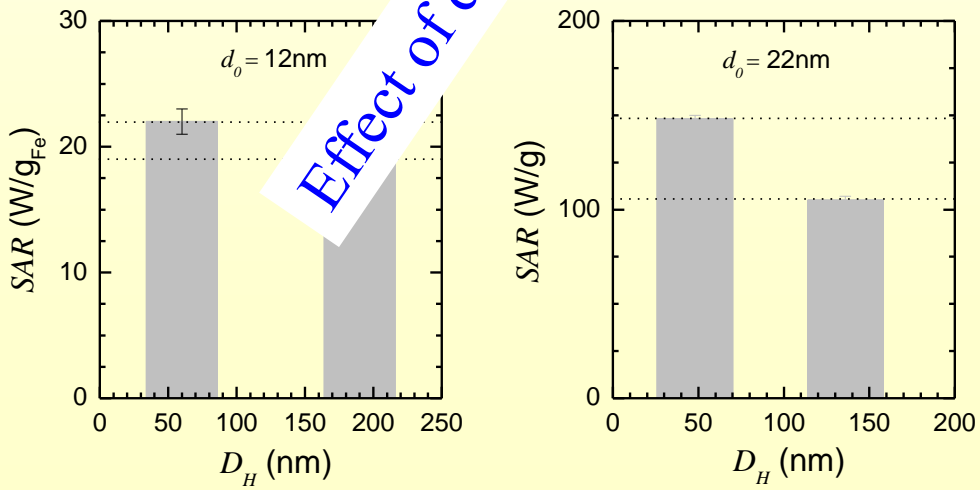
Effect of dipolar interactions

Physical rotation for sizes over 18 nm

IMDEA Nanoscience (Madrid), INSA (Toulouse) and UHJ (Jena)

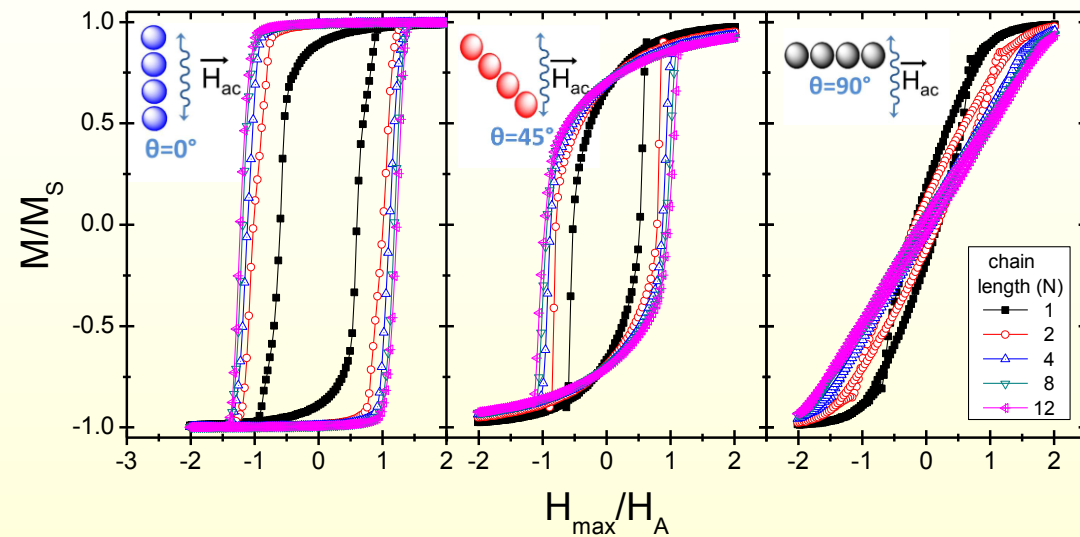
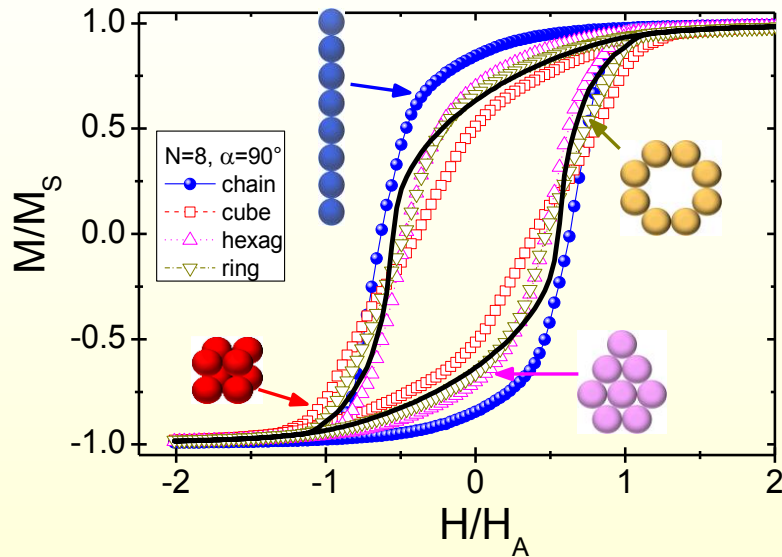
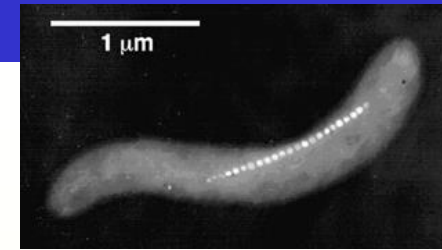


DELEGATION



NANOPARTICLE ASSEMBLING

David Serantes, I. Conde-Leborán, D. Baldomir, K. Simeonidis, M. Angelakeris, Ò. Iglesias, O. Chubykalo-Fesenkoa and C. Martínez-Boubeta

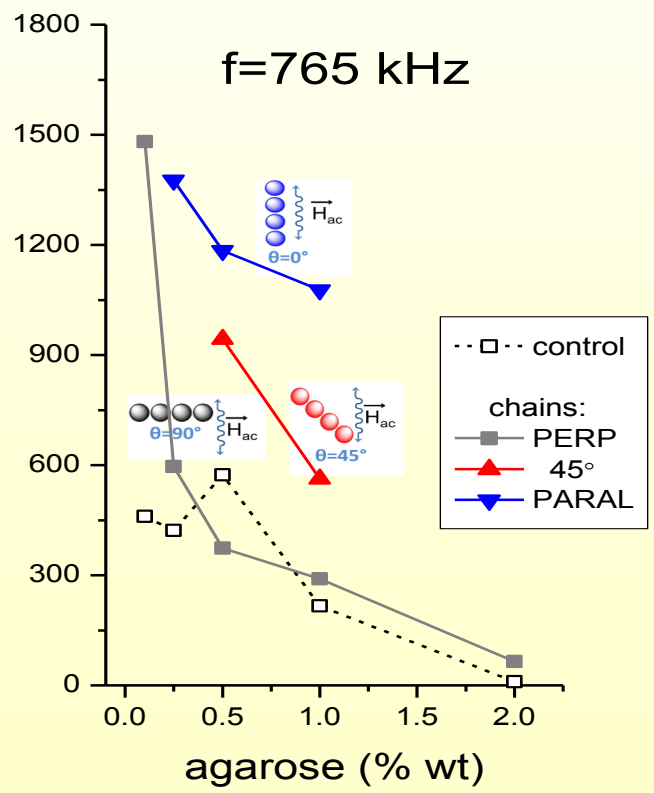
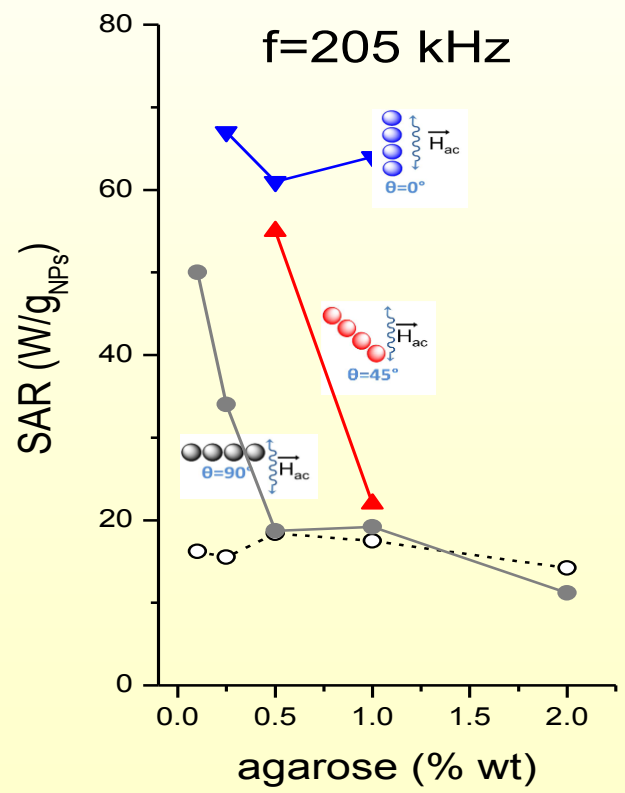
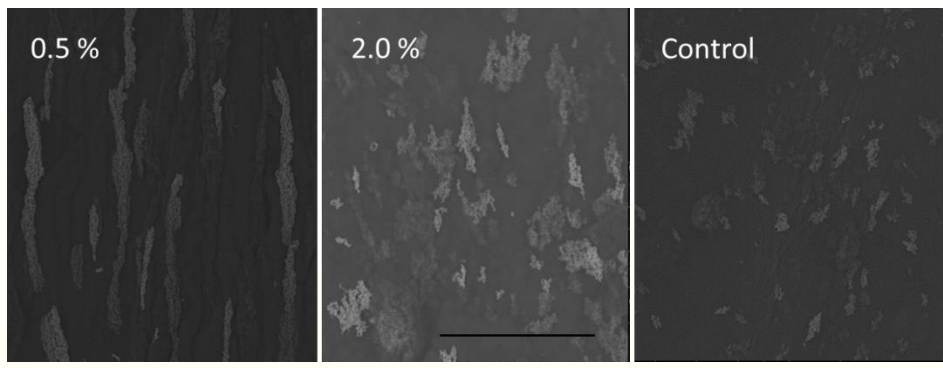
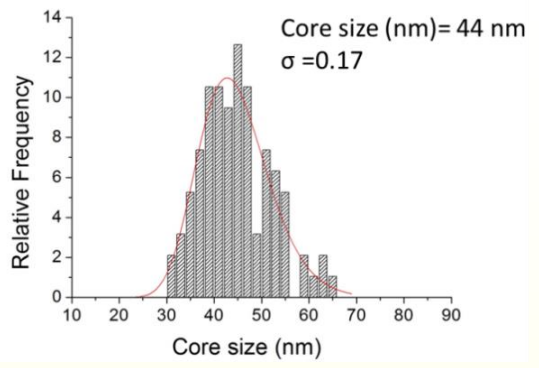
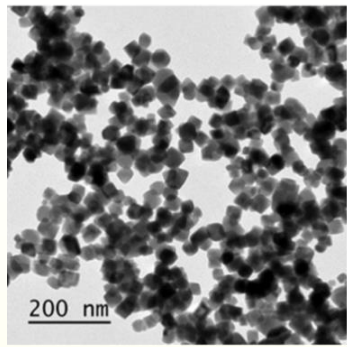


➤ The highest area $M(H)$ curve is attained for chain-like shape

➤ Dependence of area $M(H)$ curve on chain length and orientation

➤ What happens in real situations, with variable viscosity conditions?

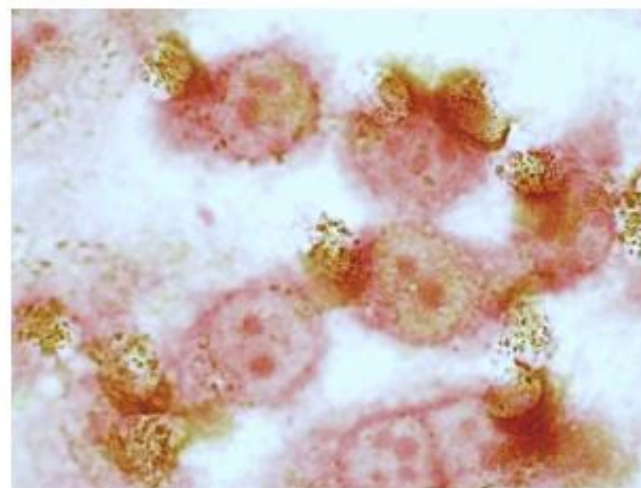
NANOPARTICLE ASSEMBLING



✓ chaining allows to reduce the dosage of NPs for hyperthermia treatment.

Nanopartículas ferromagnéticas recubiertas de dextrano aminado (cargadas positivamente) DX 0.5 mg/mL 3h de incubación + campo magnético 100 kHz 150 Gauss durante 30 min. Las células se mantuvieron en el incubador y se procesaron 24h después del tratamiento. Tinción con rojo neutro y Hoechst.

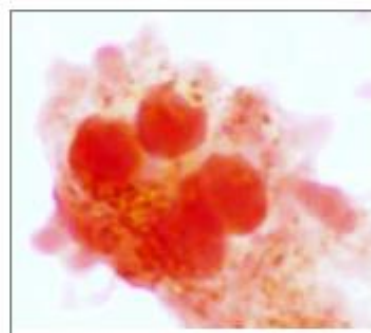
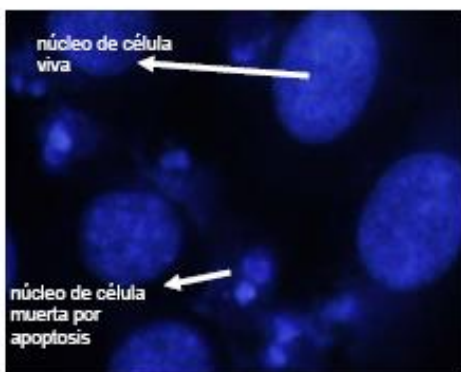
Dx (catiónico)



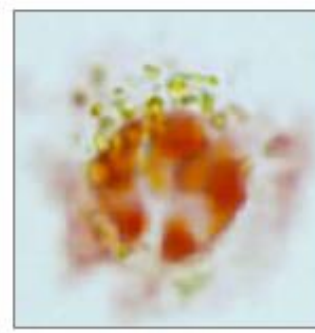
Resultados:

Un % significativo de las células han muerto por apoptosis y se observa: disminución del tamaño celular, redondeamiento y el núcleo condensado y fragmentado.

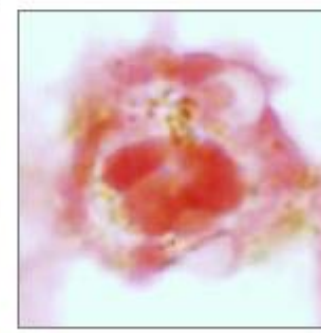
Las células contienen en su interior nanopartículas (color amarillo-marrón)



Apoptosis



Apoptosis



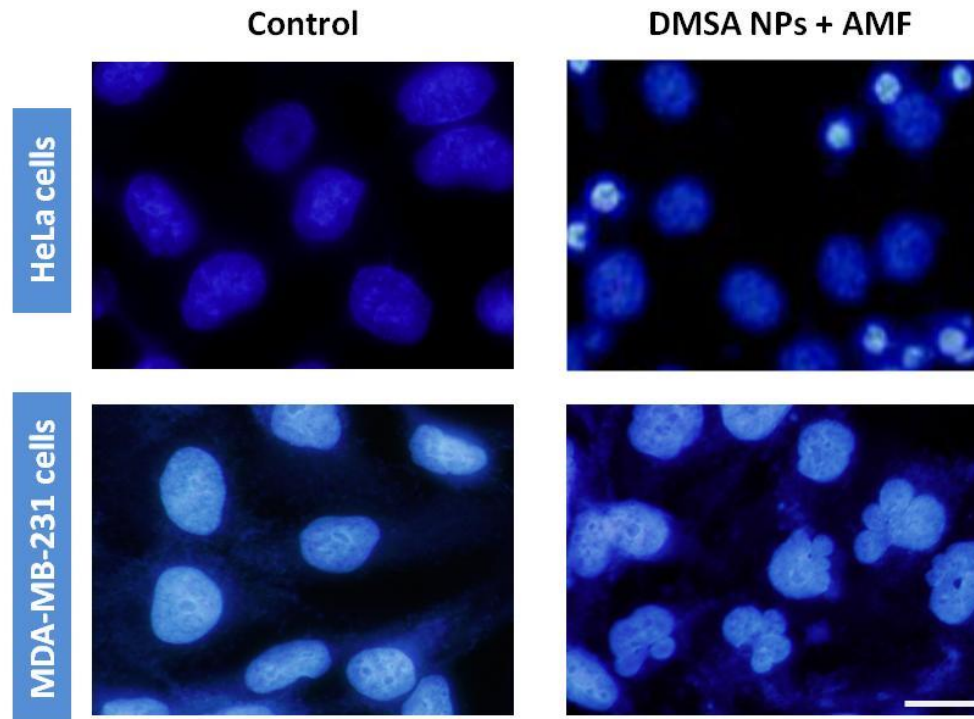
Apoptosis

Hyperthermia: DMSA coated particles

UAM-IMDEA

HeLa and MDA-MB-231 cells (stained with Hoechst 33258) were incubated with DMSA coated NPs, and exposed to an AC magnetic field (AMF).

24 h after the treatment apoptotic cells (HeLa) and giant and multinucleated cells (MDA-MB-231) were observed.



DMSA (anionic)

AMF conditions: 161 kHz, 210 G, 15 min exposure (HeLa cells),
225 kHz, 150 G, 45 minutes exposure (MDA-MB-231 cells).

Hyperthermia

Table 3. Summary of nanoparticle features favoring MRI and/or magnetic hyperthermia applications.

MRI (contrast)	Nanoparticle feature	Magnetic hyperthermia (heating)
+	High magnetization (size and surface coating)	+
+	SPIO	-
+	USPIO	-
+/-	Large size (core diameter >10 nm)	+
+	Sequestration by MPS	-
-	Long plasma half-life (targeting)	+
+	Short plasma half-life (targeting)	-

+: Favoring feature/parameter; -: Disfavoring feature/parameter; MPS: Monocyte phagocyte system; SPIO: Superparamagnetic iron oxide; USPIO: Ultrasmall superparamagnetic iron oxide.

Ingrid Hilger et al., Nanomedicine 2012

<http://www.magforce.de/en>

http://www.youtube.com/watch?v=BZLmD3SOR_Y

<http://www.clinicaltrials.gov/ct2/show/study/NCT00003052>

<http://www.mhaus.org/>

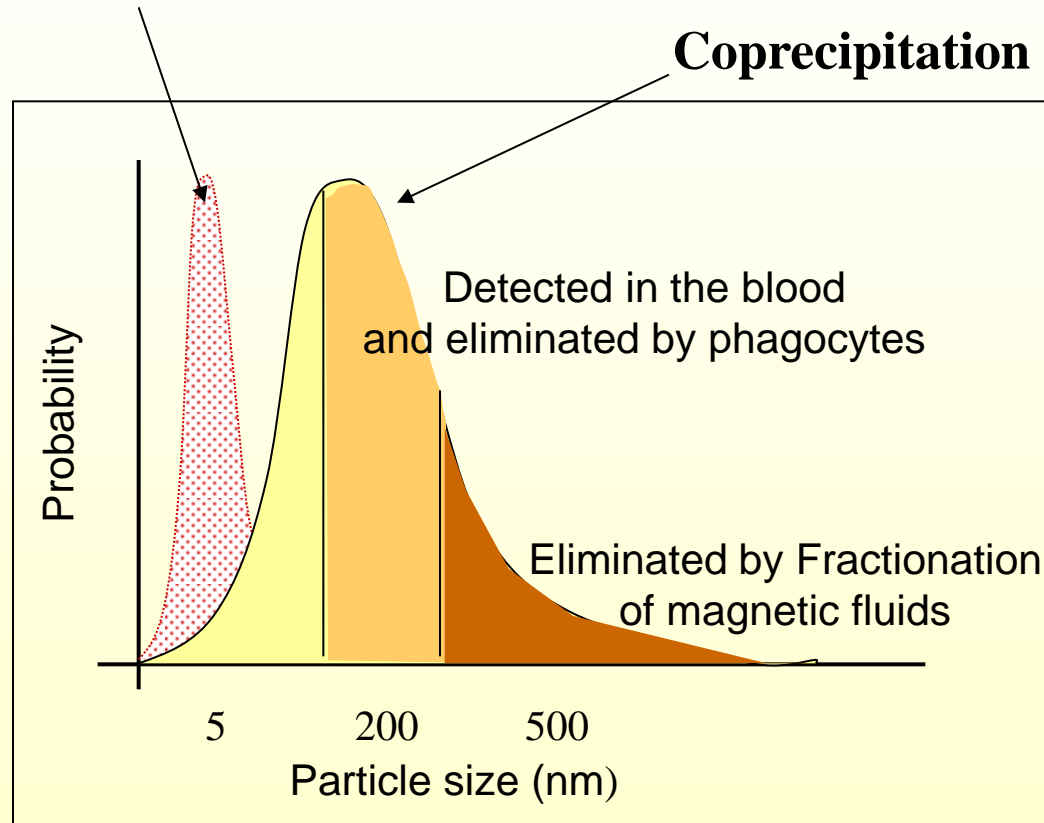
Preparation and Biomedical Applications of Magnetic Nanoparticles

Summary

- 1- What are magnetic nanoparticles?
 - 2- Requirements for biomedical applications
 - 3- Basic principles in magnetism
 - 4- Biomedical applications
 - in vitro
 - in vivo
-
- 5- Synthesis routes
 - in solution
 - aerosol
 - 6-Example

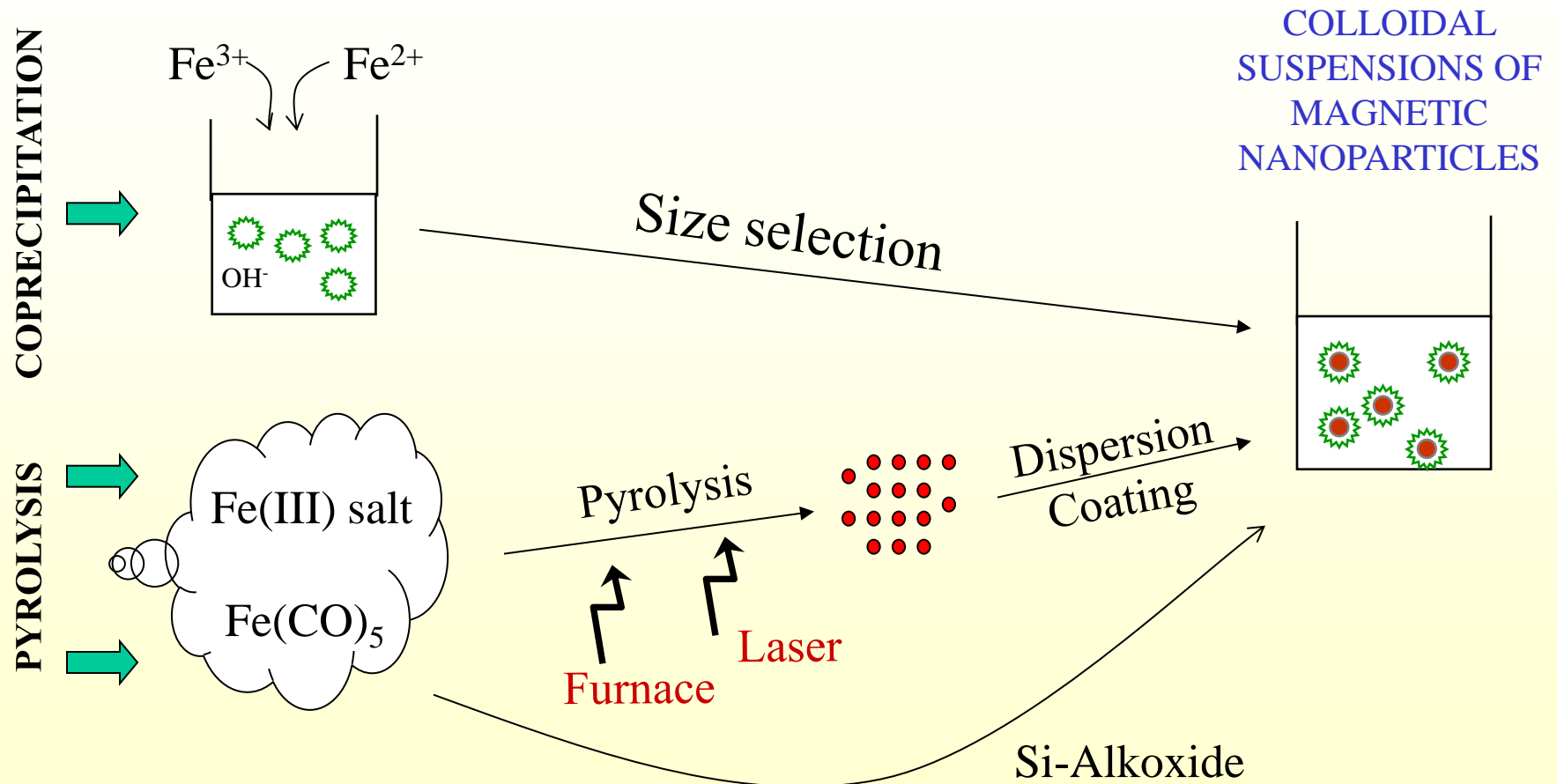
Synthesis of magnetic nanoparticles

UNIFORM NANOPARTICLES

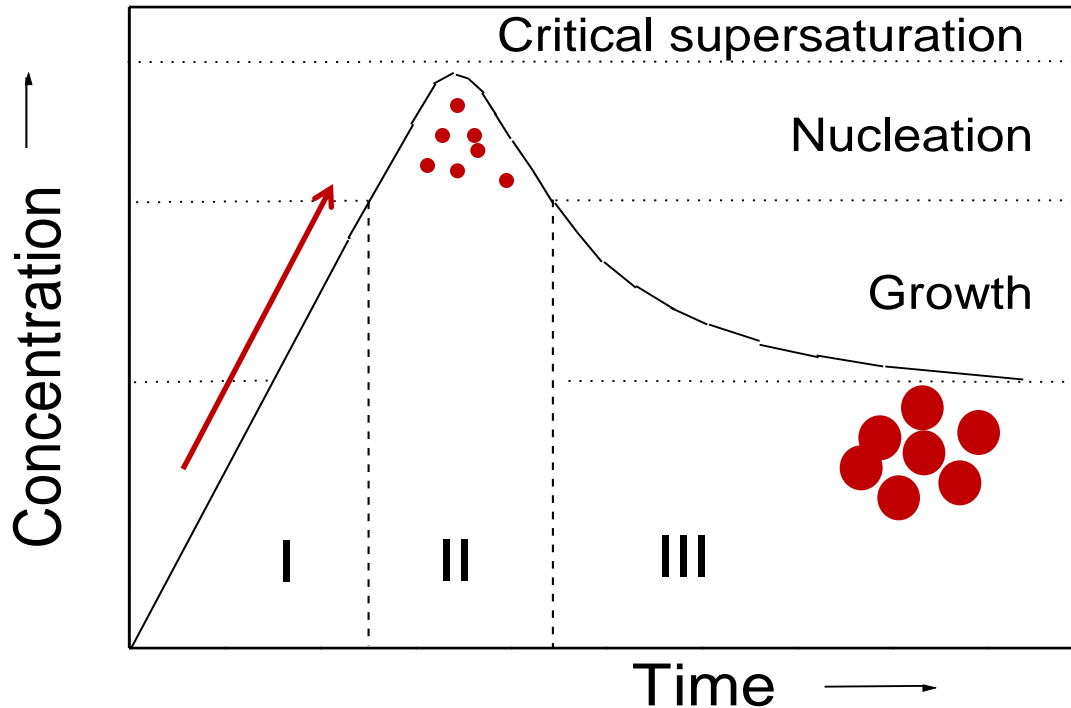


In the case of contrast agents prepared by coprecipitation, upon application, only a small number of particles contribute to the desired magnetic effect.

Synthesis of magnetic nanoparticles



Synthesis of magnetic nanoparticles



Modelo Clásico
LaMer and Dinegar

NUCLEATION

Ions/Complexes

Clusters

Nuclei (8-10 Å)

Homogeneous phase

GROWTH

Diffusion growth

Nanosized primary particles

Surfactant

Stable nanosystems

Diffusion growth

Large crystalline particles

Coagulation

Large polycrystalline particles or crystalline

Synthesis of magnetic nanoparticles

TABLE 2.1 Summary Comparison of the Synthetic Methods.

Synthesis Method	Reaction Time	Solvent	Surface-Capping Agent	Sizes	Size Distribution	Shape Control	Yield
Coprecipitation	Minutes	Water	No	2–15	Broad	Not good	Medium
Thermal decomposition	Hours–days	Organic compound	Yes	4–30	Very narrow	Very good	Medium
Polyol process	Hours	Polyglycol	Yes	5–150	Narrow–broad	Good	Medium
Microemulsion	Hours	Organic compound	Yes	5–50	Narrow	Good	Low
Spray pyrolysis	Seconds	Water and volatile solvents	No	2–10	Broad	Not good	High
Laser pyrolysis	Milliseconds	Gases	No	2–10	Very narrow	Good	High

Synthesis and Characterization of Nanoparticles: Synthesis of Inorganic Nanoparticles,

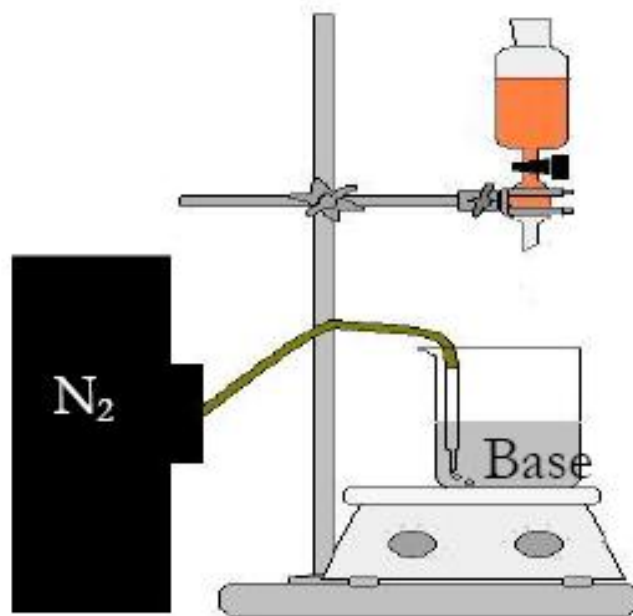
Gorka Salas, Rocio Costo and María del Puerto Morales
Part I, Vol. 4 Nanobiotechnology, Inorganic Nanoparticles
vs Organic Nanoparticles edited by J.M. de la Fuente and
V. Grazu, 2012 Elsevier Ltd, FRONTIERS OF
NANOSCIENCE, Series, Editor: R. E. Palmer, UK.

Synthesis by precipitation in water

Método convencional

Sal de Fe(II) y Fe(III)

$$\text{Fe}^{2+}/\text{Fe}^{3+} = 0.5$$

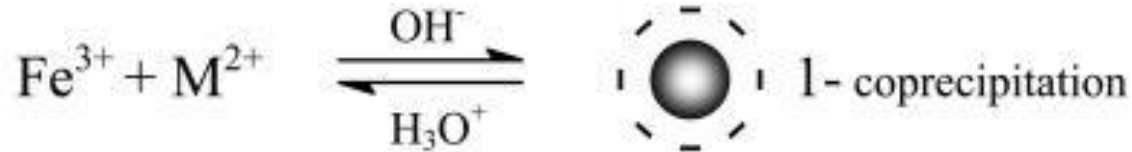


- Concentration
- Temperature
- Atmosphere
- Stirring

Fe_3O_4
(Magnetite)

Synthesis by precipitation in water

Coprecipitation



- Salt concentration
- Nature of M (Na, K, NH_4)
- Temperature

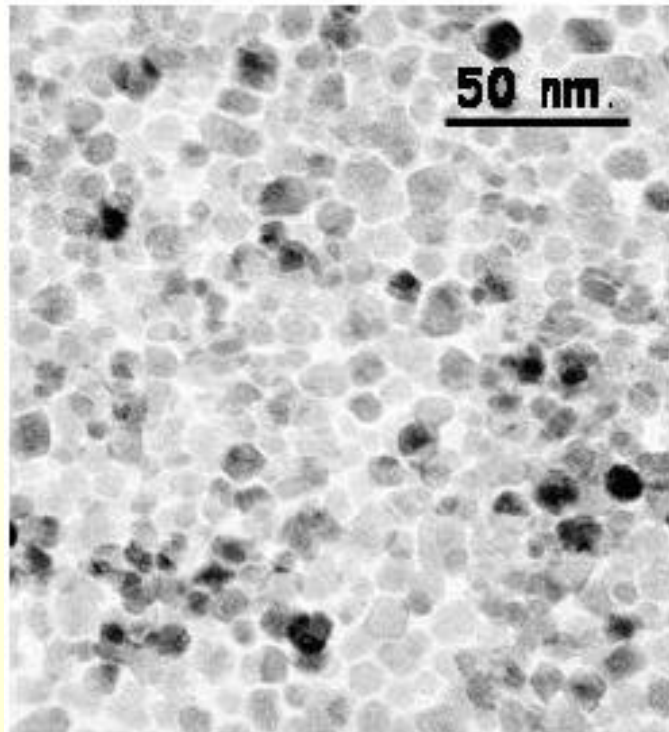


Ferrofluid (pH = 2; $I = 10^{-2}$ mol/L)

3- peptization

Synthesis by precipitation in water

Coprecipitation



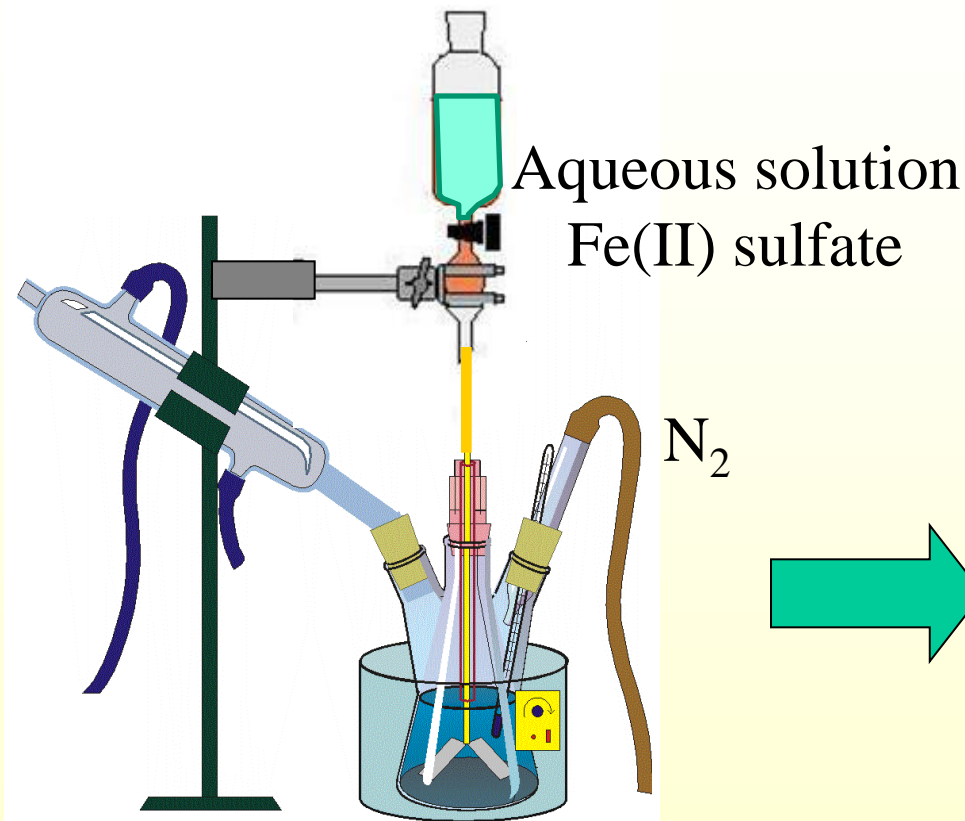
Fe_3O_4 Nanoparticles with sizes
between 2-12 nm

	KOH
	C1
Size XRD (nm)	8.4
Size TEM (nm)	9 ± 3.9
$M_{50\text{kOe}}$ (emu/g sample)	45
χ (emu/g sample · kOe)	52
Hex 5 K (Oe)	0
% C	0
% weight loss (TG)	3.5

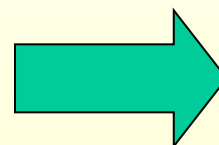
J. P. Jolivet, in Metal Oxide Chemistry and Synthesis: From Solutions to Solid State, Wiley, New York, 2000.

Synthesis by precipitation in water

Sal de Fe(II)



Aqueous solution
 $Na(OH) + KNO_3$



$90^{\circ}C \pm 0.1$
24 hours

Undisturbed system

Synthesis by precipitation in water

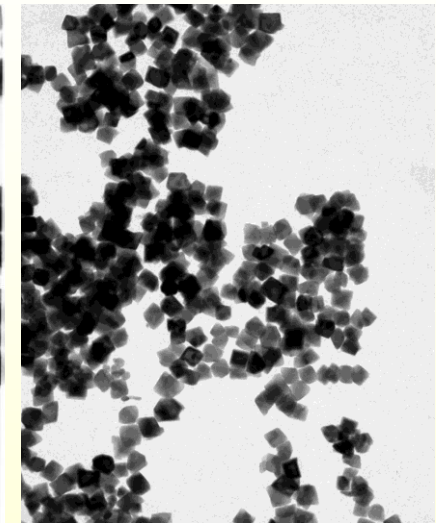
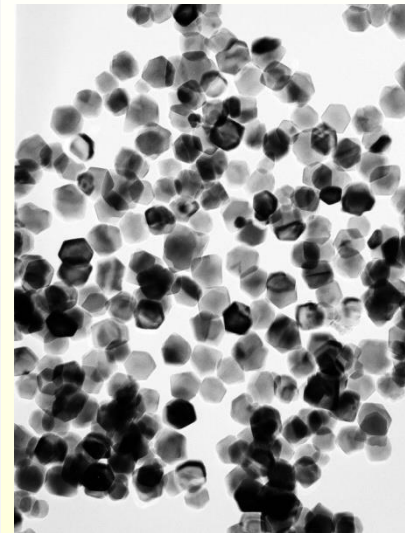
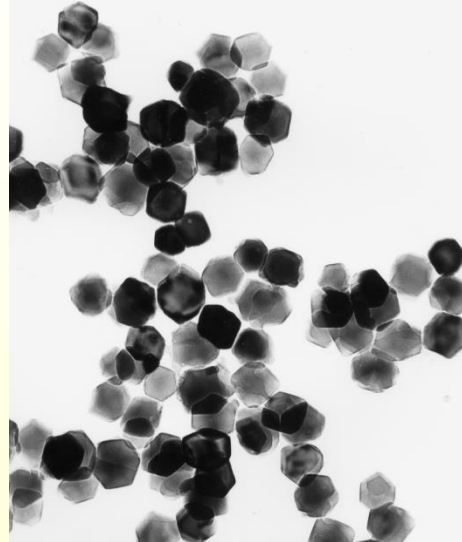
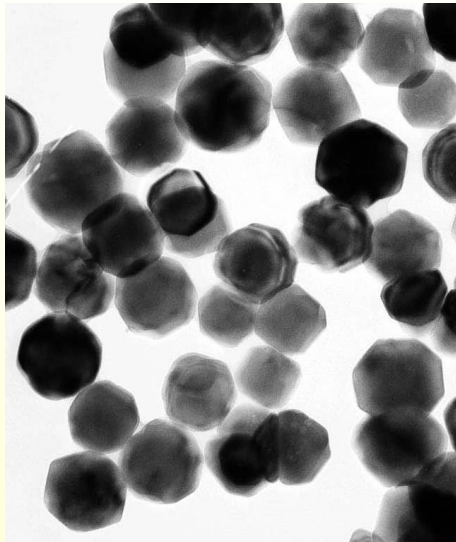
Oxidation control

150 nm

95 nm

70 nm

30 nm



200 nm

[Fe(II)] concentration decreases

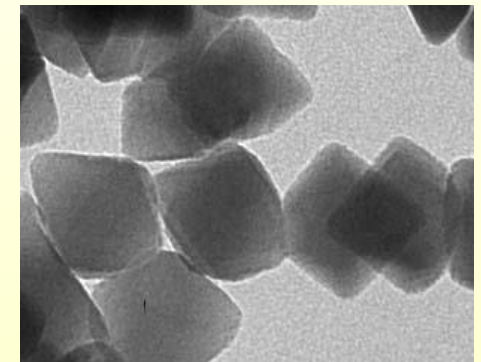
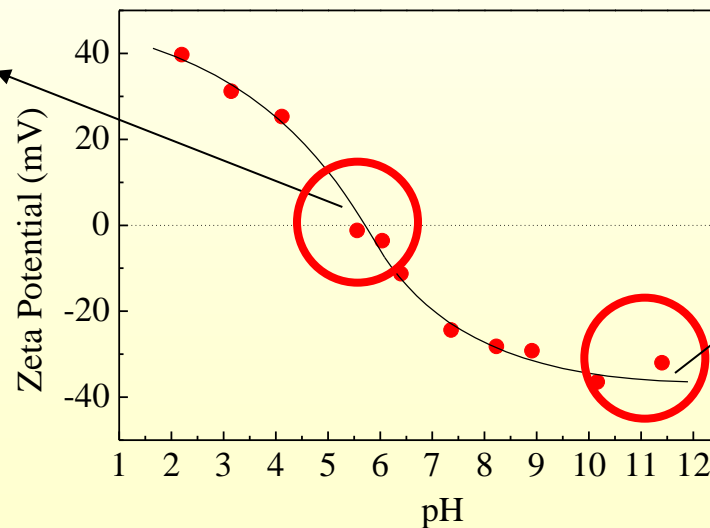
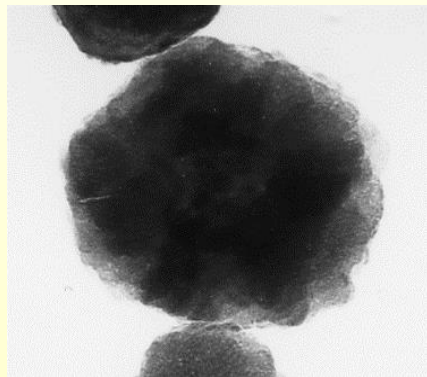
$[\text{OH}]_{\text{exc}}$ increases from 0.0002 M to 0.02 M

Particle size decreases from 300 nm to 30 nm

Synthesis by precipitation in water

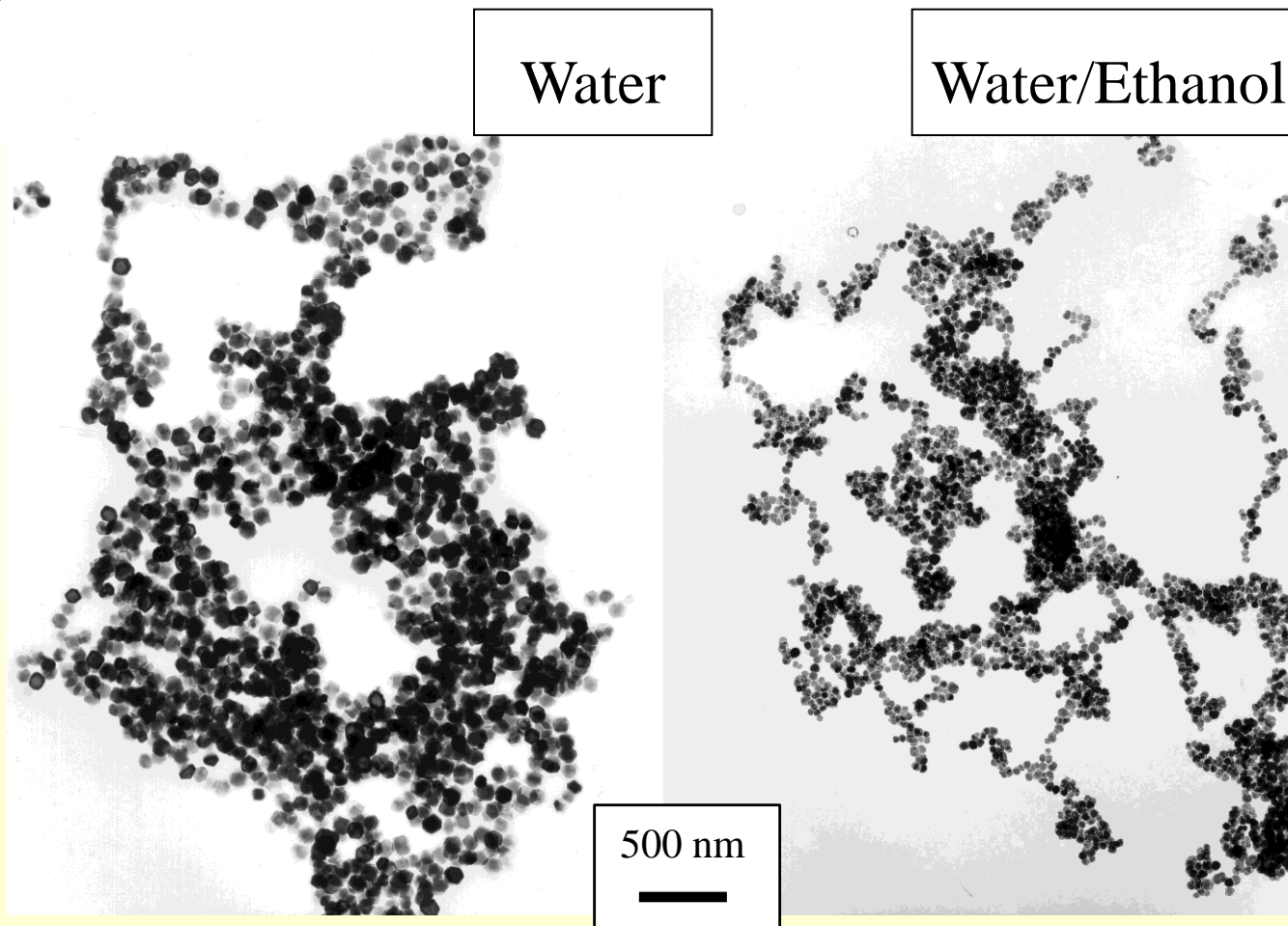
PARTICLE SHAPE

- At pH 6, electrostatic repulsion between the primary particles is small and coagulation of the very small primary particles would be expected to take place
- However, in excess of OH^- , particles are of cubic morphology with a well-defined habit, which suggests a direct crystal growth mechanism.



SURFACE CHARGE FOR MAGNETITE

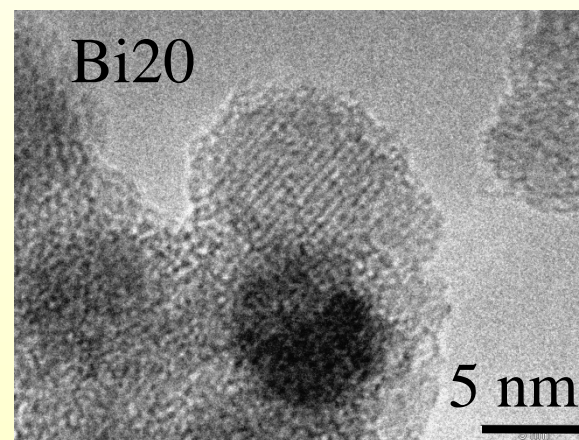
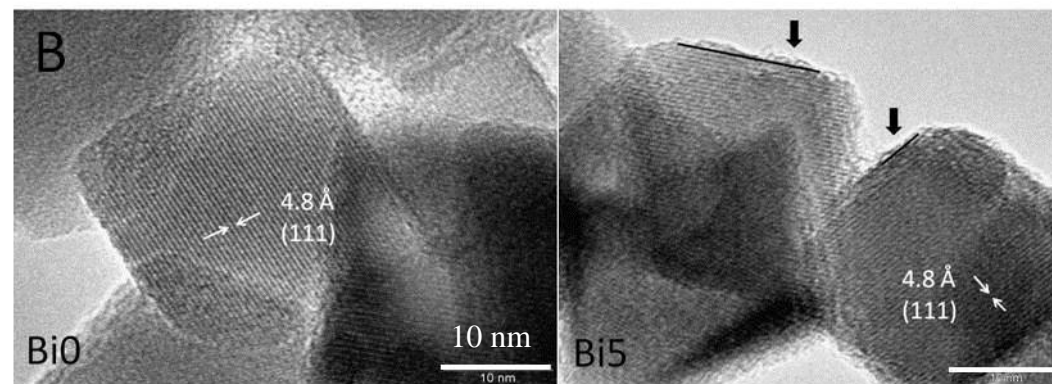
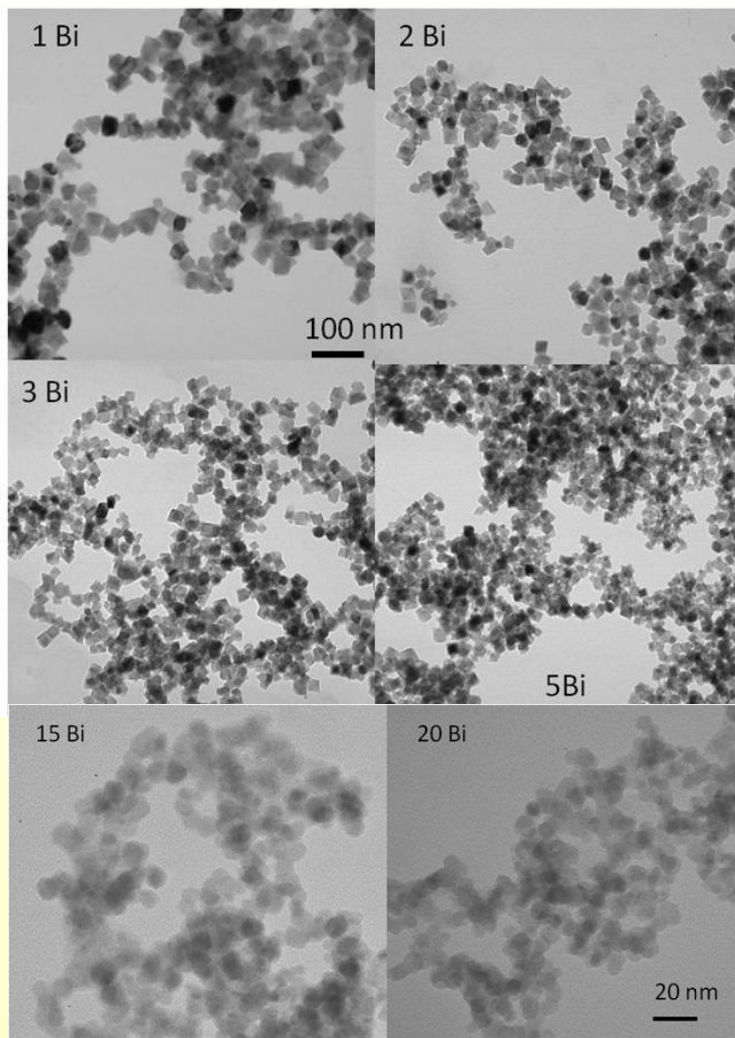
Synthesis by precipitation in water



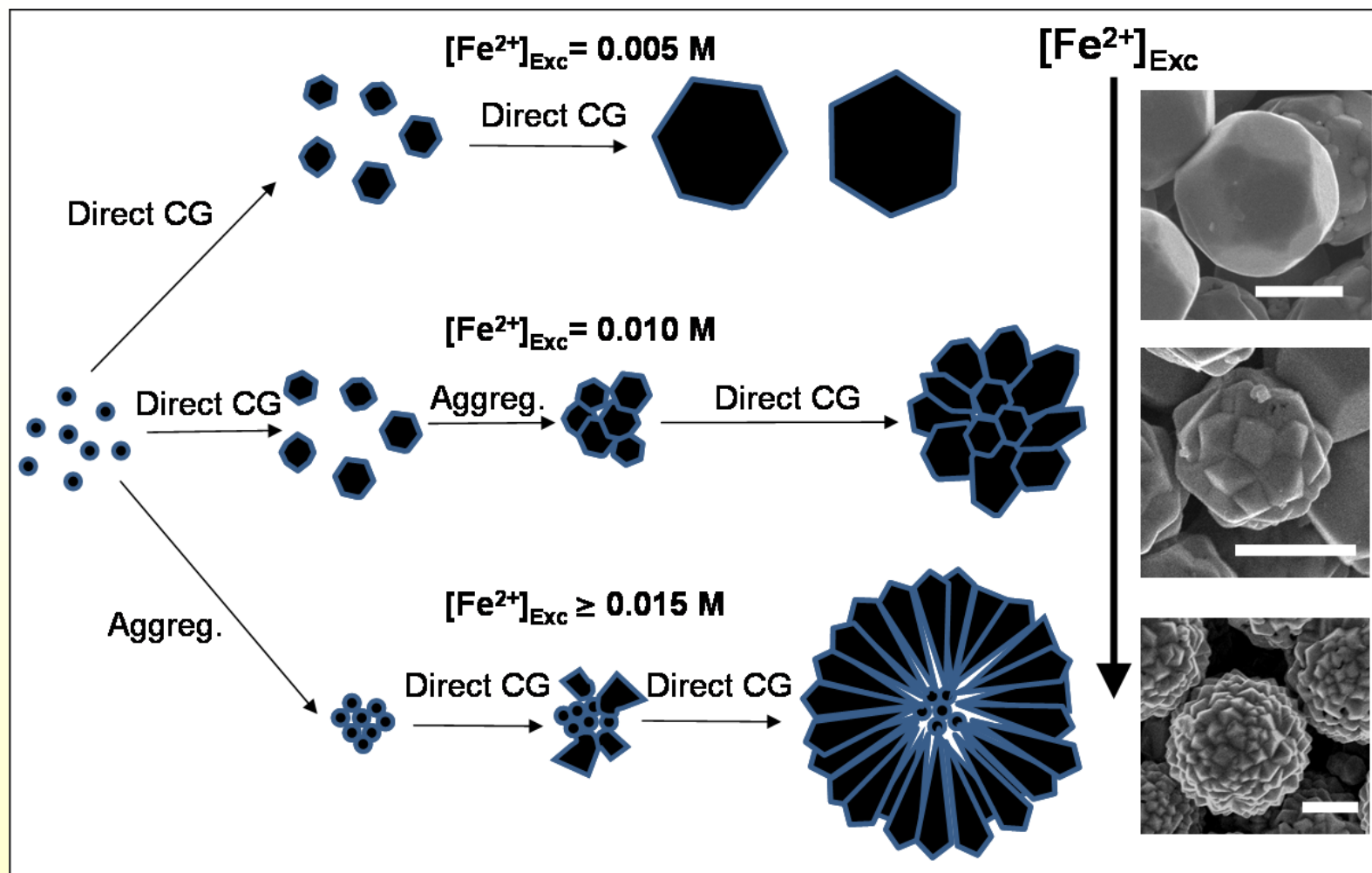
Introduction of ethanol in the media lead to a important reduction in particle size

Hyperthermia + Dual imaging agent (NMR + CT)

Core/Shell Magnetite/Bismuth Oxide Nanocrystals with Tunable Size, Colloidal, and Magnetic Properties

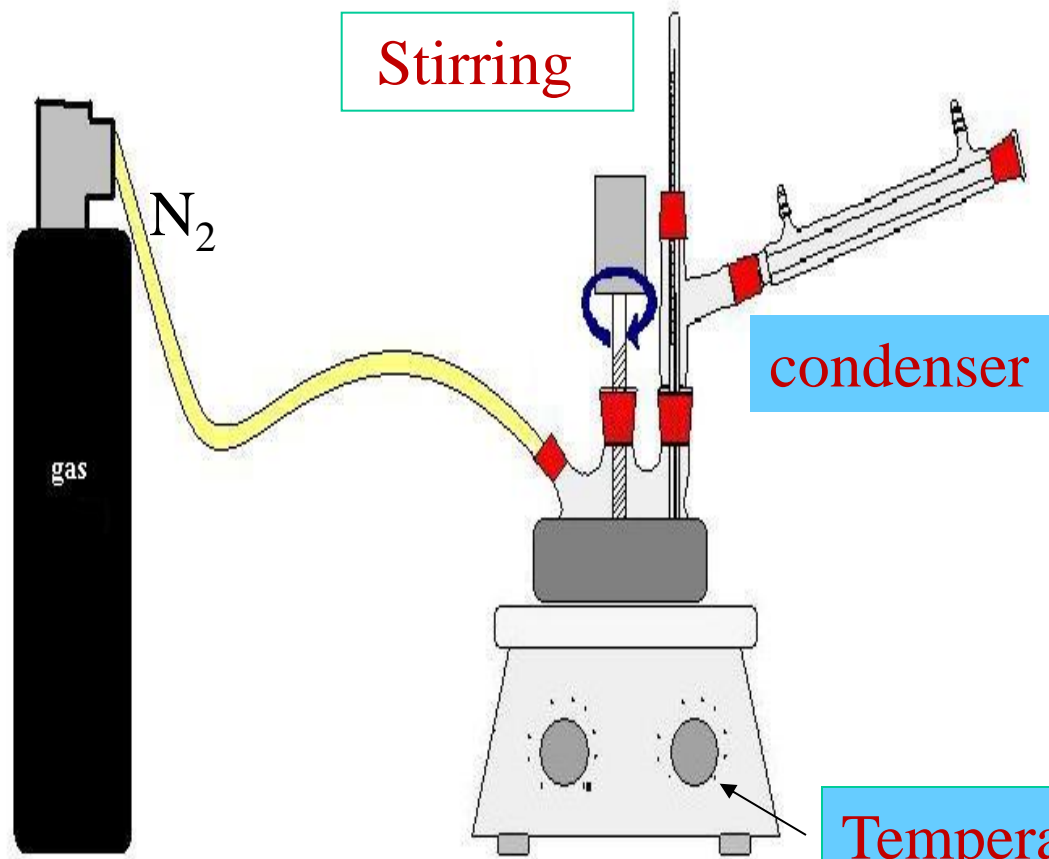


Synthesis by precipitation in water



Rodríguez-González, B.; Vereda, F.; de Vicente, J.; Hidalgo-Álvarez, R. *J. Phys. Chem. C* **2013**, 117, 5367

High temperature decomposition of organic precursors



Atmosphere control



Temperature control (200-400°C)

High temperature decomposition of organic precursors

Composition	Crystal structure	Diameter [nm]	Capping agent [a]
Fe	bcc	3.0–9.3	OA, LA, HA ₂ , HA _m
α -Co	fcc	3.5–17	OA, LA, TOP
Co	hcp	2.0–12	OA, TOP, TBP, TOPO
Ni	fcc	5.0–13	OA, TOA, TOPO
FePt	fcc, fct	3.0–17	OA, OAm
CoPt	fcc, fct	7.0	ACA, HDA
γ -Fe ₂ O ₃	fcc	3.0–25	OA, SA
Fe ₃ O ₄	fcc	8.0–30	OA
CoO	fcc	~8	TOP
CoFe ₂ O ₄	fcc	2.0–12	OA

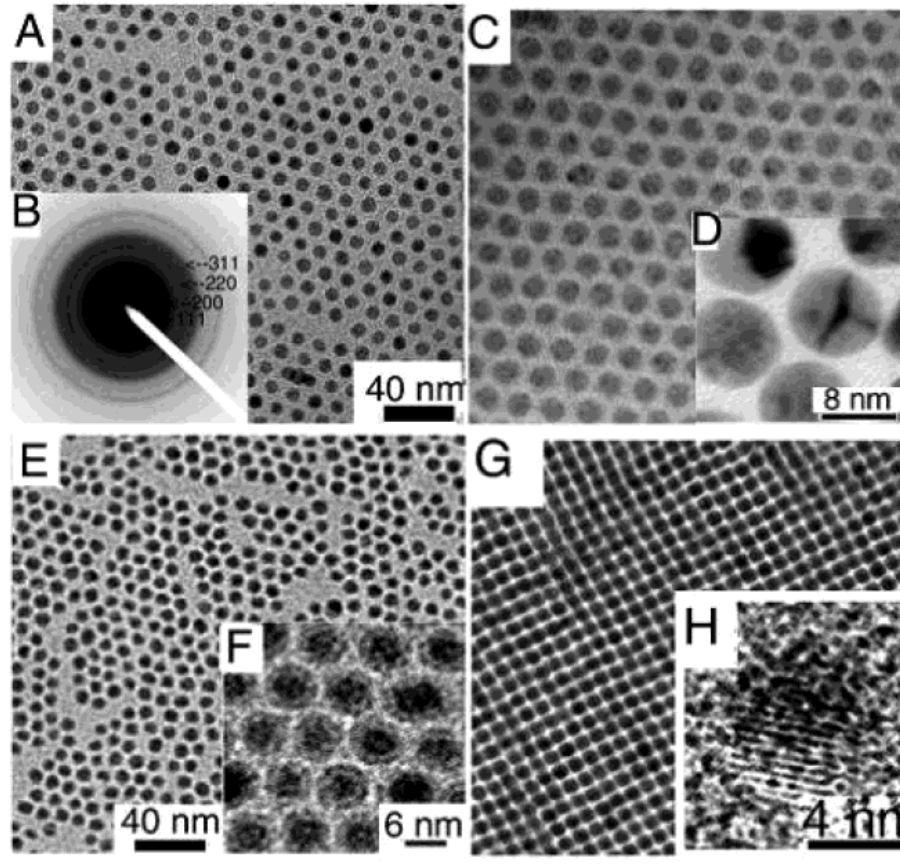
Synthesis of Monodisperse Spherical Nanocrystals

Jongnam Park, Jin Joo, Soon Gu Kwon, Youngjin Jang, and Taeghwan Hyeon

Angew. Chem. Int. Ed. 2007, 46, 4630 – 4660

High temperature decomposition of organic precursors

**8 nm Co-Ni
alloy nanoparticles**



**8 nm Co
nanoparticles**

**6 nm Fe
nanoparticles**

**6 nm FePt
nanoparticles**

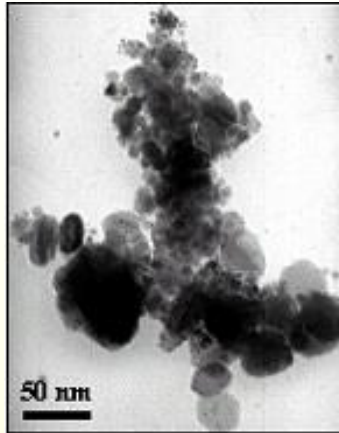
Sun and Murray et al. 2000 Science, 287, 1989

High temperature decomposition of organic precursors

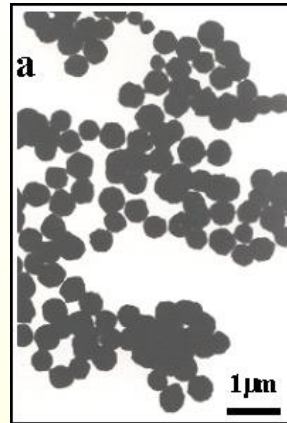
Surfactant

Co

No surfactant

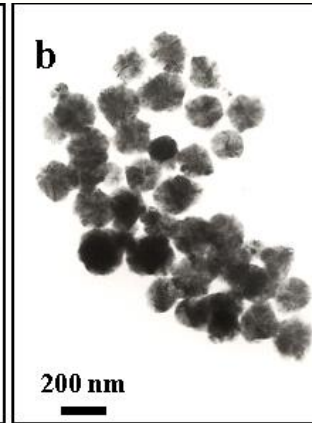


Seeds: Ag



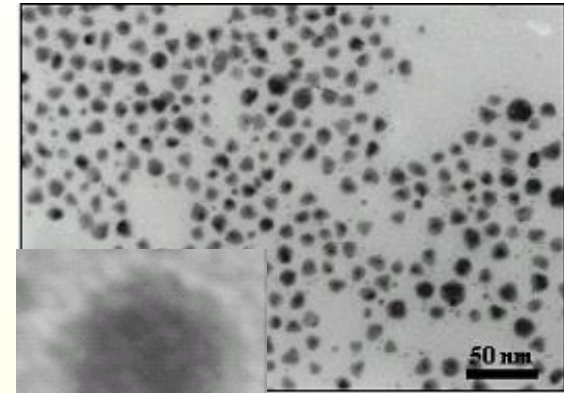
500 nm

Pt

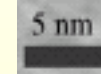


100 nm

Pt + oleico



10 nm



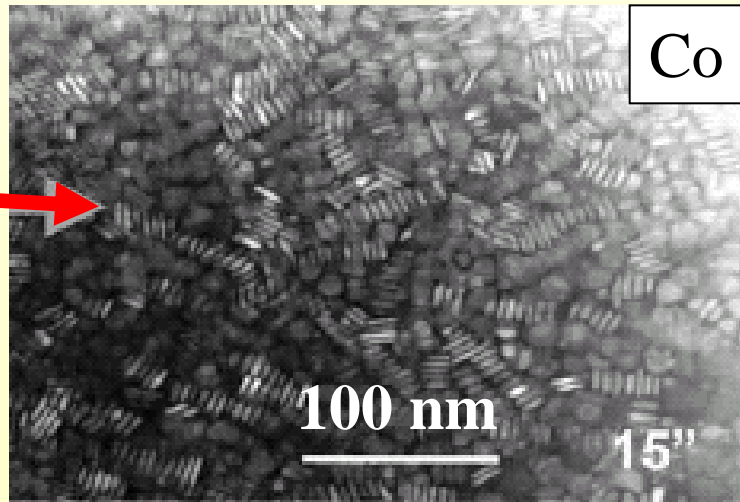
Nanotechnology 14, 268, 2003 and
Nanotechnology 15, S293, 2004

$\text{Co}_2(\text{CO})_8$

Oleic acid

+

TOPO



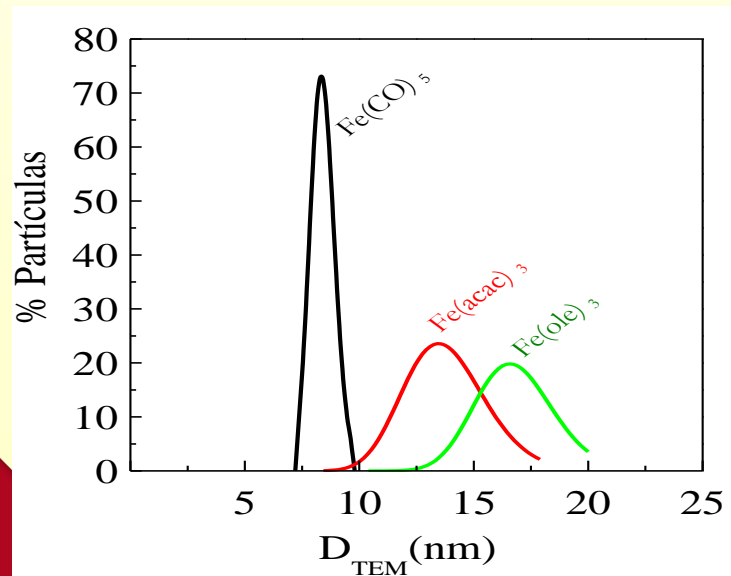
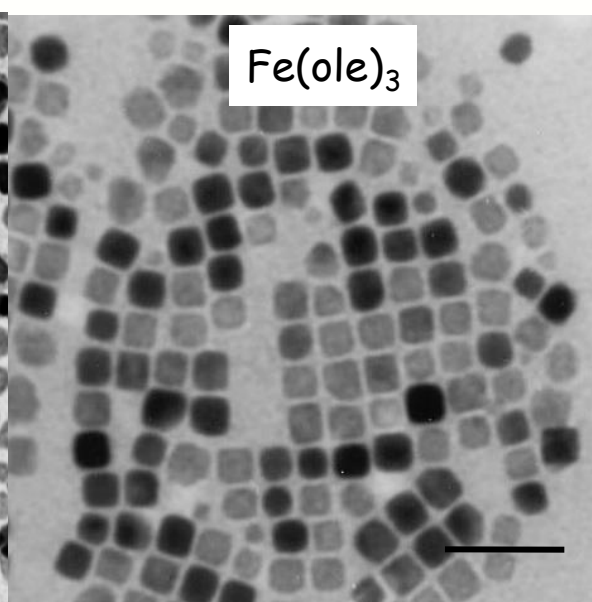
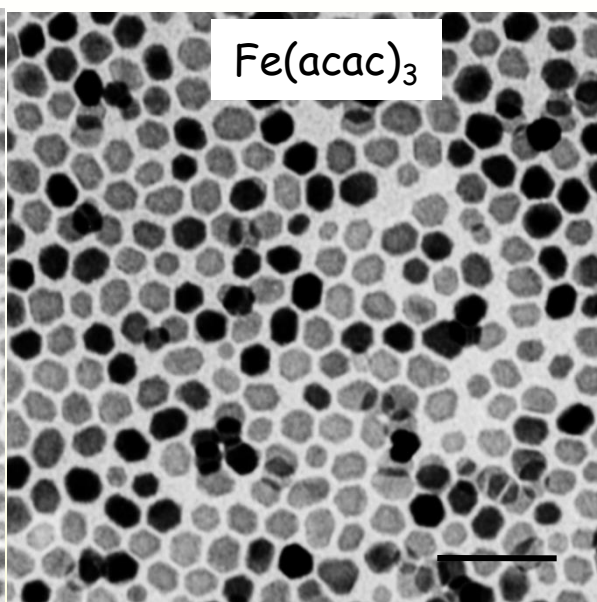
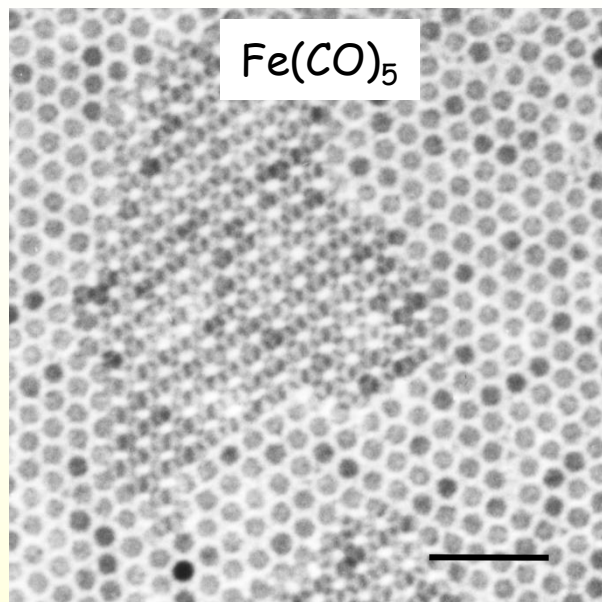
V.F. Puntes et al., Science 291 (2002) 2115

**Effect on
particle size
and shape**

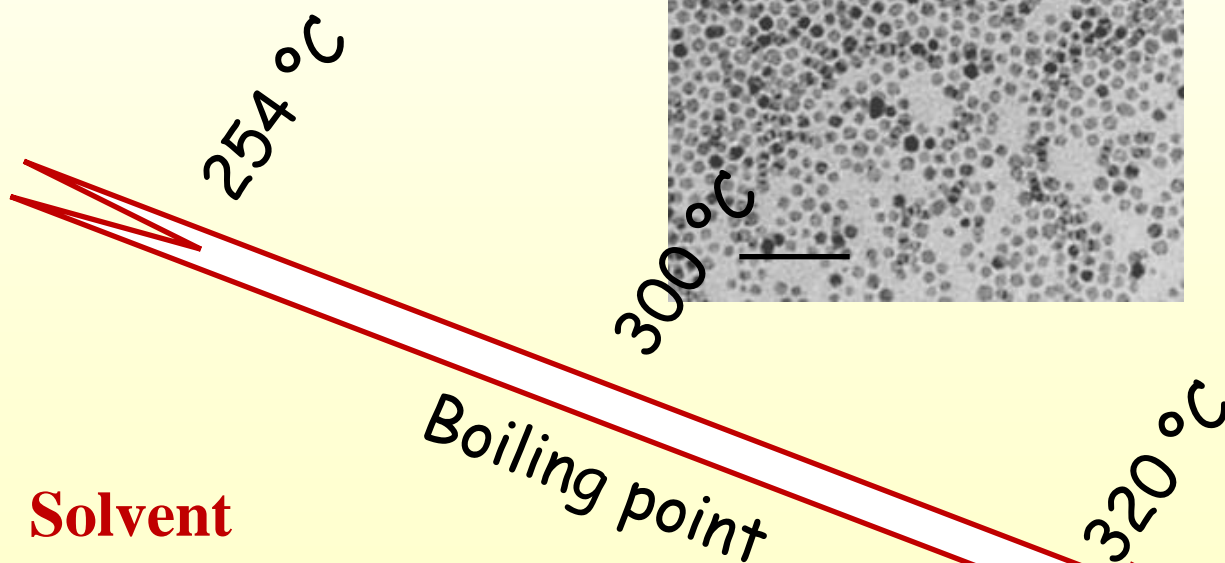
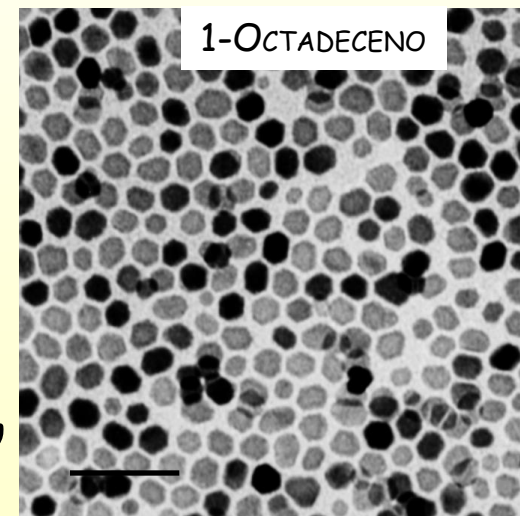
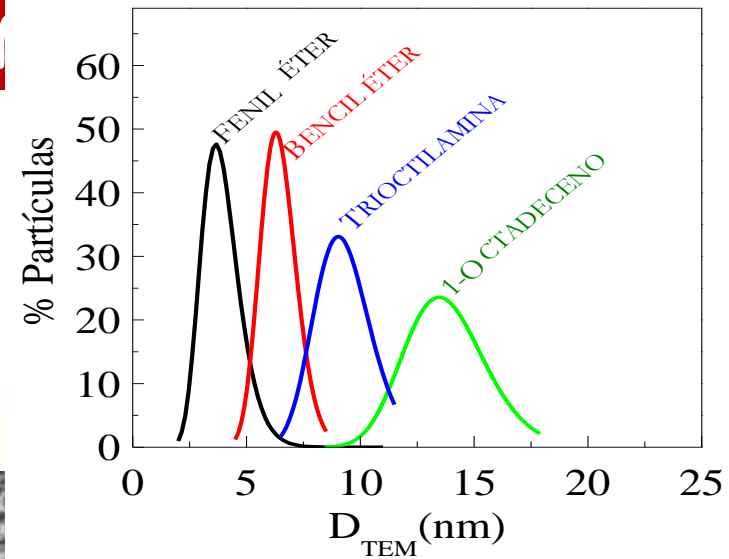
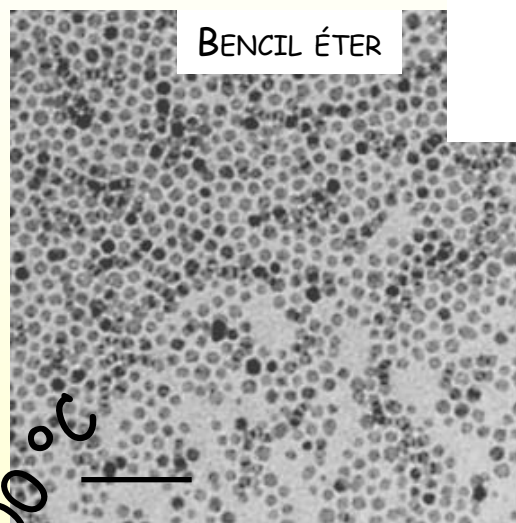
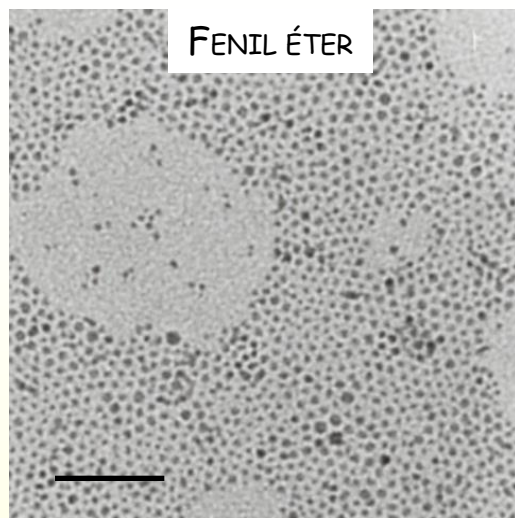
High temperature decomposition of organic precursors

Precursor

Fe_3O_4

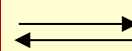
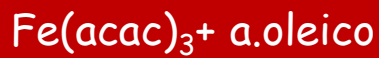
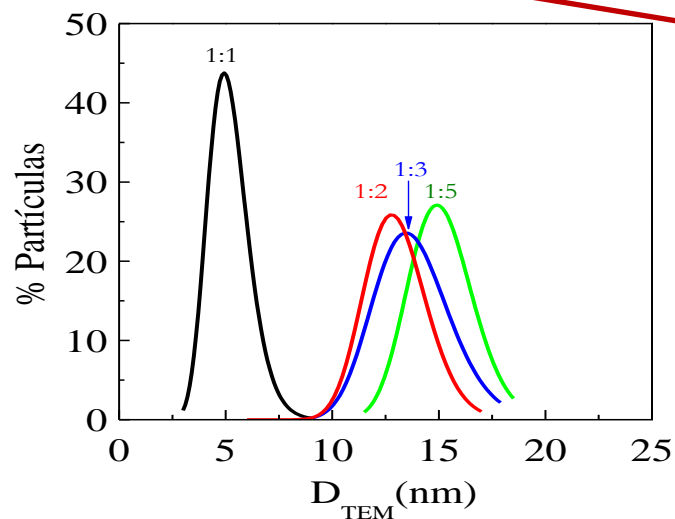
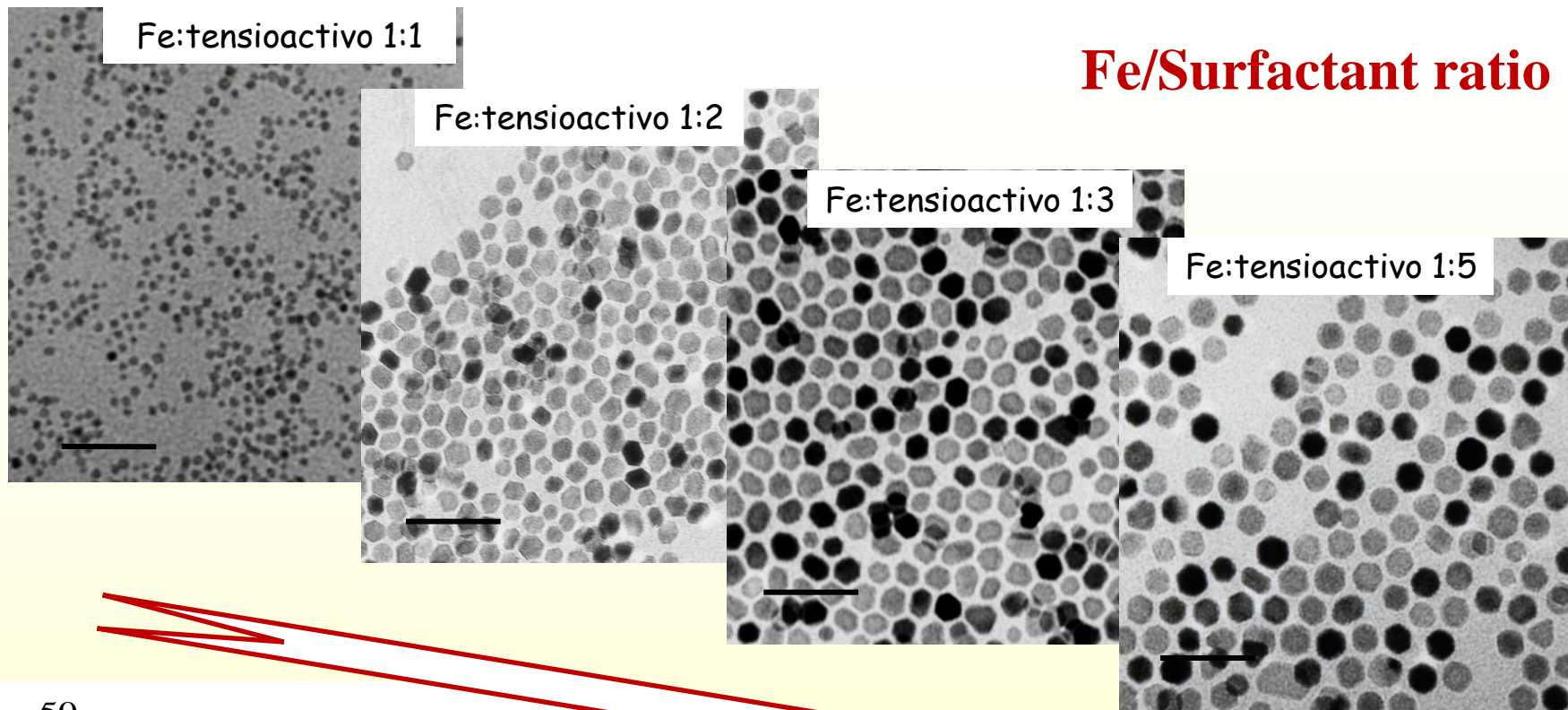


High temperature decomposition of



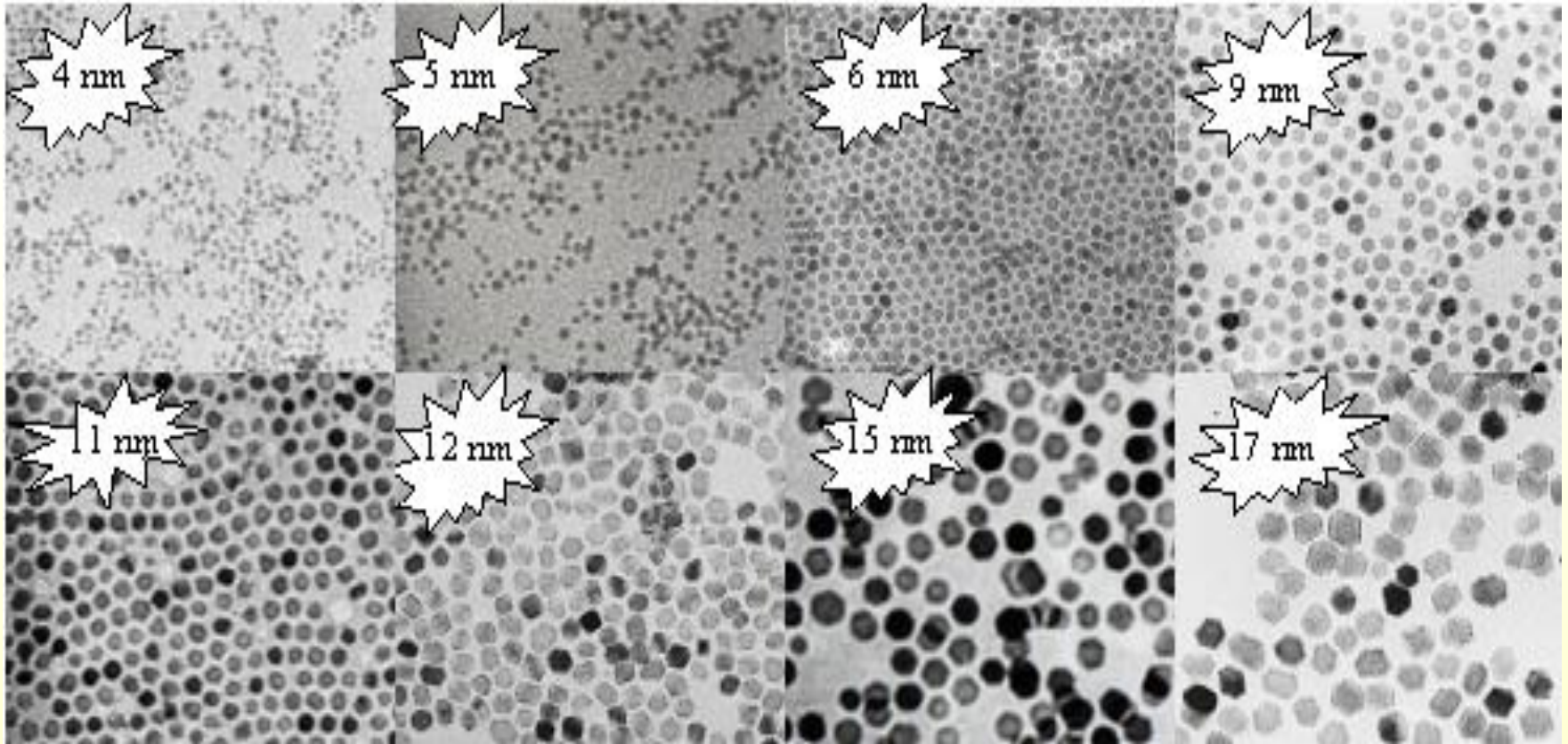
High temperature decomposition of organic precursors

Fe/Surfactant ratio



High temperature decomposition of organic precursors

Size control



Iron oxide nanoparticles showing one nanometer increments in diameter

Roca, A. G. et al *Nanotechnology* **2006**, *17*, 2783-2788.

IEEE TRANSACTIONS ON MAGNETICS, *42*, 3025 (2006)

Instituto de Ciencia
de Materiales de Madrid

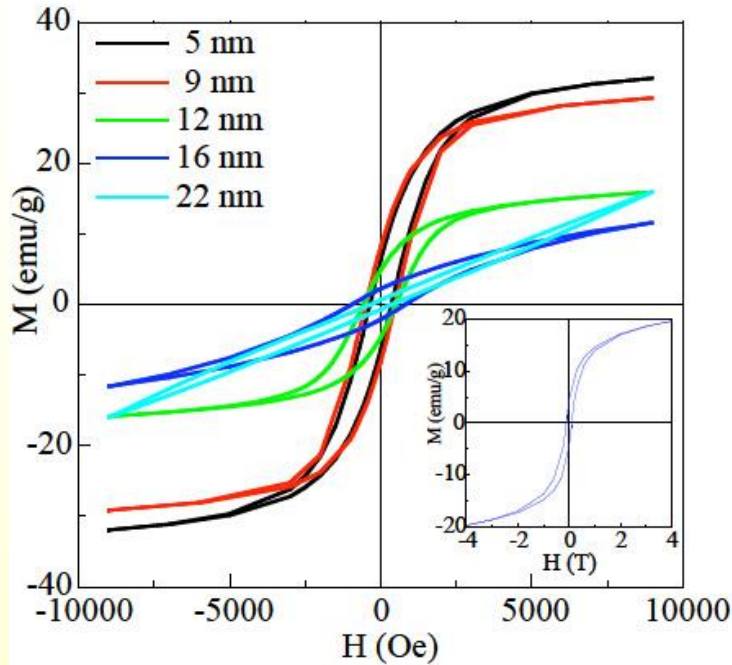


CSIC

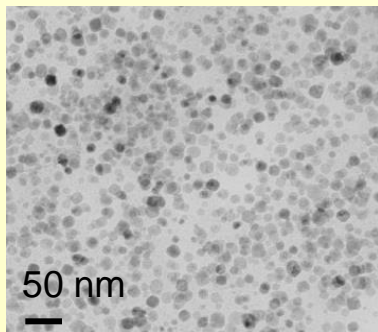
CONSEJO SUPERIOR DE INVESTIGACIONES CIENTÍFICAS

High temperature decomposition of organic precursors

Problems: low Ms at larger sizes

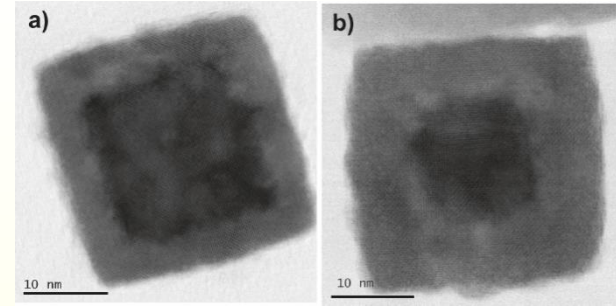


Park, J. *et al. Nat. Mater.* **2004**, 3, 891-895



Broad size-distribution

Other phases

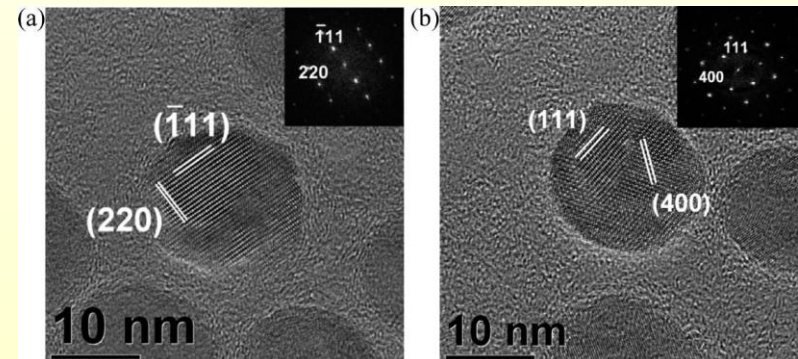


wüstite-spinel core-shell structure



Pichon *et al Chem. Mater.* **2011**, 23, 2886-2900

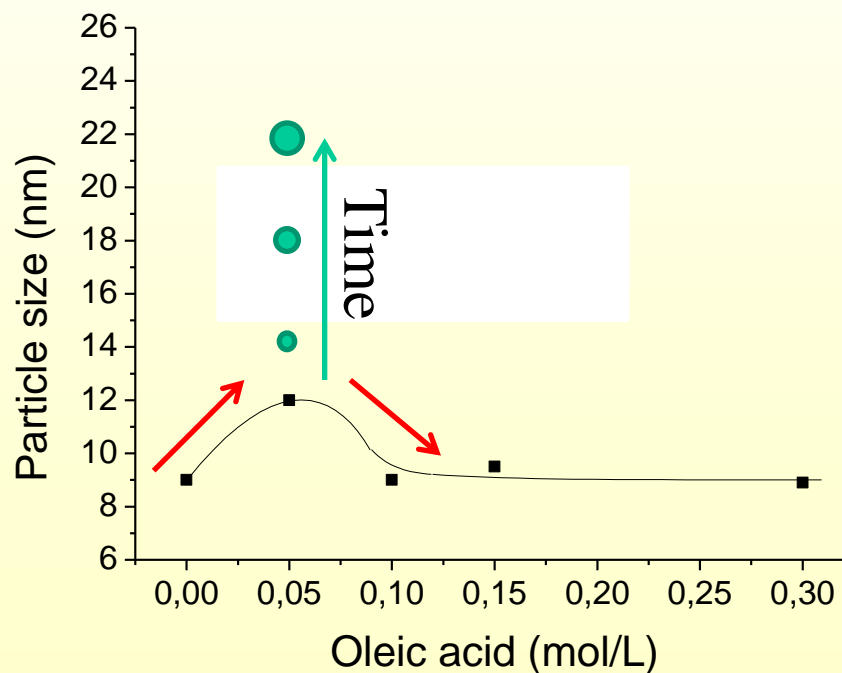
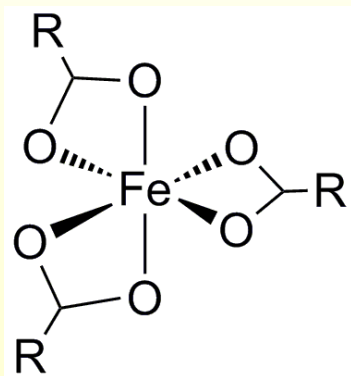
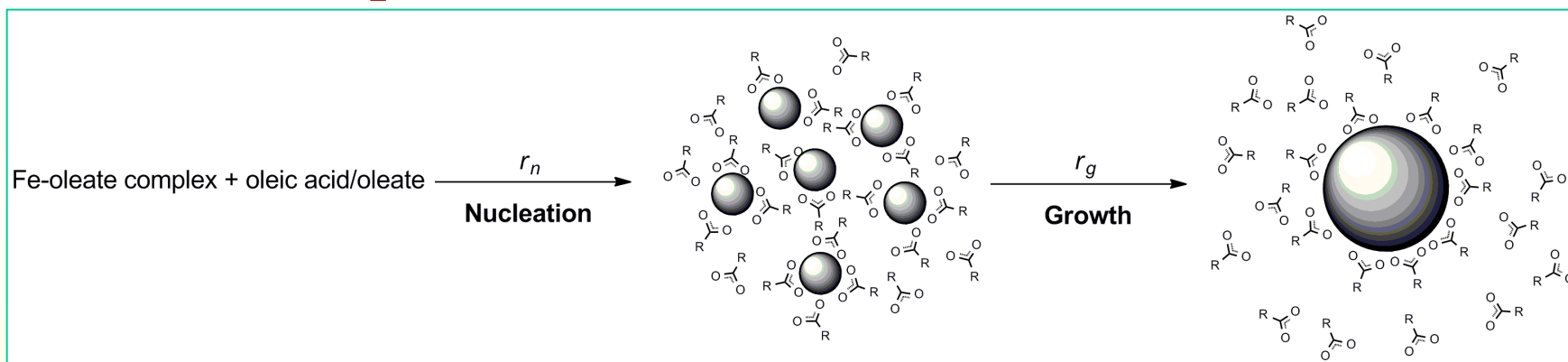
Structural imperfections



[*Chem. Mater.* 2011, 23, 4170–4180

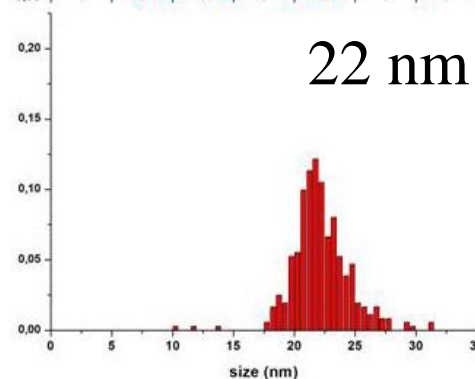
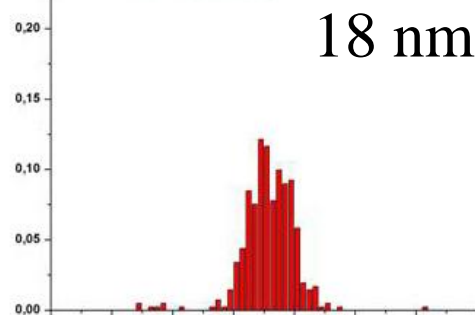
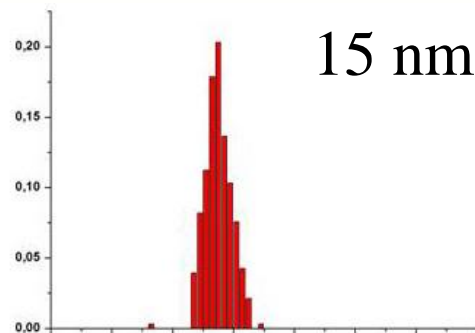
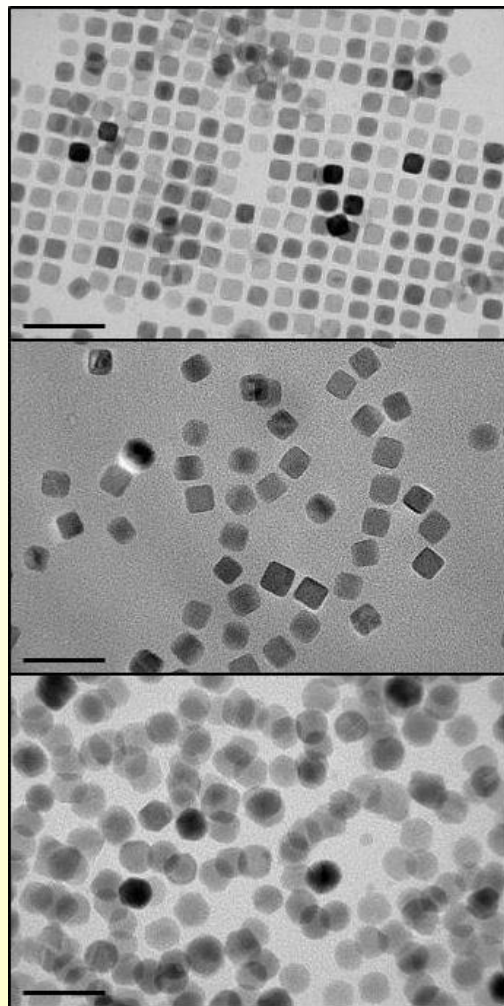
High temperature decomposition of organic precursors

Iron oleate as precursor



High temperature decomposition of organic precursors

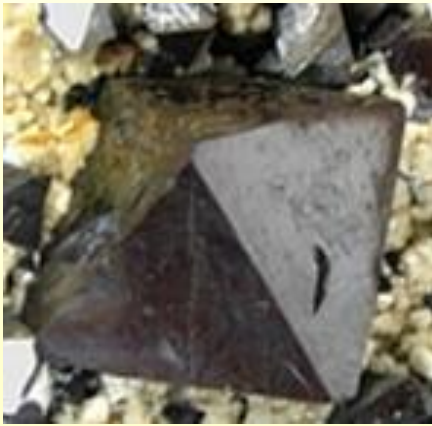
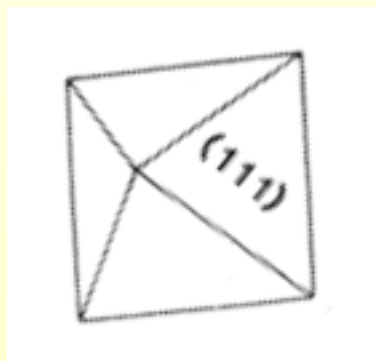
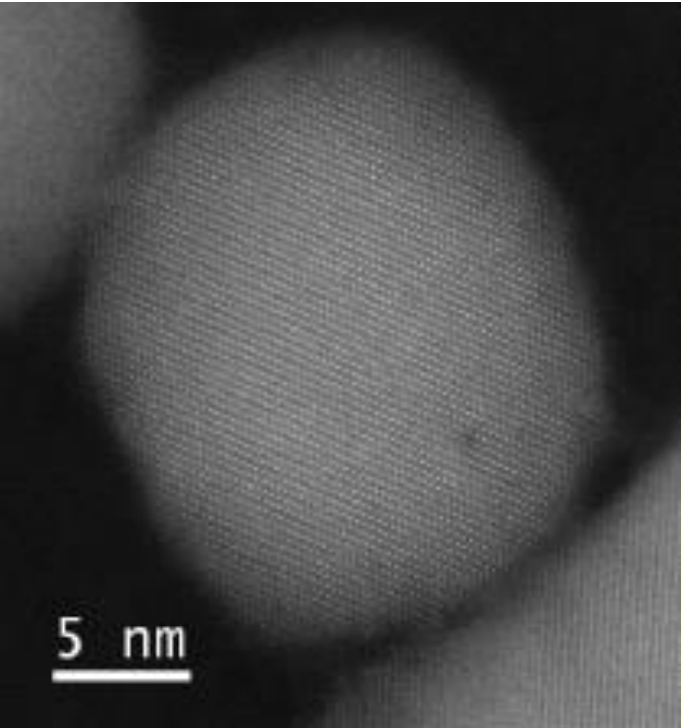
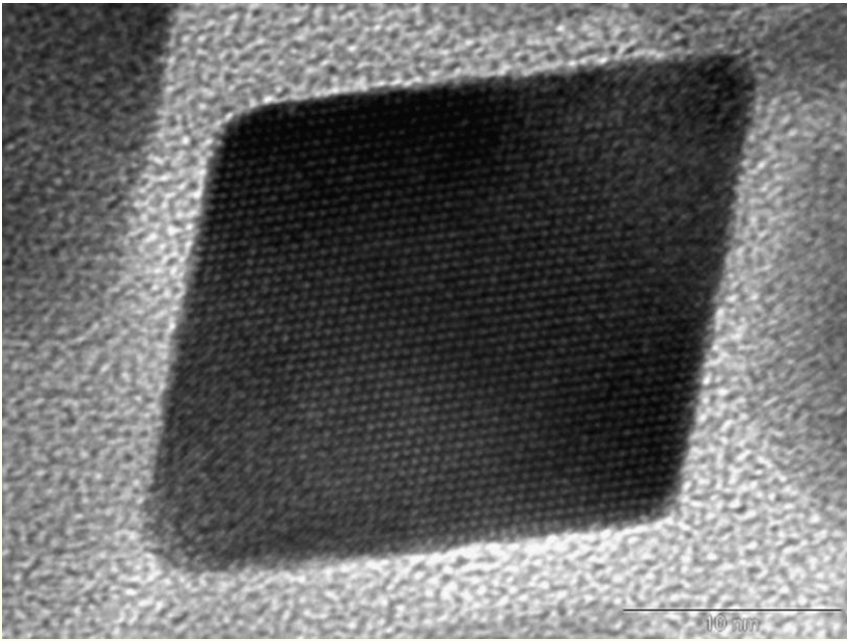
Iron oleate as precursor + longer reaction times + No stirring



$$\sigma = 9\%$$

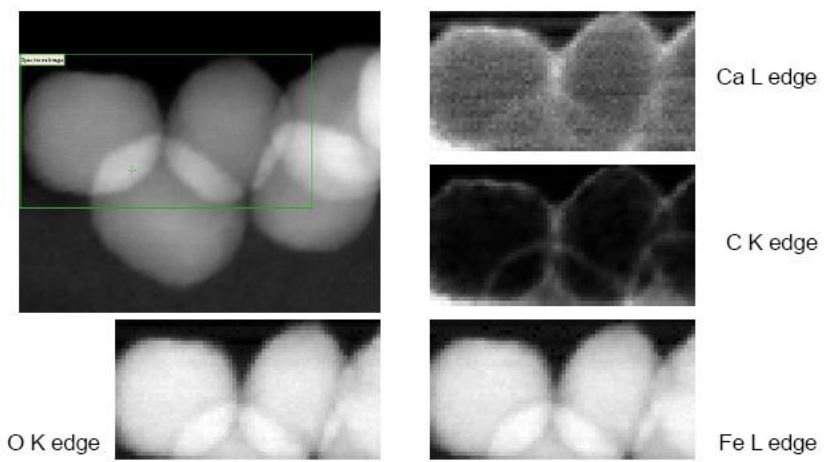
HIGH QUALITY NANOCRYSTALS

M. Varela, UltraSTEM200 2 200 kV, Oak Ridge National Laboratory

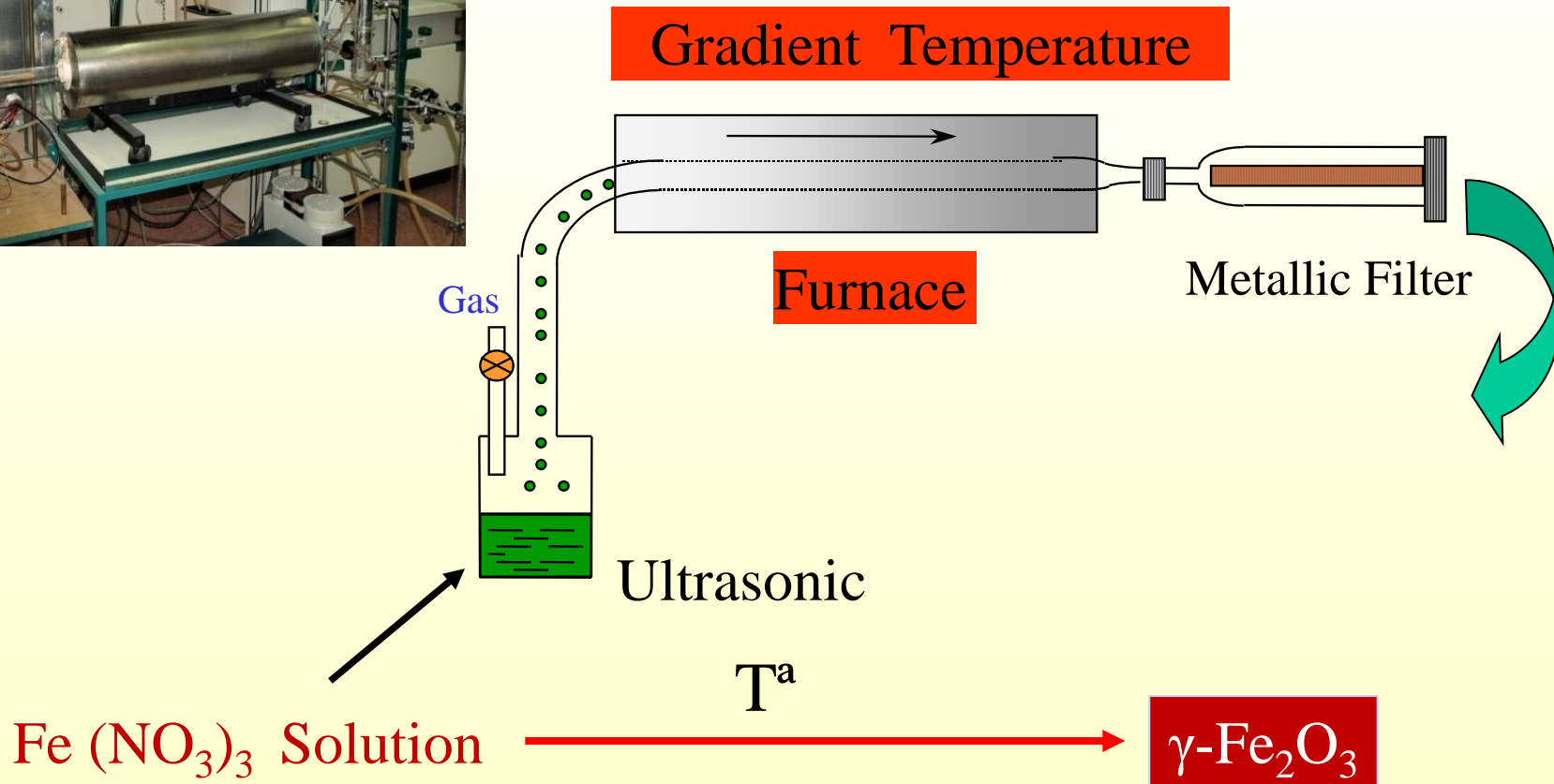


Magnetita: octaedro de 1.8 cm.
Cerro Huañaquino (Bolivia)

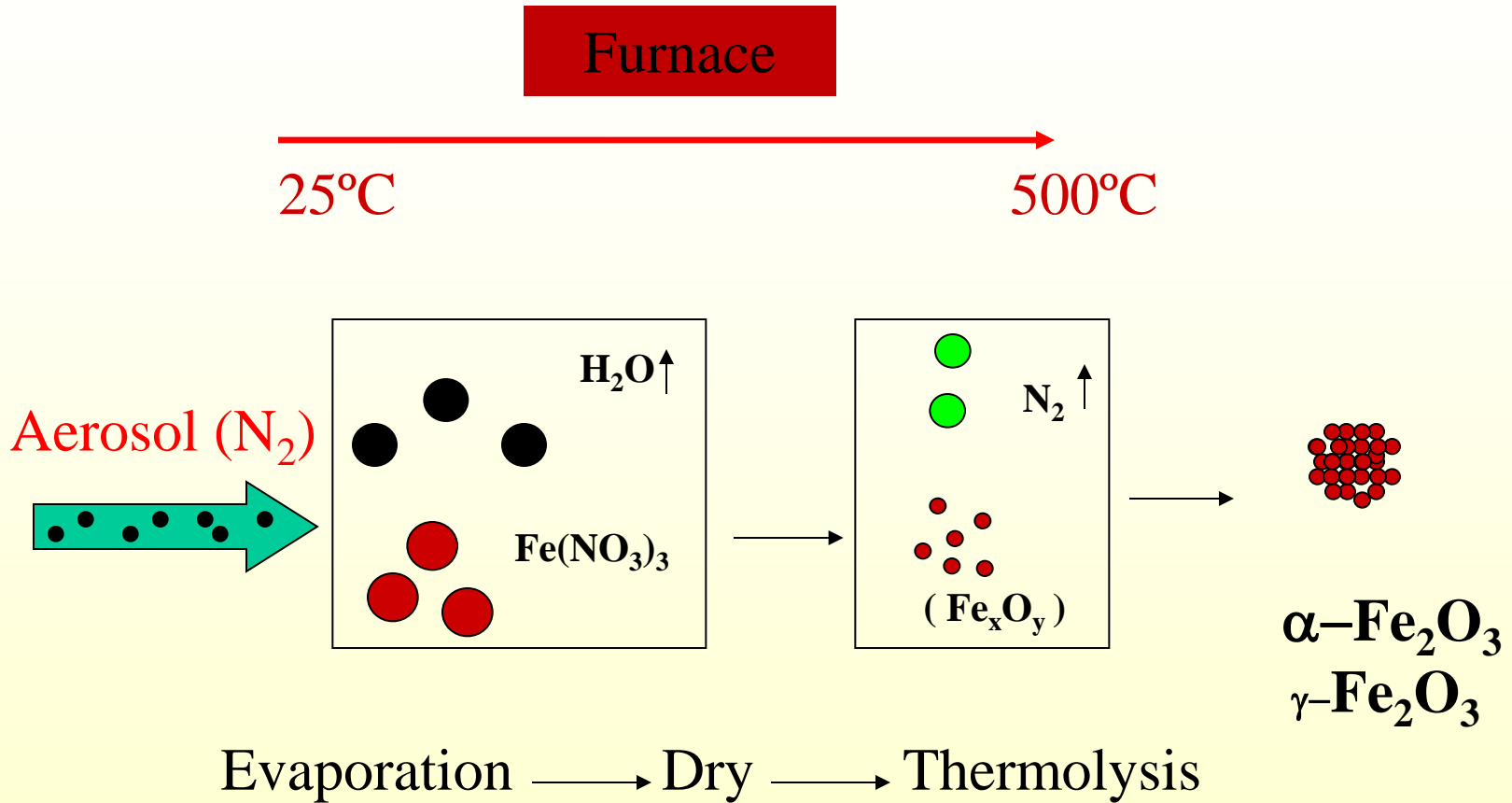
EELS elemental maps



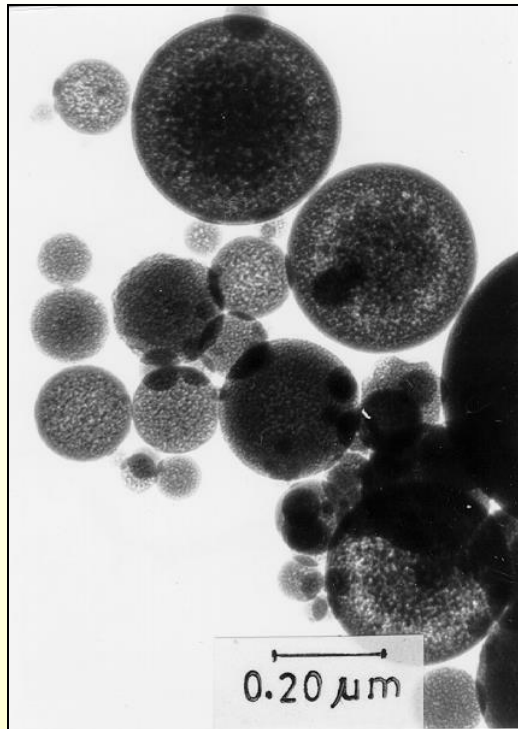
SPRAY PYROLYSIS METHOD



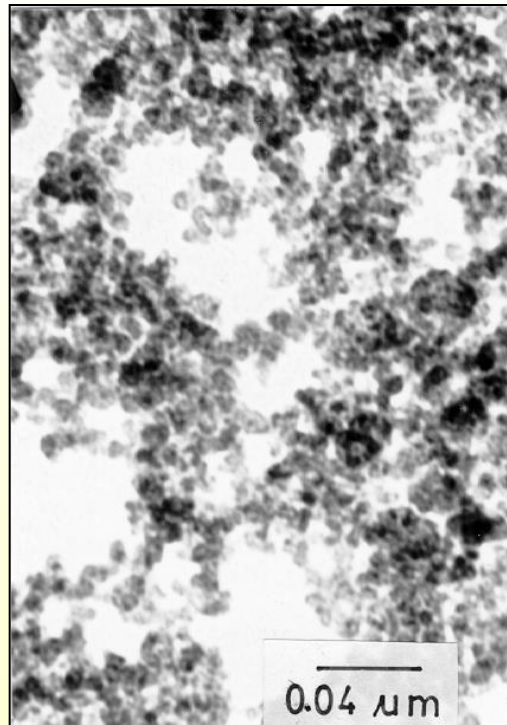
SPRAY PYROLYSIS METHOD



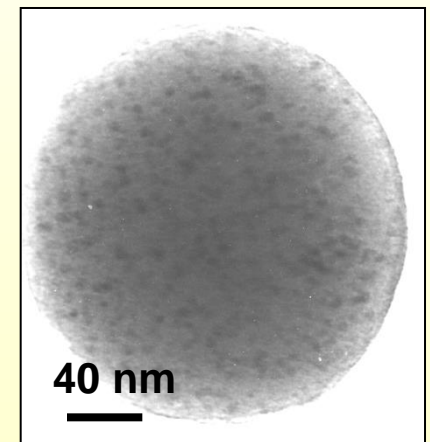
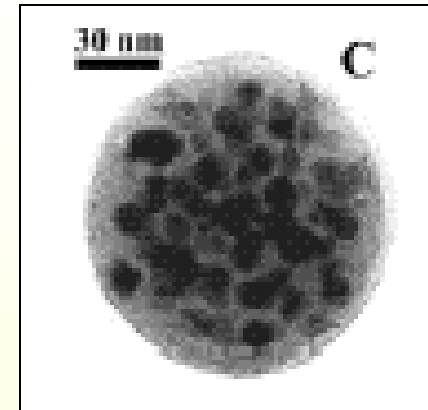
SPRAY PYROLYSIS METHOD



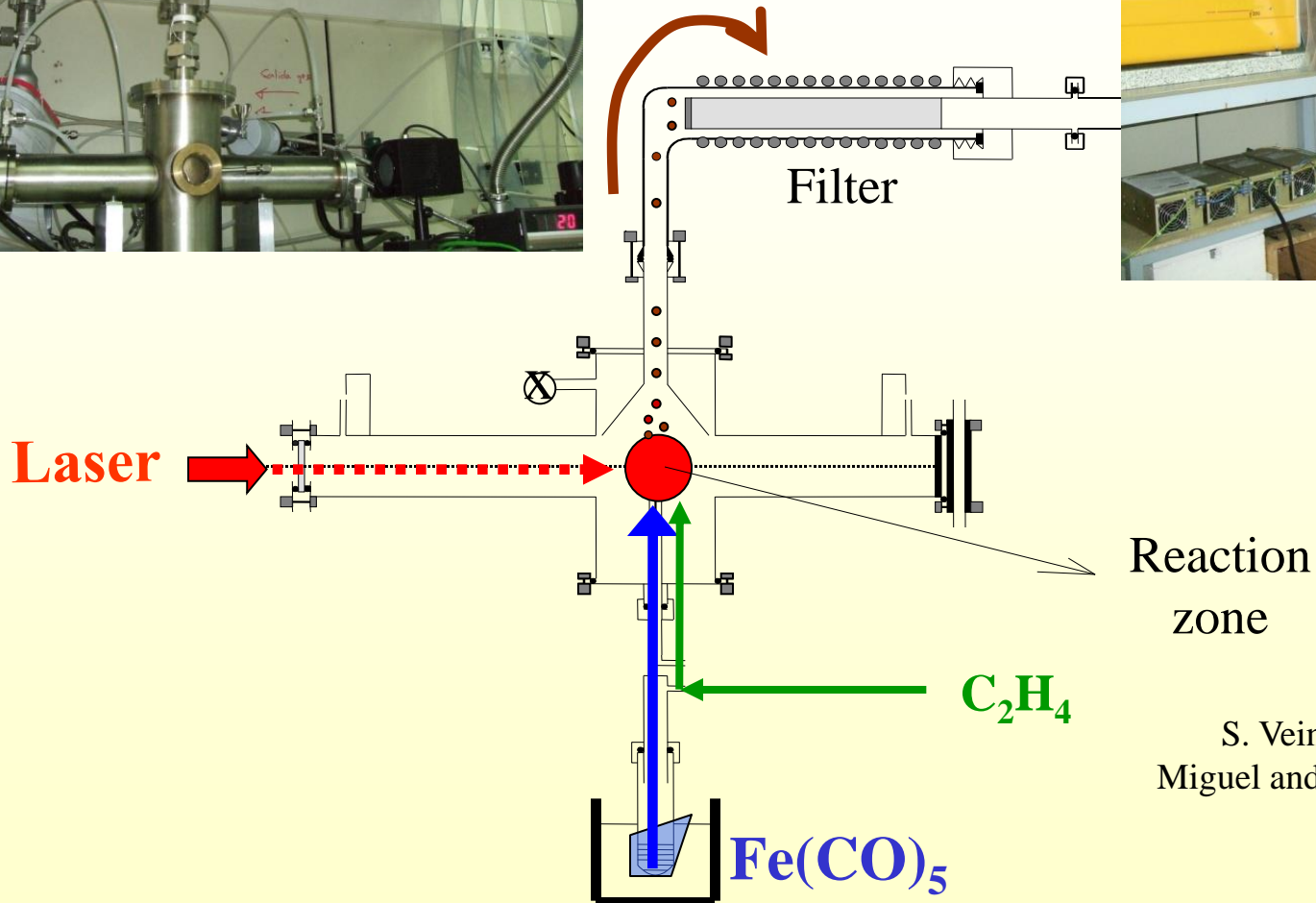
Nitrates



Acetylacetonate



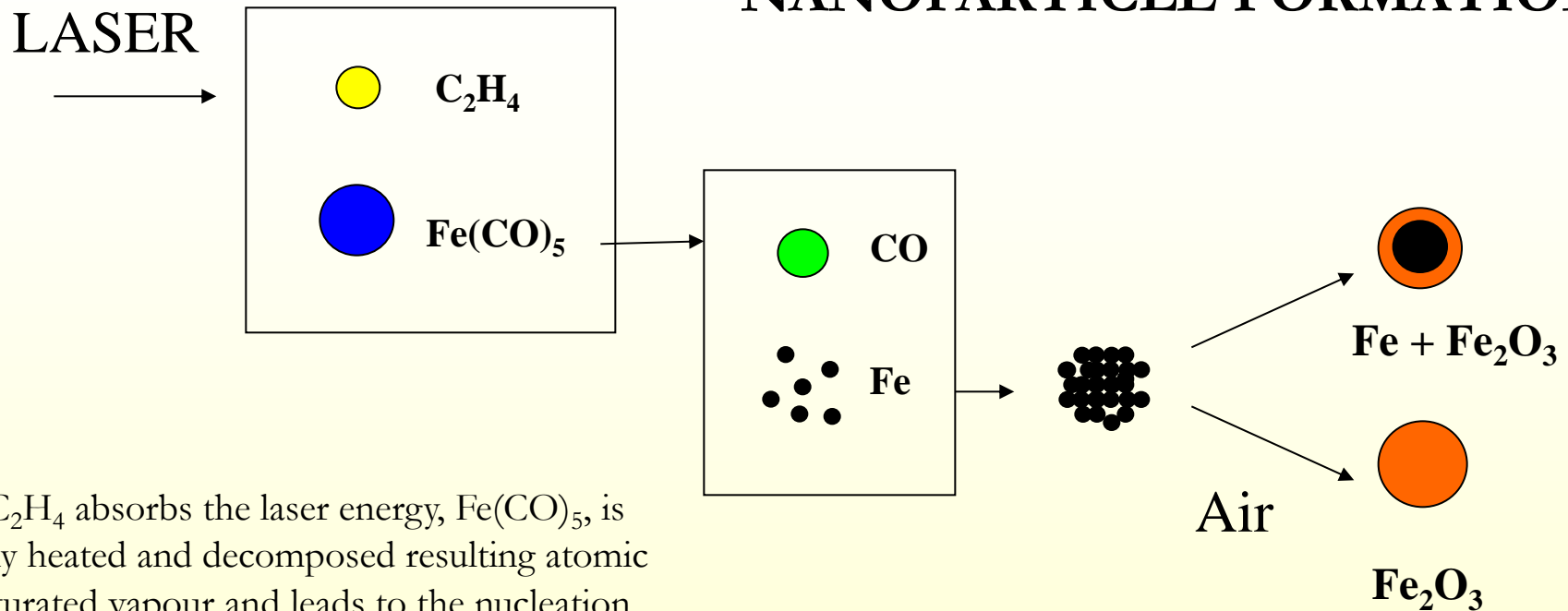
Laser Pyrolysis



S. Veintemillas-Verdaguer, O. Bomati-Miguel and M.P. Morales. *Scripta Mater.*, 47, 589-593 (2002)

Laser Pyrolysis

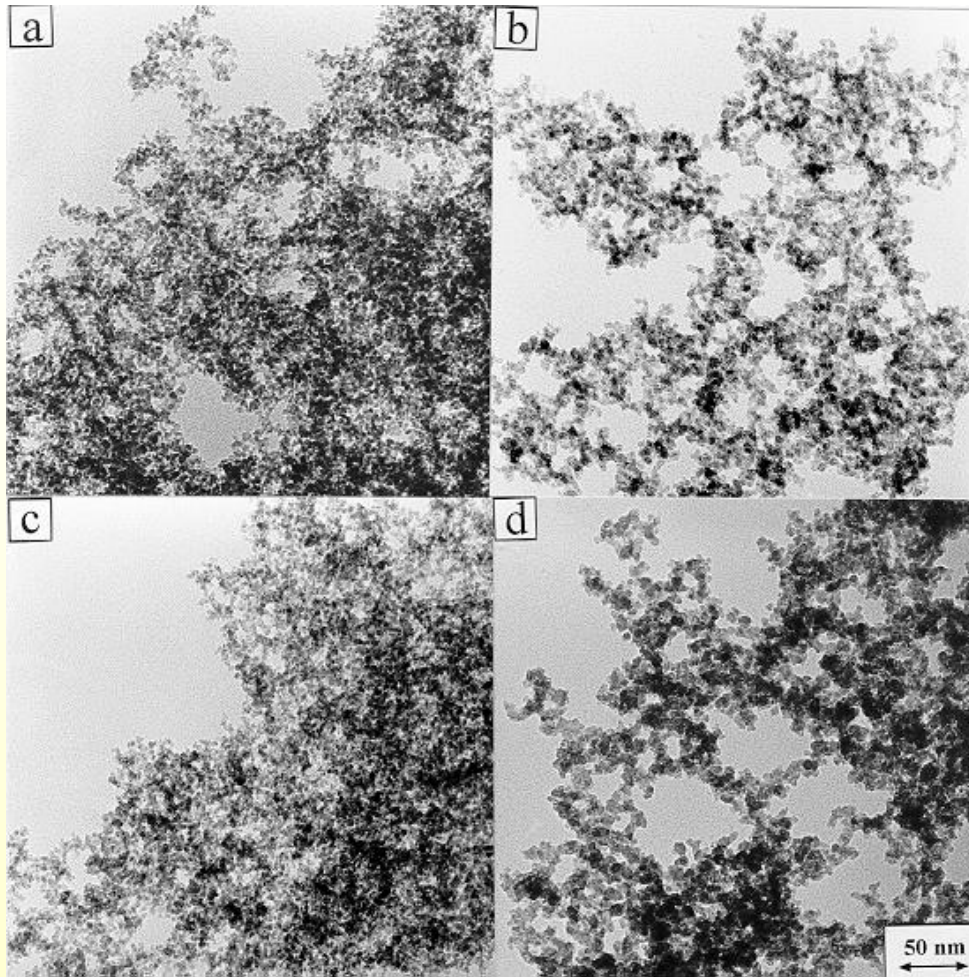
MECHANISM OF NANOPARTICLE FORMATION



The C_2H_4 absorbs the laser energy, $Fe(CO)_5$, is rapidly heated and decomposed resulting atomic Fe saturated vapour and leads to the nucleation and growth of iron metal nucleus

To stabilise the powders, a mixture of air and ethylene can be introduced together with the iron pentacarbonyl (hard oxidation) or after the laser pyrolysis (soft oxidation).

Laser Pyrolysis



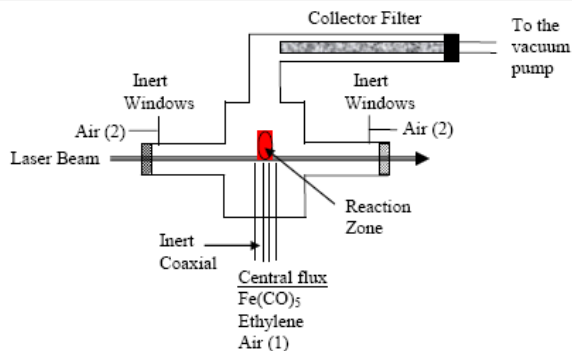
Increasing size
as increasing
precursor
temperature and
therefore the
concentration of
iron atoms in
the reaction cell

$\gamma\text{-Fe}_2\text{O}_3$ Nanoparticles with sizes between 3-5 nm

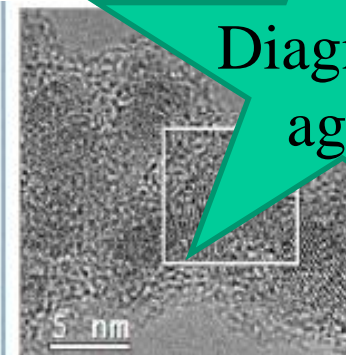
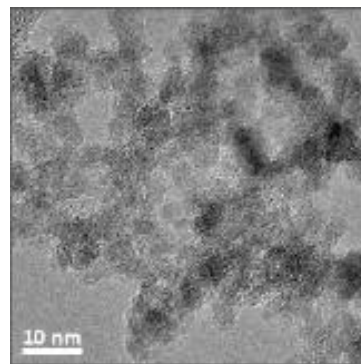
FP VI/ BONSAI: Bio-imaging with Smart Functional Nanoparticles



Preparation of magnetic iron oxide nanoparticles by laser pyrolysis



The Laser Pyrolysis technique enables the continuous production of uniform iron oxide nanoparticles induced by the fast laser heating of iron pentacarbonyl in an oxidant environment.



Diagnostic agent

< 5 nm

Acid treatment

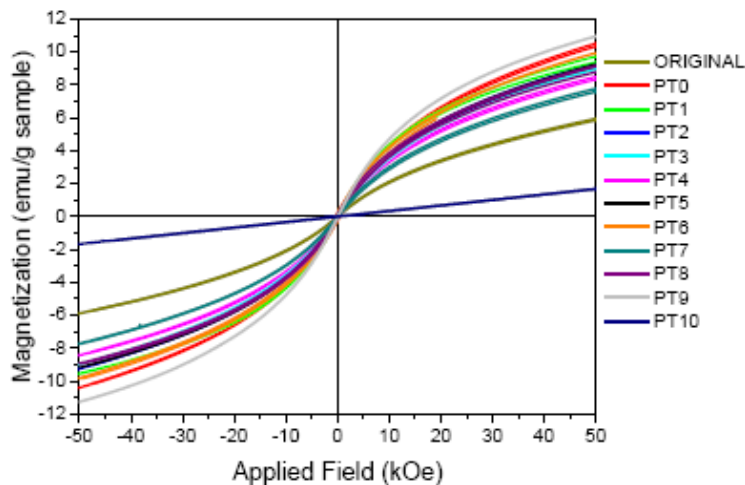


Figure 4.10: Magnetic curves at room temperature for all the samples. Sample named PT10 corresponds to PT10-30. . Sample PT11 presents a large amount of akaganeite and it has not been included in the graph.

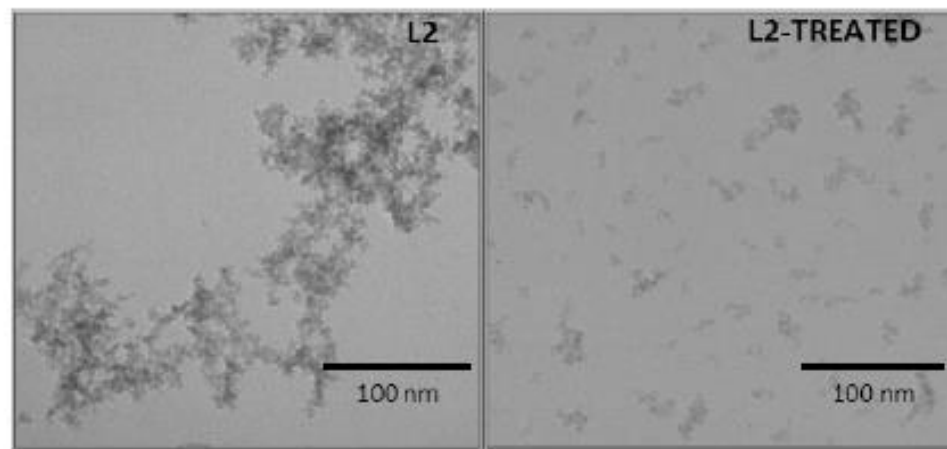


Figure 4.20: Low resolution TEM images of the original sample (L2) on the left and the sample after the acid treatment (L2-TREATED) on the right.

Hydrophilic coating (polar - H₂O)

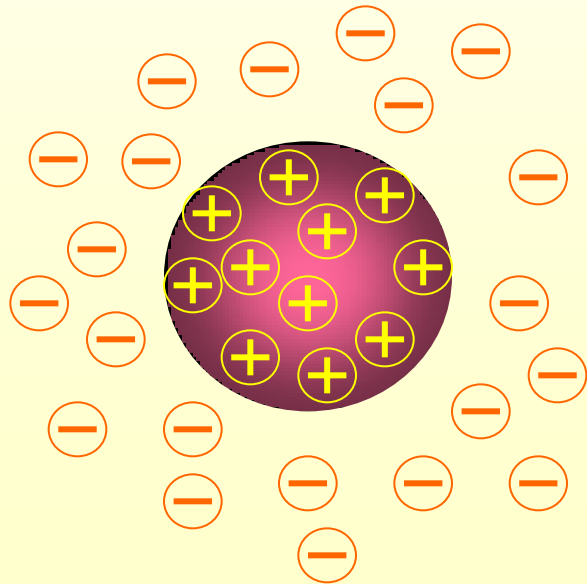
- ✓ Avoid aggregation
- ✓ Avoid no specific adsorption of proteins
- ✓ Low toxicity
- ✓ Selectivity
- ✓ Allow further functionalization

**In general,
small, neutral, hydrophilic
=> Longer blood circulation times**

Electrostatic and Steric Stabilisation

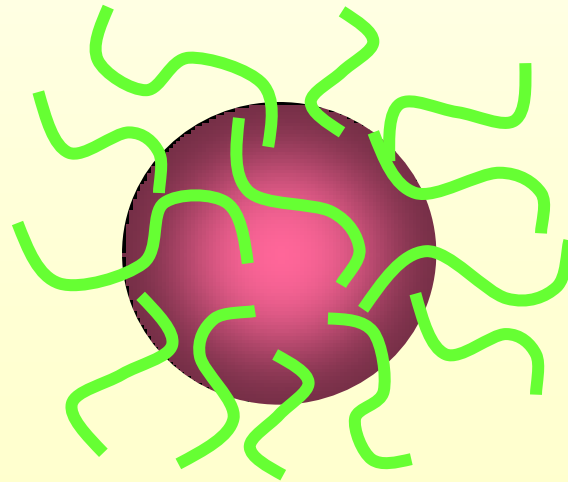
ELECTROSTATIC

- ▶ Easy to measure the controlling parameter (zeta potential)
- ▶ Reversible
- ▶ May only require change in pH or ion concentration

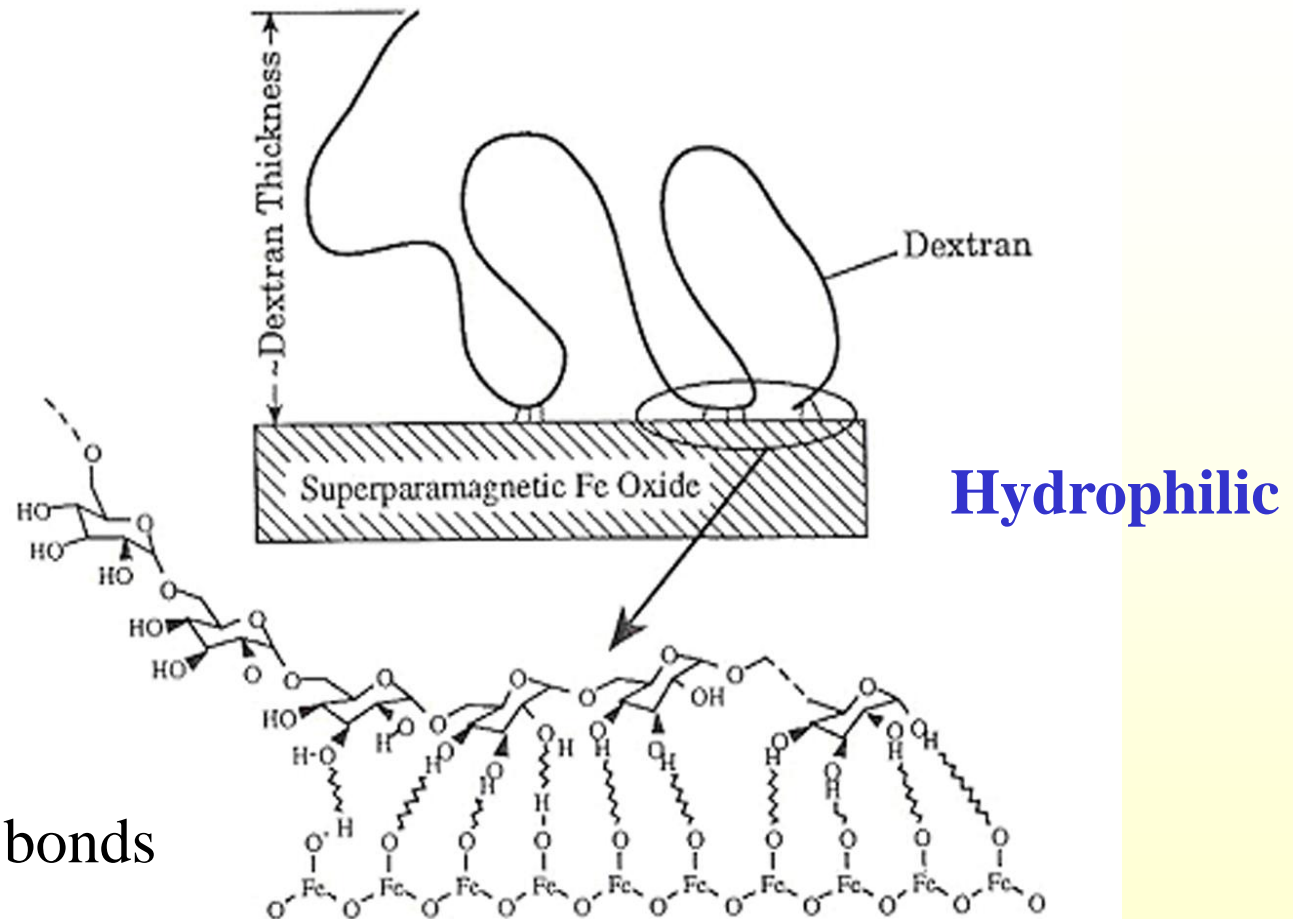


STERIC

- ▶ Simple, but limited options
- ▶ Irreversible
- ▶ An extra component

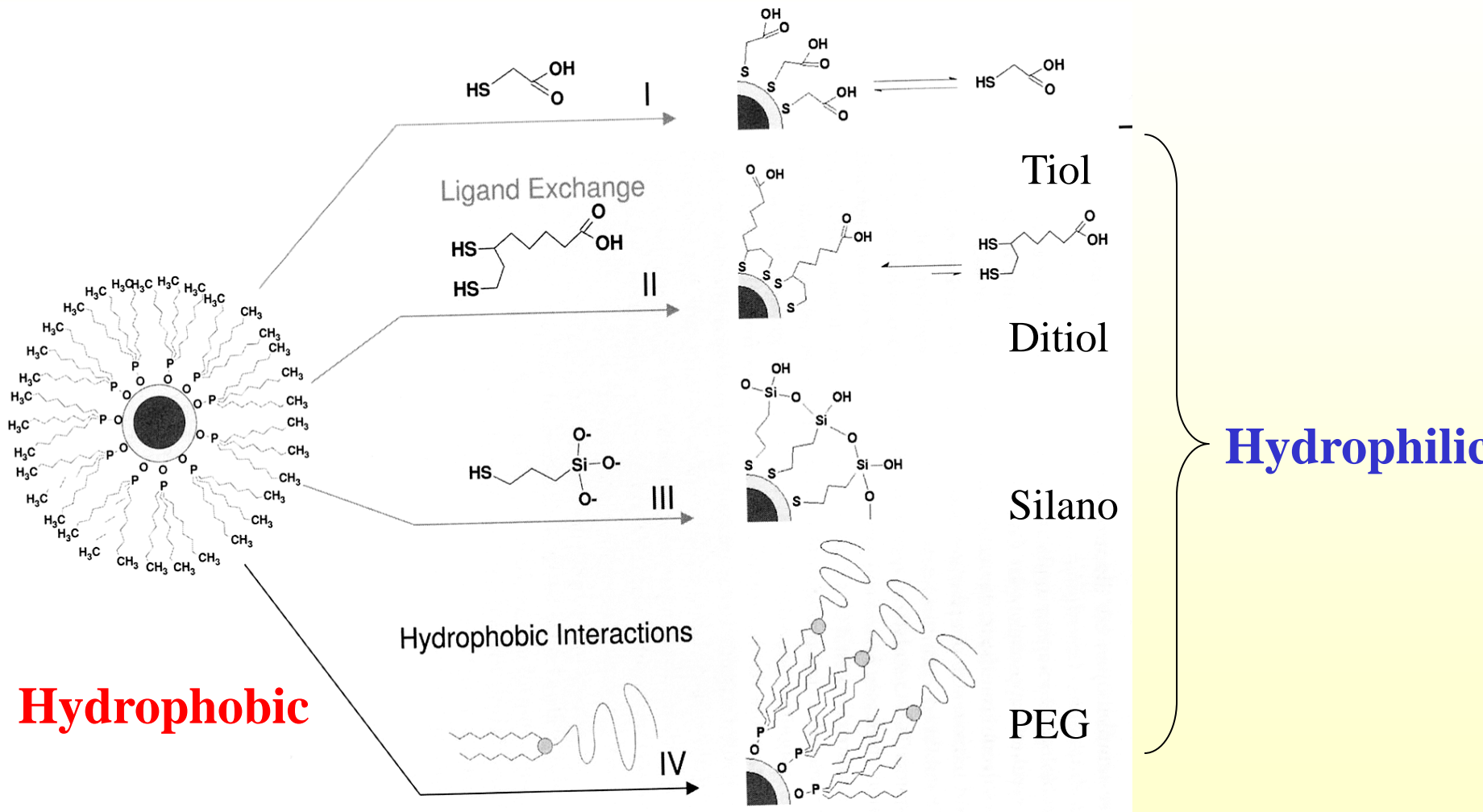


Adsorption



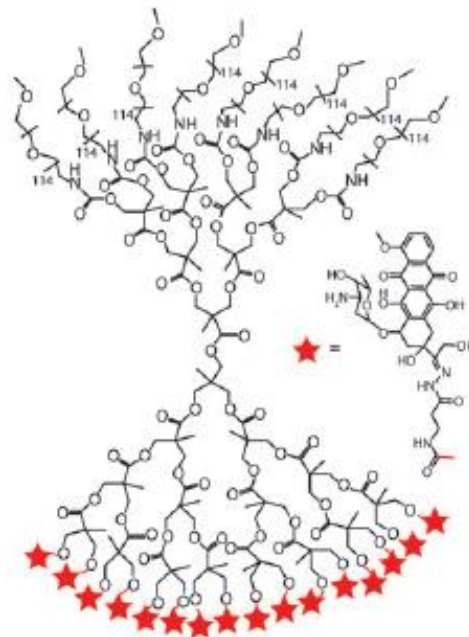
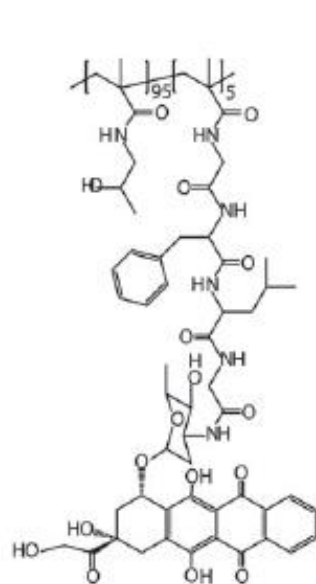
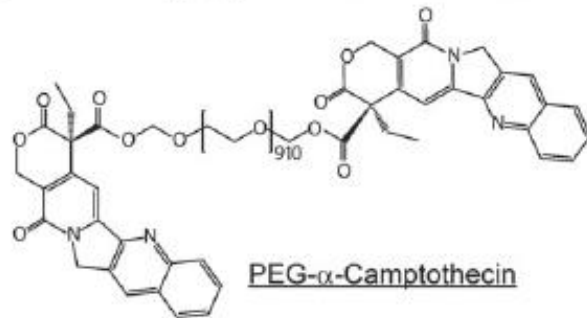
Hydrogen bonds

Ligand exchange or anphyphilic molecules

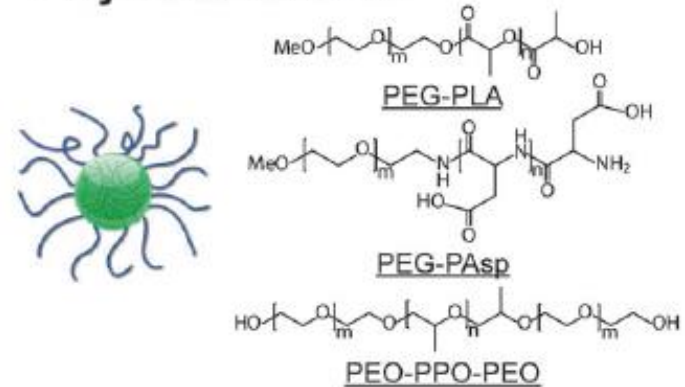


Surface Modification

Polymer conjugates and dendrimers



Polymeric micelles



Liposomes and polymersomes

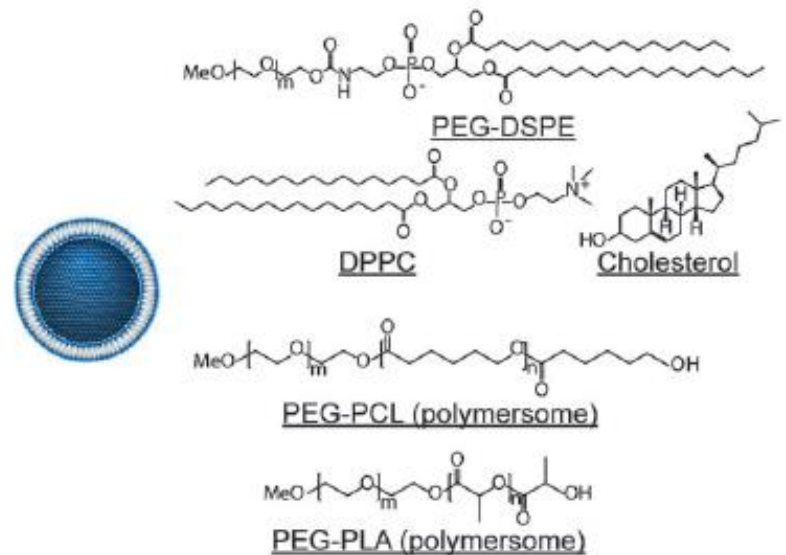


Fig. 4 Schematic illustration of chemical structures of representative polymer conjugates and dendrimers (*left*), polymeric micelles (*top right*), and liposomes and polymersomes (*bottom right*).

Biodegradable poly(D,L-lactic-co-glycolic acid) (PLGA)

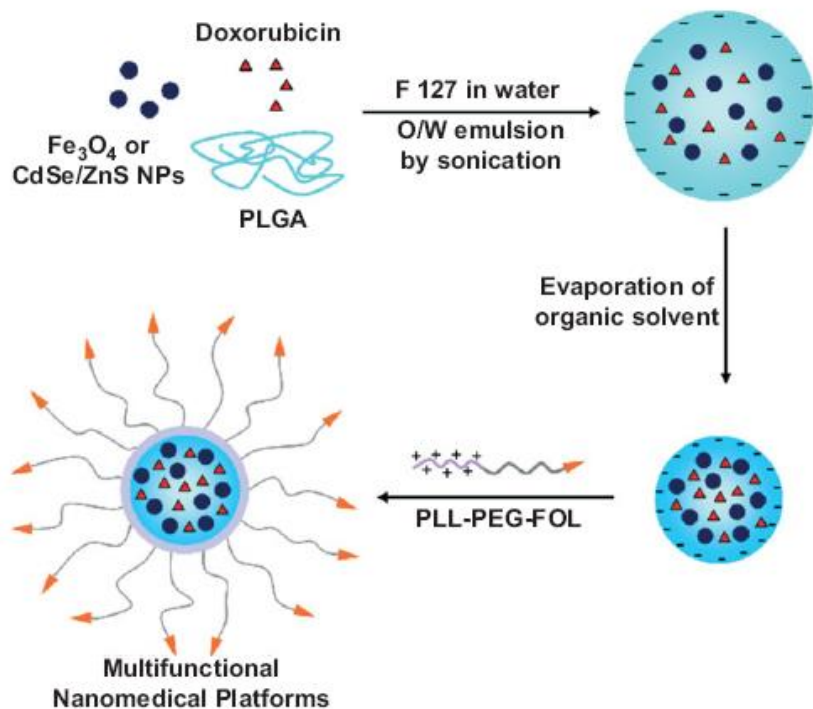


Figure 1. Synthetic procedure for the multifunctional polymer nanoparticles.

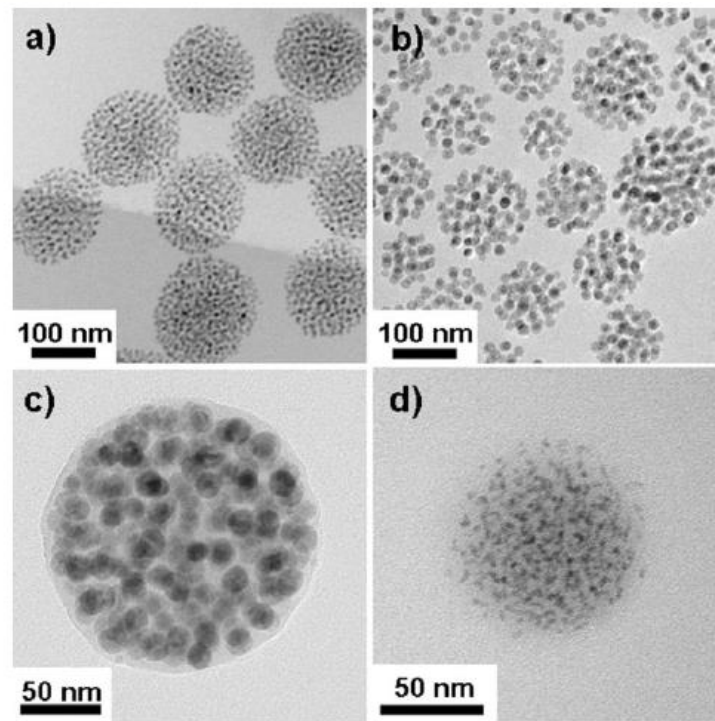


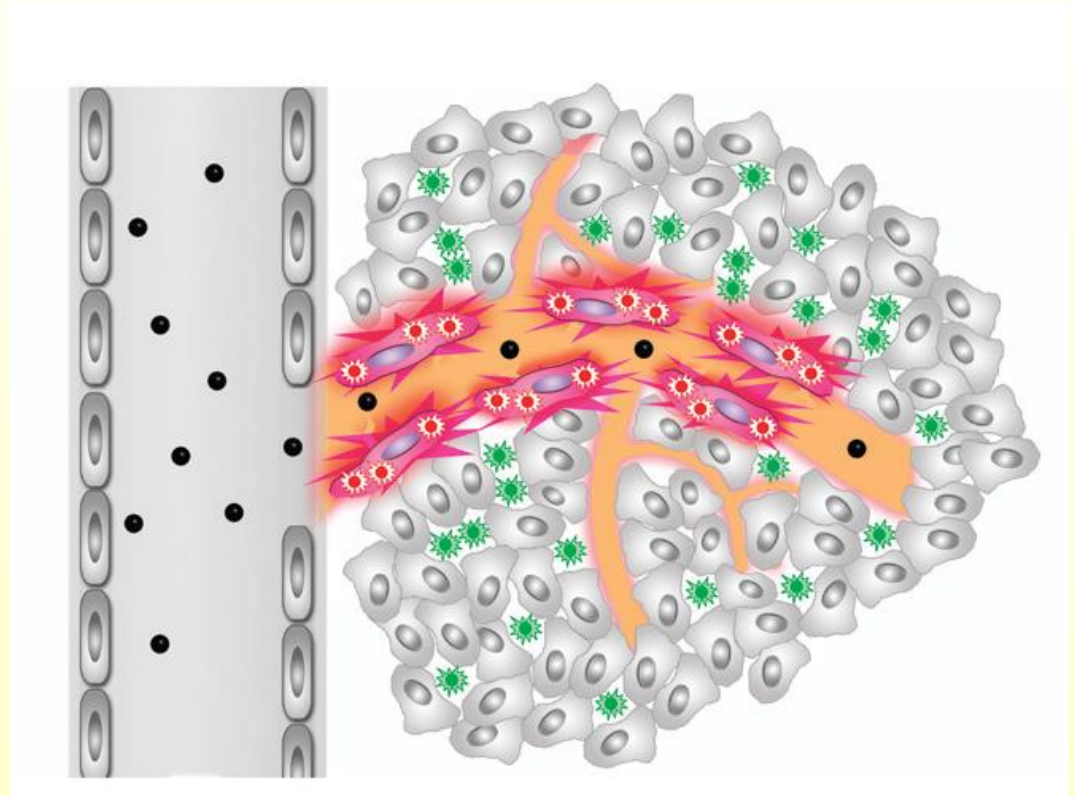
Figure 2. TEM images of PLGA(MNP/DOXO) nanoparticles embedded with a) 7-nm, and b), c) 15-nm Fe_3O_4 nanocrystals, and d) PLGA(QD/DOXO) nanoparticles embedded with 3-nm CdSe/ZnS nanocrystals.

Hydrophobic nanocrystals, DOXO, and PLGA in methylene chloride was poured into an aqueous solution containing F127, ultra-sonication, organic solvent was evaporated at room temperature by mechanical stirring and subsequently washed with deionized water several times.

Lighting up tumours : Detection of a wide range of tumours remains a challenge in cancer diagnostics.

pH-responsive polymeric nanomaterial

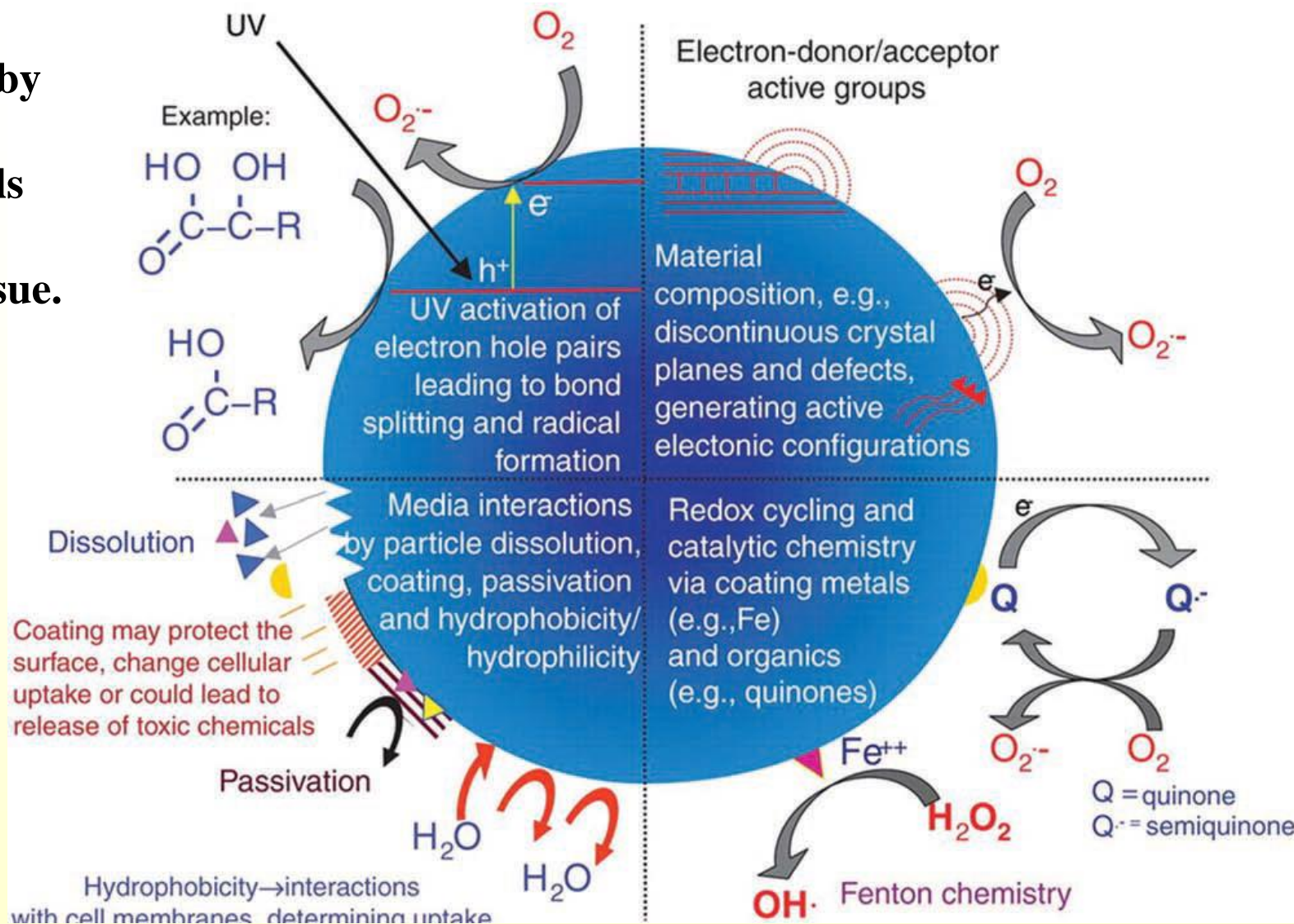
Highly fluorescent monomers within the acidic milieu of tumours (pHe, 6.5–6.8) or endocytic vesicles (pHi, 5.0–6.0) of the tumour endothelium.



PROBLEMS

- Nanoparticle-cell interactions
- Biodistribution

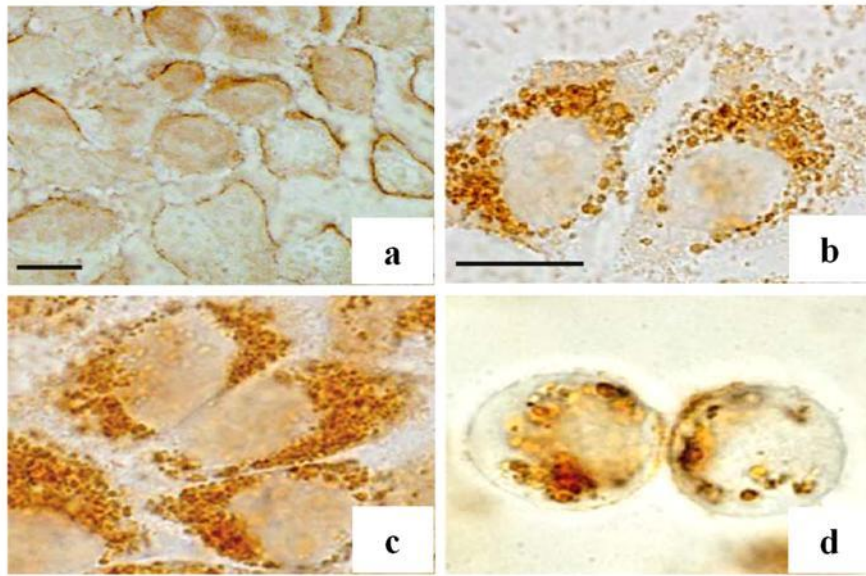
Possible mechanisms by which nanomaterials interact with biological tissue.



Material composition, electronic structure, bonded surface species (e.g., metal-containing), surface coatings (active or passive), and solubility, including the contribution of surface species and coatings and interactions with other environmental factors (e.g., UV activation).

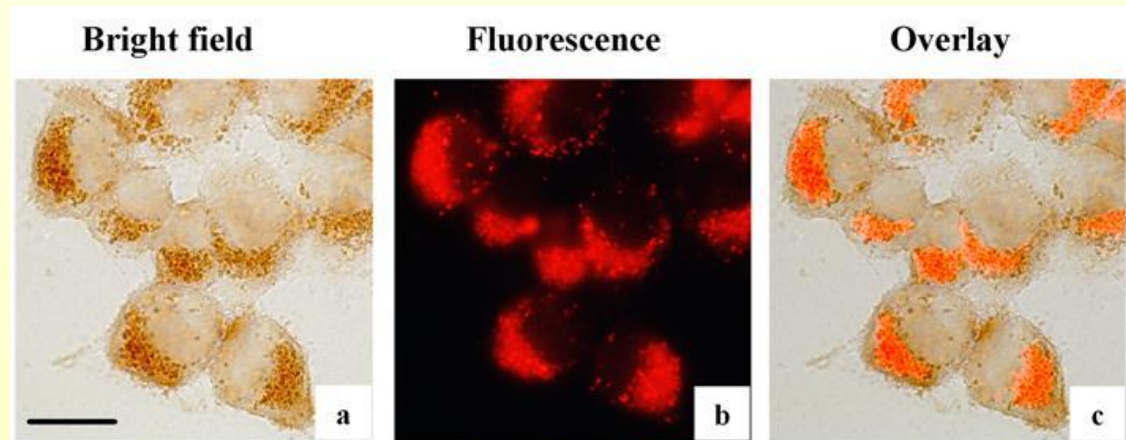
Interaction with cells

Internalization



In endocytic compartments

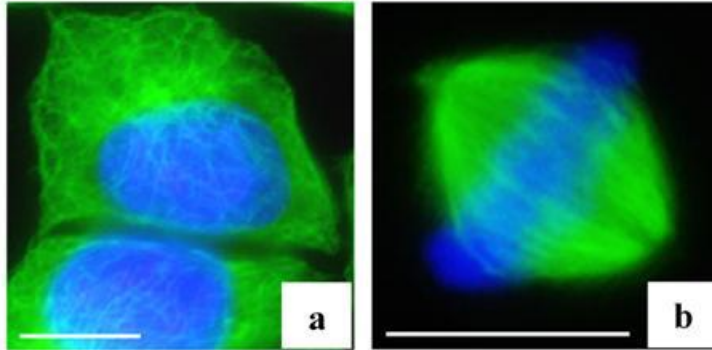
Lyso tracker red



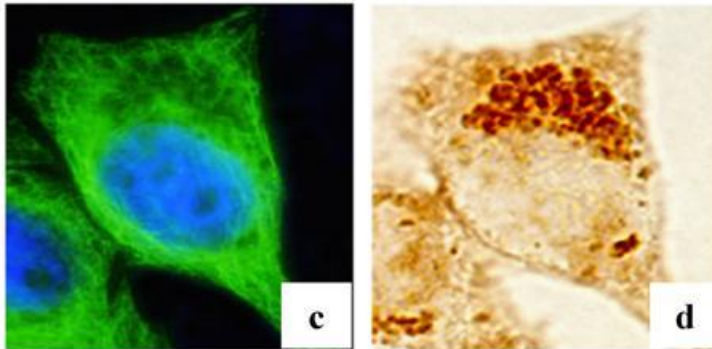
Cytotoxicity

Depending on the coating

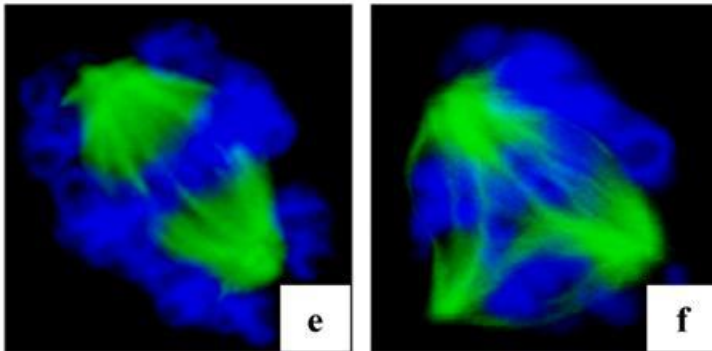
Microtubules (green)
DNA (blue)



CONTROL



DMSA (-) , APS (+)

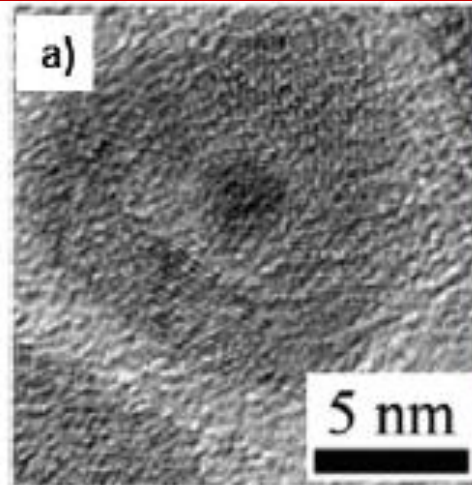


HEPARINE

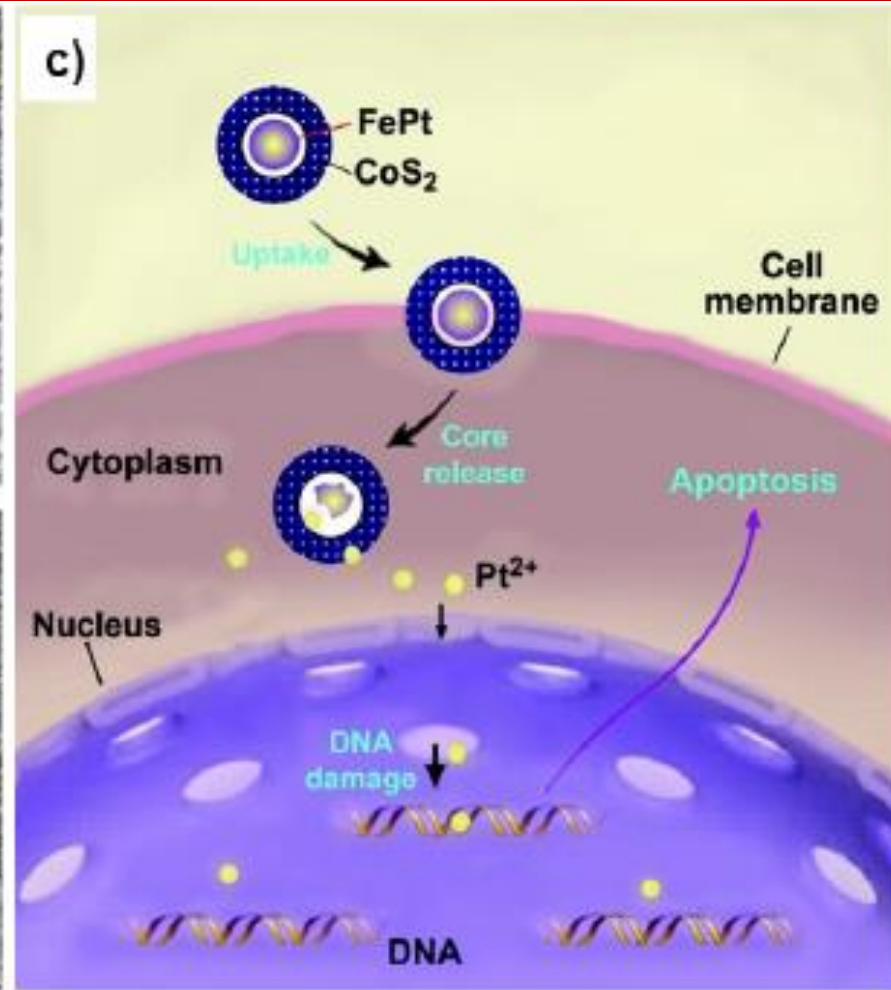
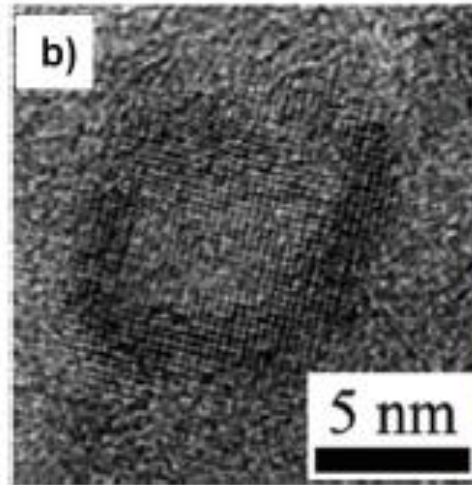
Stained with α -tubulin

Interaction with cells

FePt@CoS₂ yolk–shell
nanocrystals dispersed in
deionized water



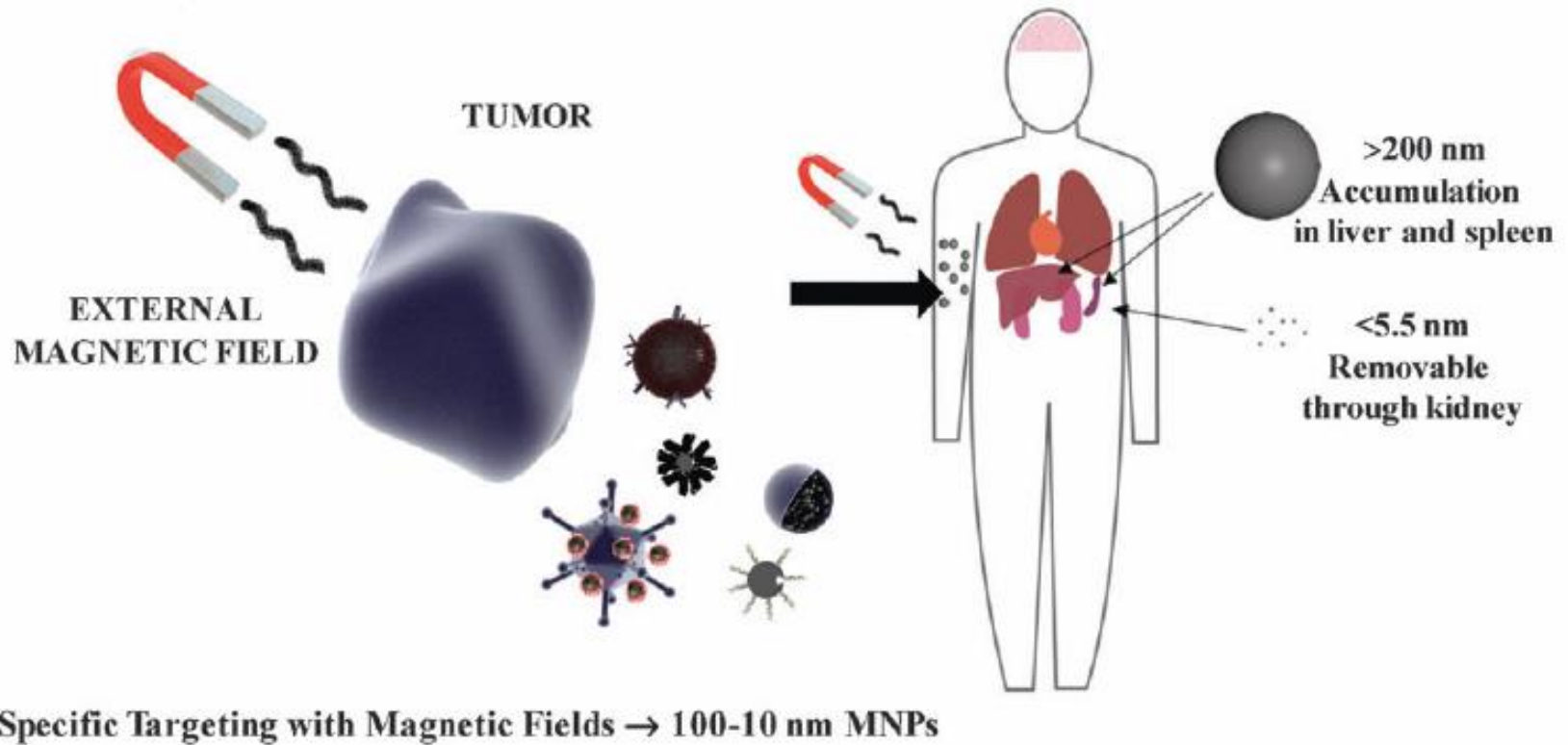
Hollow CoS₂ nanocrystals
without FePt cores are
dispersed in the mitochondria
after cell uptake.



After cellular uptake, FePt nanoparticles are oxidized to give Fe³⁺ and Pt²⁺ ions (yellow).
The Pt²⁺ ions enter the nucleus and mitochondria, bind to DNA and lead to apoptosis.

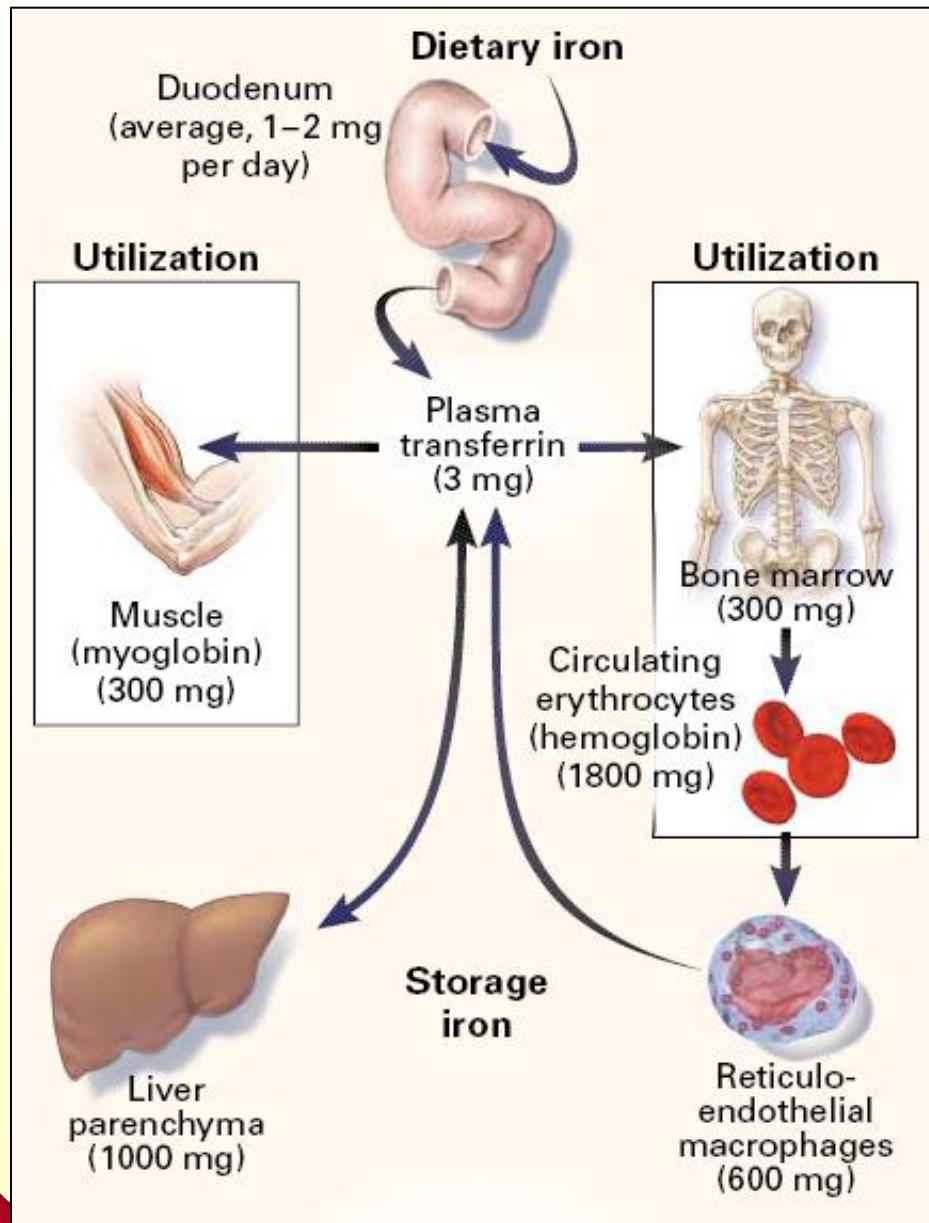
Gao J, Liang G, Zhang B, Kuang Y, Zhang X and Xu B 2007 . J. Am. Chem. Soc. 129 1428–33

Problem: Biodistribution



A SYSTEM FOR CONTROLLED
LOCAL DRUG RELEASE IN
CANCER THERAPY

Problem: Biodistribution



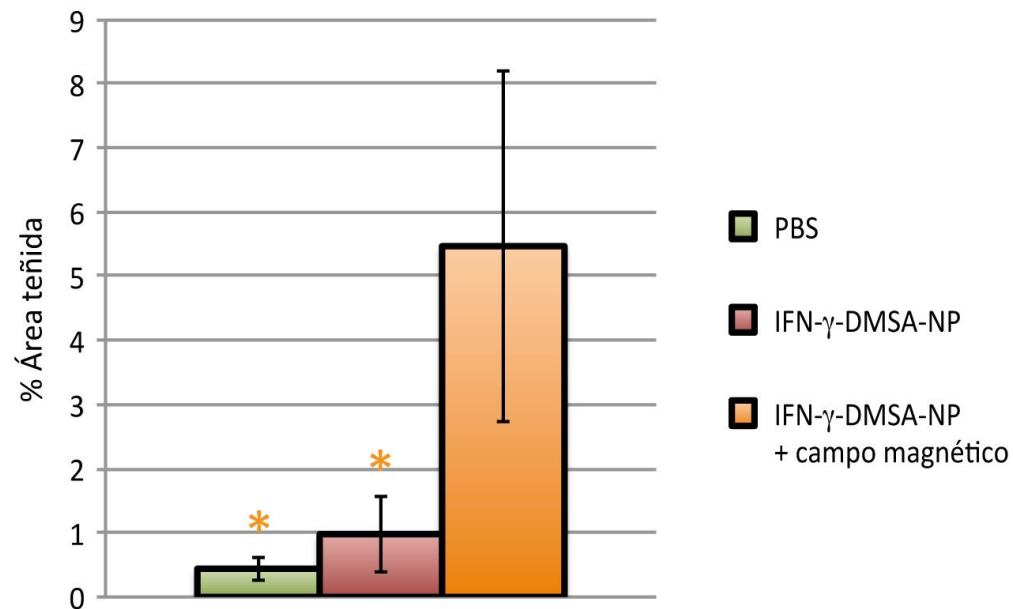
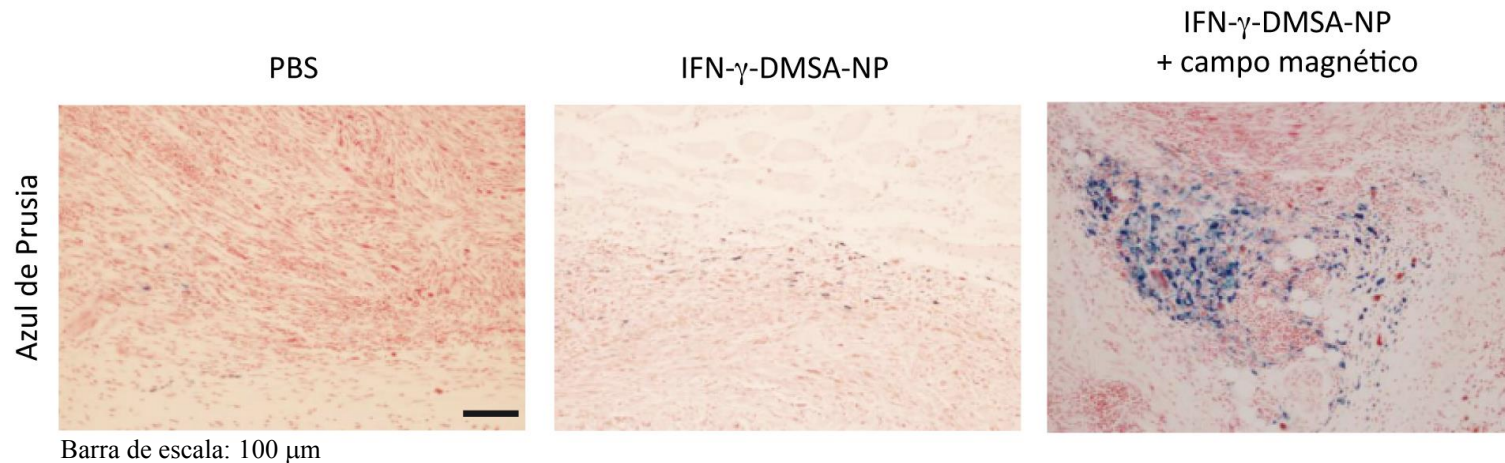
100 mg Fe => Endorem
(1-5 mg/Kg)

Distribution of Iron in Adults

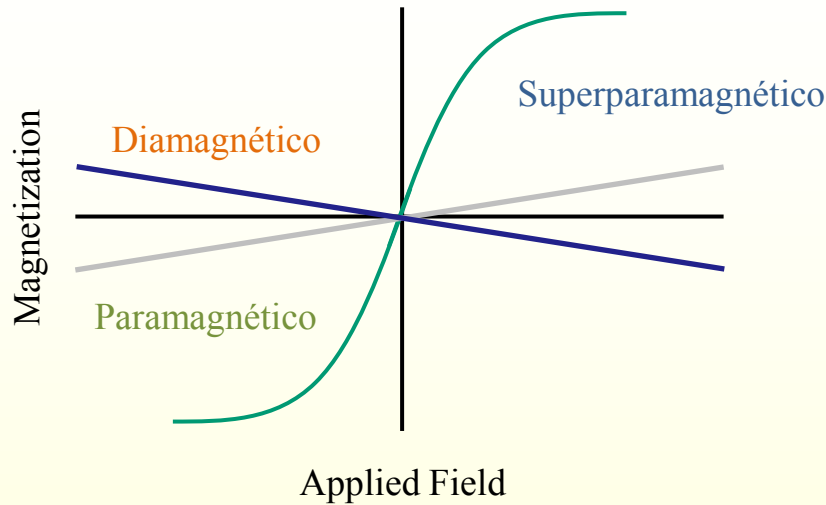
NANCY C. ANDREWS

The New England Journal of Medicine
Volume 341 Number 26, 1986, 1999

NP in the tissue Prussian blue



Magnetization curves

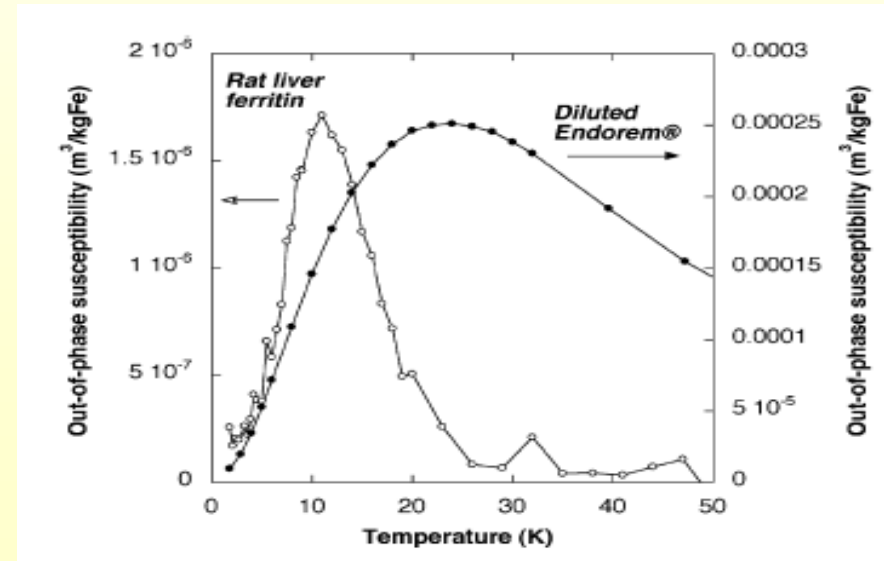
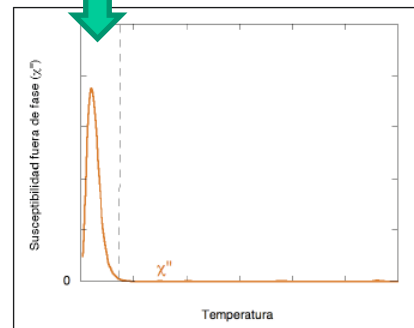
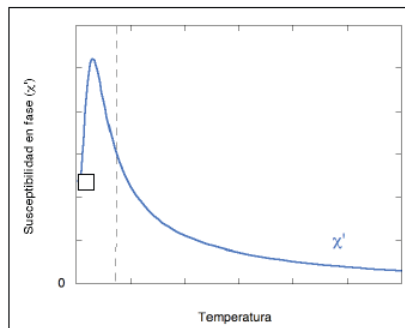


Magnetic methods

- NP
- Ferritin, hemoglobine
- Tissues...

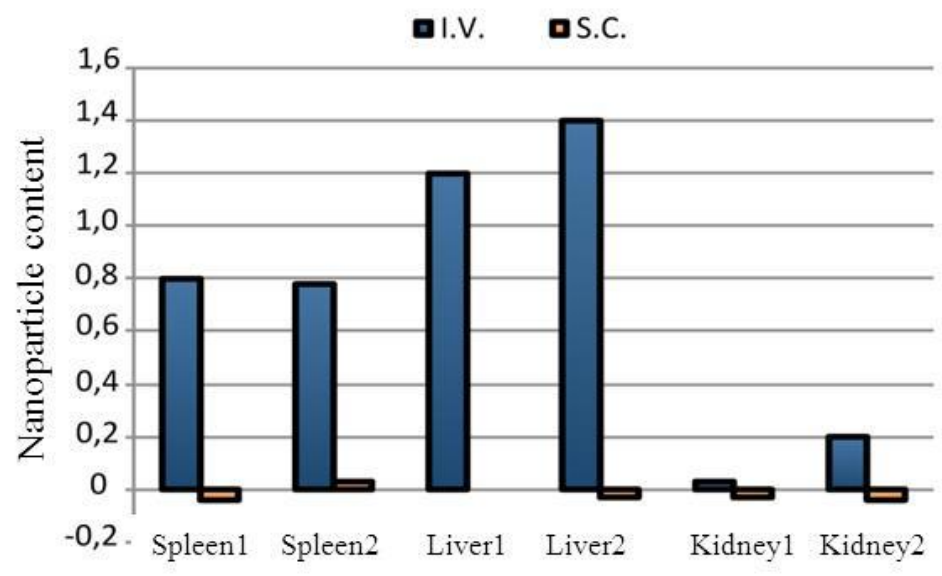
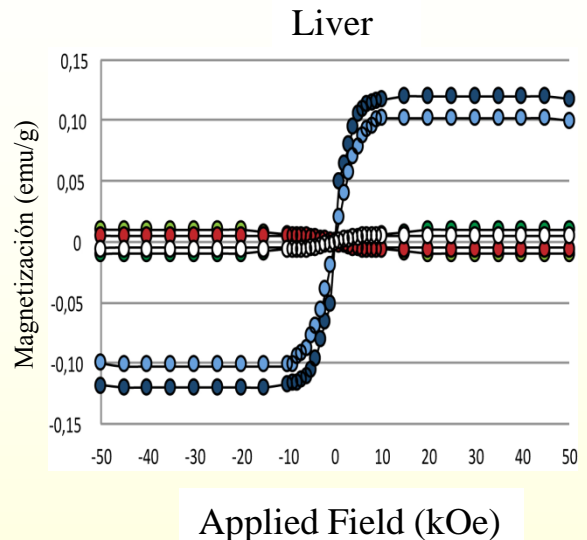
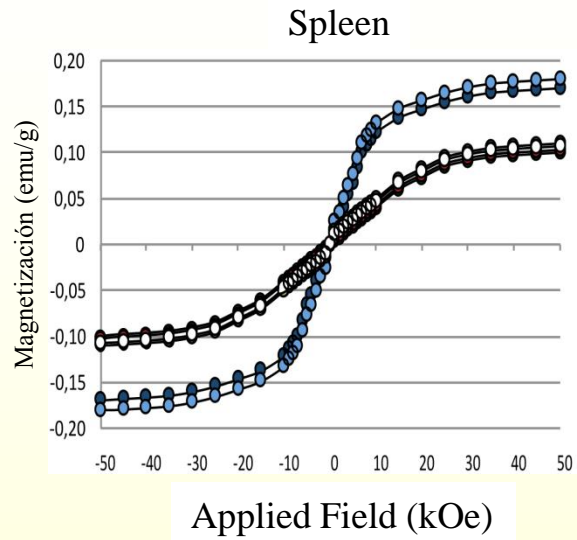
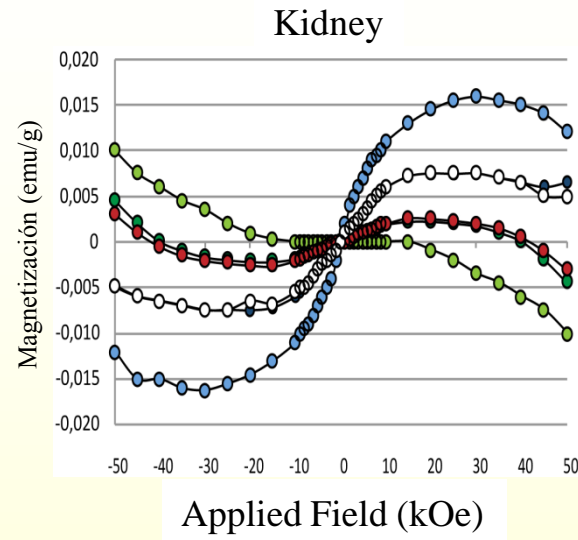
AC Susceptibility

NP



Detection, identification and quantification of NP in biosystems

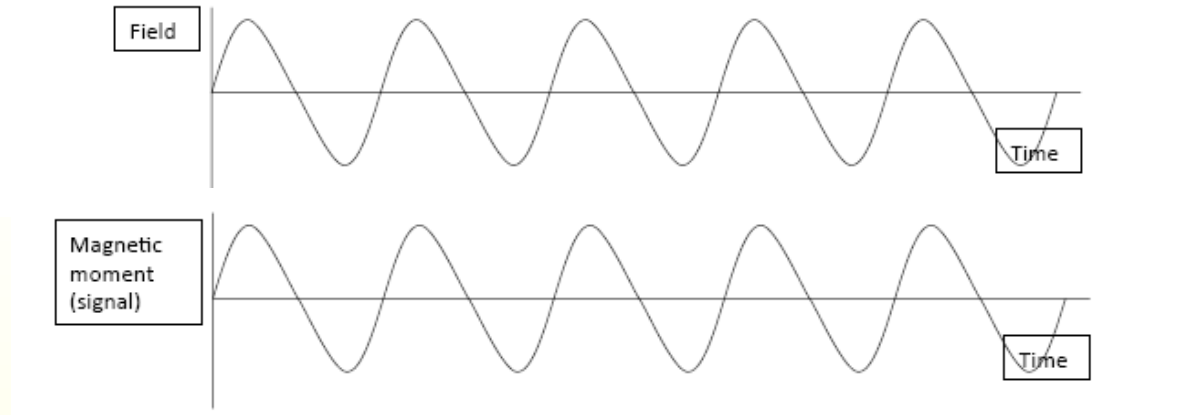
● I.V.1 ● I.V.2 ● S.C.1 ● S.C.2 ● Control 1 ● Control 2



Liver and brain imaging through dimercaptosuccinic acid-coated iron oxide nanoparticles
 Nanomedicine 5(3), 397- 408, 2010

Detection, identification and quantification of NP in biosystems

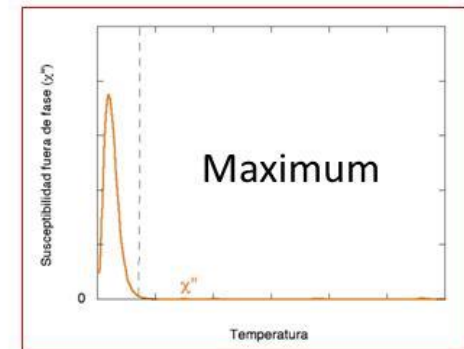
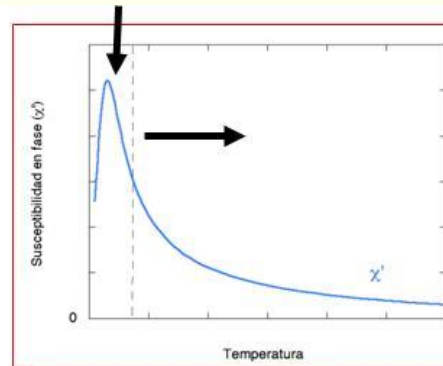
AC Magnetic Susceptibility



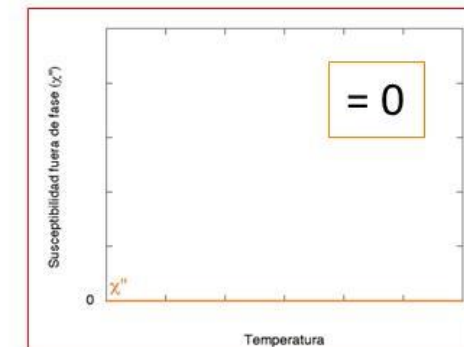
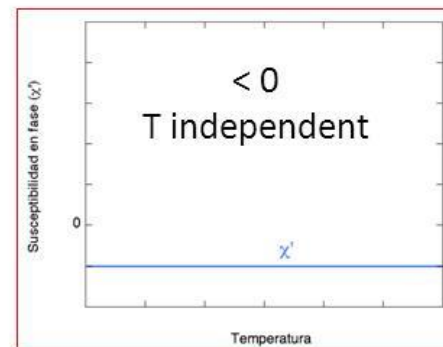
In-phase susceptibility (χ')

Out-of-phase susceptibility (χ'')

Nanometric particles
High Temperature: Curie Law
Low Temperature: Relaxation



Diamagnetic contribution

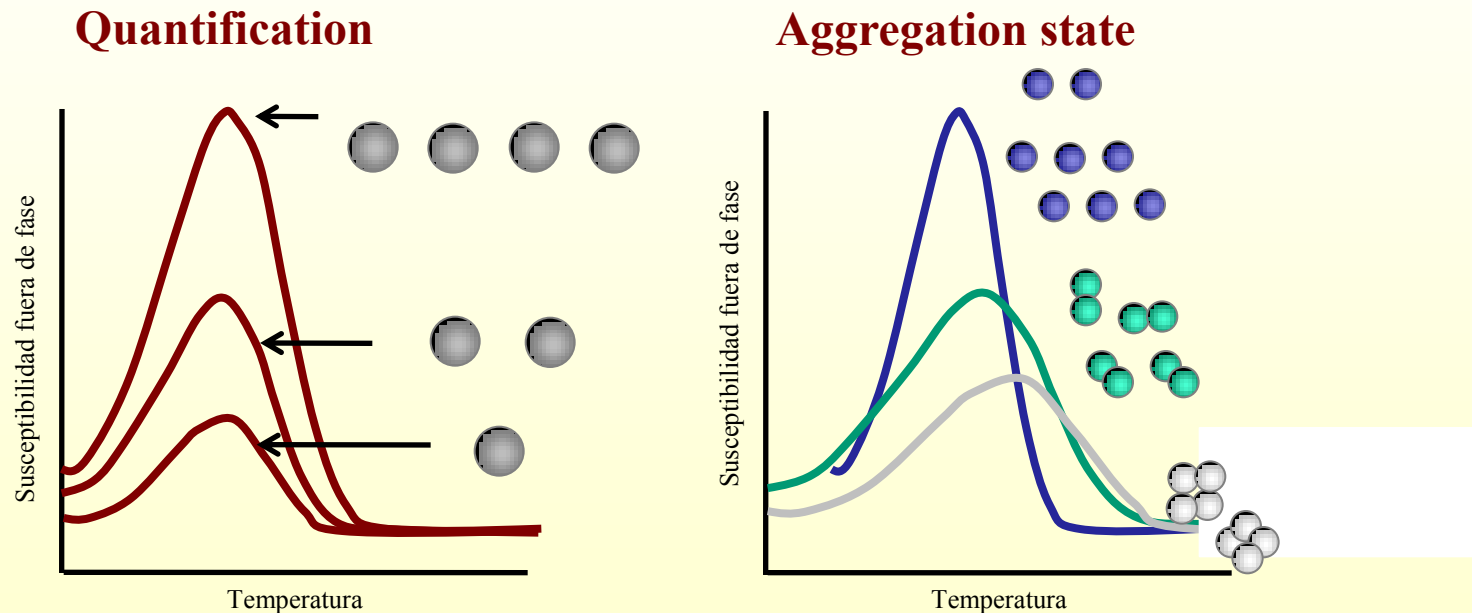


Detection, identification and quantification of NP in biosystems

AC Magnetic Susceptibility

Out-of-phase susceptibility (χ'')

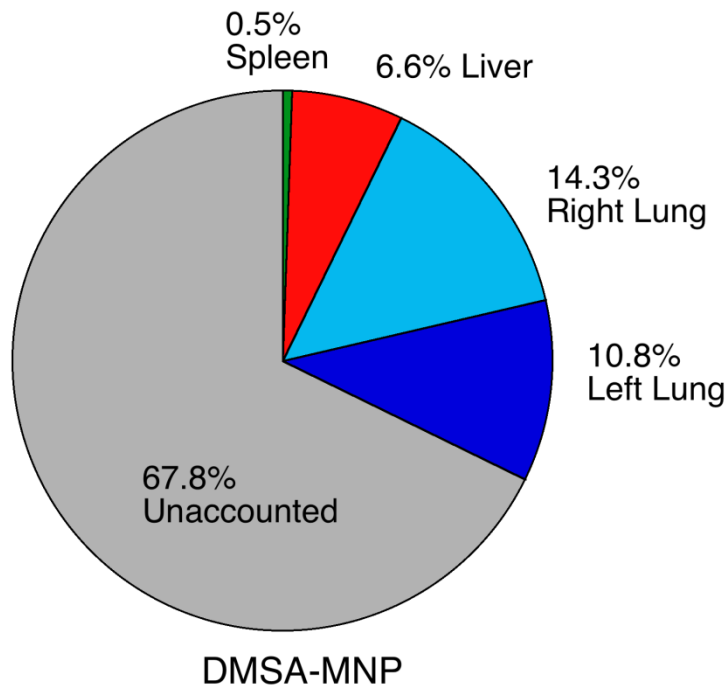
Size, Crystallinity, Aggregation



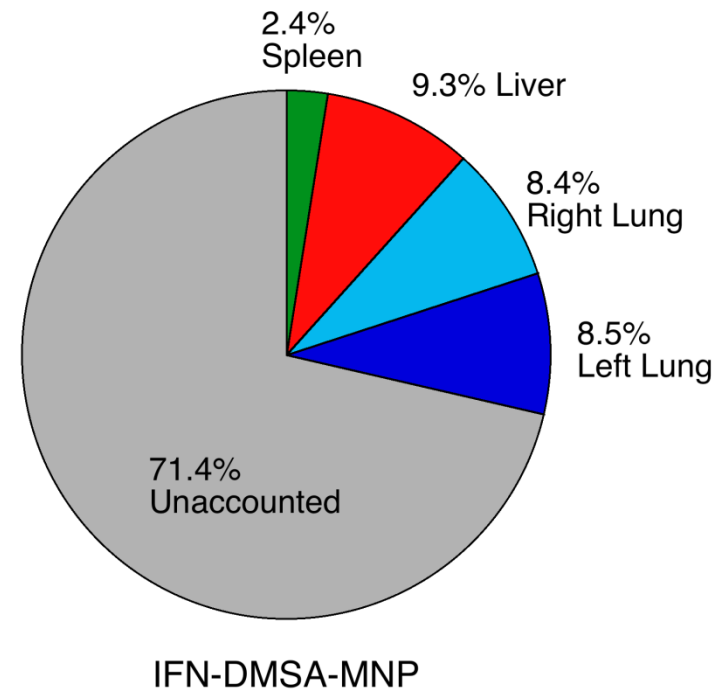
With the appropriated standards it is possible to calculate the amount of the total iron that is in the form of the magnetic nanoparticles.

Detection, identification and quantification of NP in biosystems

a)

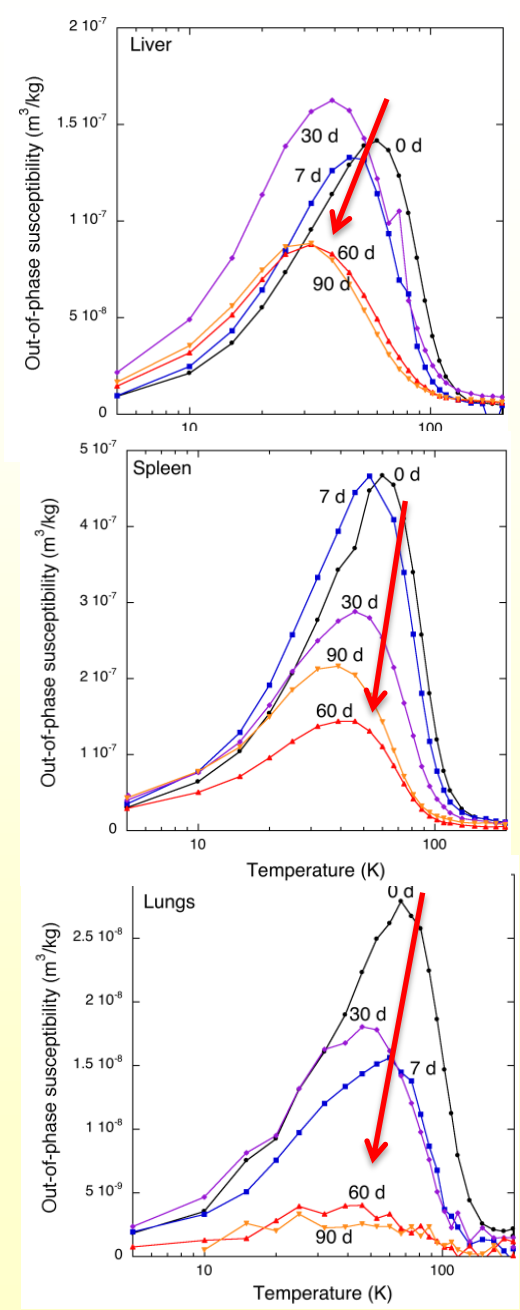
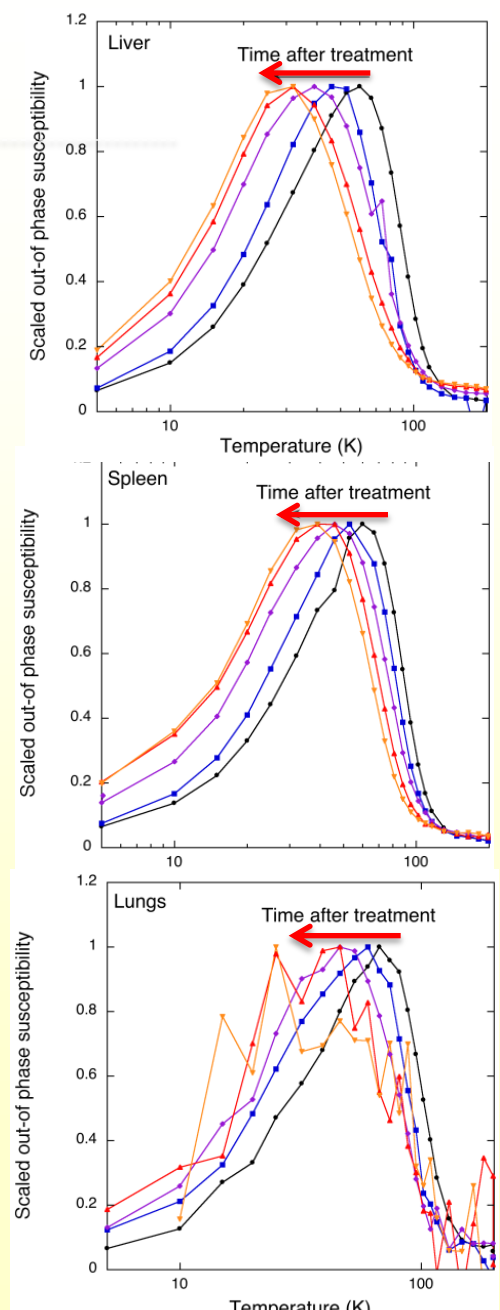
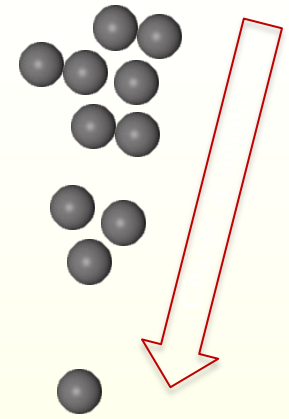
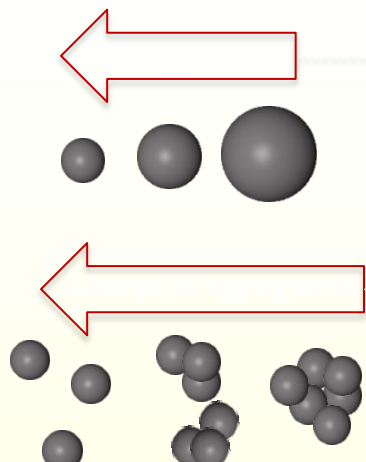


b)

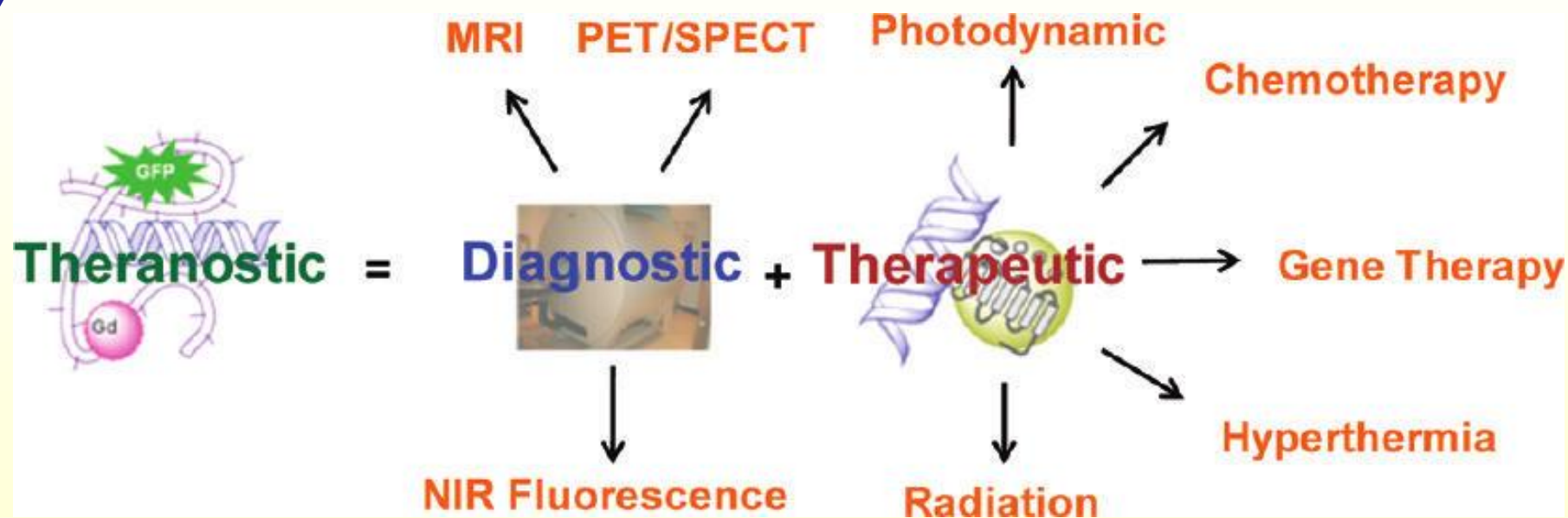


Percentage of the magnetic nanoparticles from the last MNP administration found in each organ. Values have been calculated from the total amount of iron found in each whole tissue in the form of MNP and the total amount of injected iron in the last administration.

Long term particle transformations

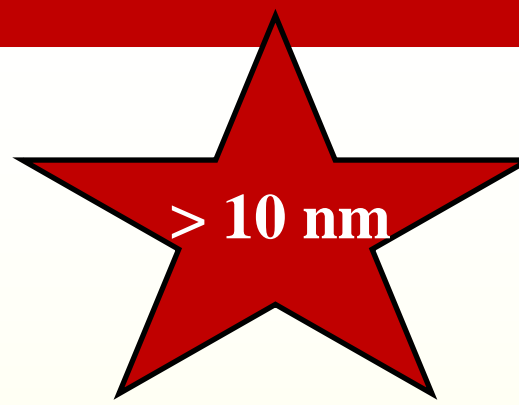


Ideal

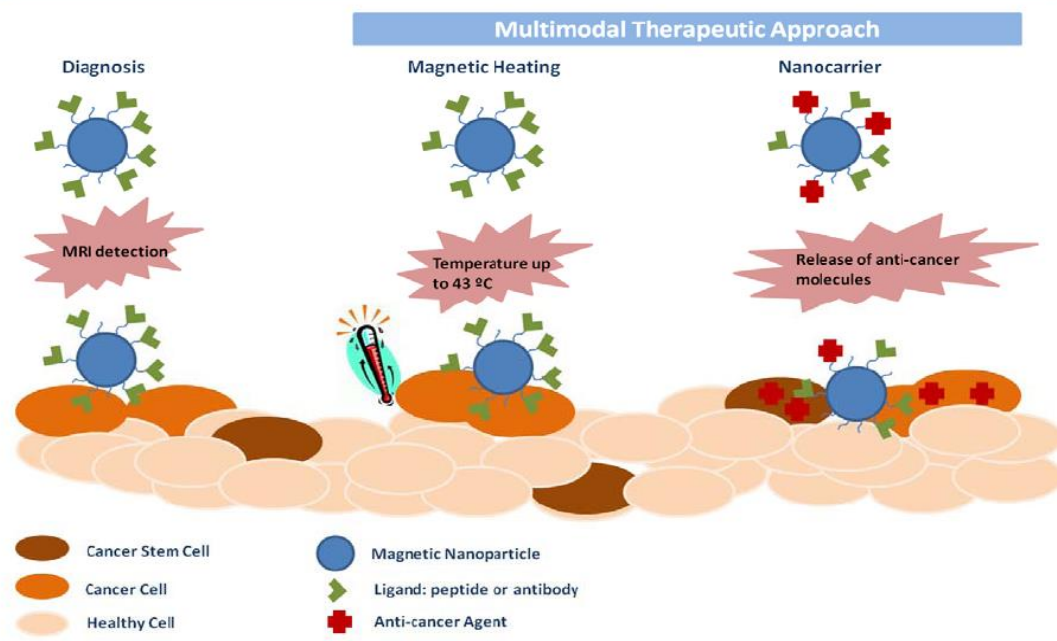


Bioconjugate Chem. 2011, 22, 1879–1903

FP VII/ MULTIFUN: Multifunctional nanotechnology for selective detection and treatment of cancer



THERAGNOSIS: MRI detection + Multimodal Therapeutic Approach



Pancreatic Cancer

Cancer Cells

Targeting markers & ligands →
 EGFR & LARLLT peptide
 Nucleolin/Nucleophosmin & NUCANT

Therapeutic Modalities:
 Magnetic heating
 NUCANT
 SiRNA (Bcl-2)
 Gemcitabine or PM001183

Breast Cancer

Cancer Cells

Targeting markers & ligands: →
 Her-2 & MARAKE peptide
 Nucleolin/Nucleophosmin & NUCANT

Therapeutic Modalities:
 Magnetic heating
 NUCANT
 SiRNA (Bcl-2)
 Fluorouracile or PM001183

Cancer Stem Cells

Targeting markers & ligands →
 CD44 & antibody
 Search high select. Markers

Therapeutic Modalities :
 Magnetic heating
 NUCANT
 miRNA-145 mimic
 Gemcitabine or PM001183

Cancer Stem Cells

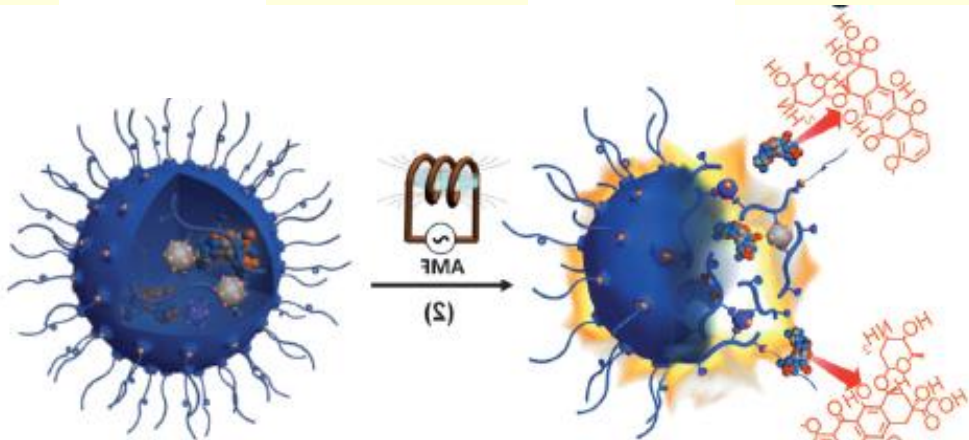
Targeting markers & ligands →
 CD44 & antibody
 Search high select. Markers

Therapeutic Modalities:
 Magnetic heating
 NUCANT
 miRNA-145 mimic
 Fluorouracile or PM001183

MAIN THEMES TACKLED IN MULTIFUN

- **Large scale production** of biocompatible iron oxide nanoparticles with optimal magnetic features.
- Functionalization of nanoparticle for **selective targeting** and for carrying different anticancer agents (i.e. drugs, sRNA, peptides)
- Implementation of **multimodal nanoparticle-based therapeutic** approach by combining heating capabilities and anticancer agents.
- **Toxicity and biodistribution** of nanoparticles in animal models (mice and pigs).
- Development of new **equipments for heat treatment and the detection-quantification** of nanoparticles in tissues, blood and urine.

Combine hyperthermia and drug delivery

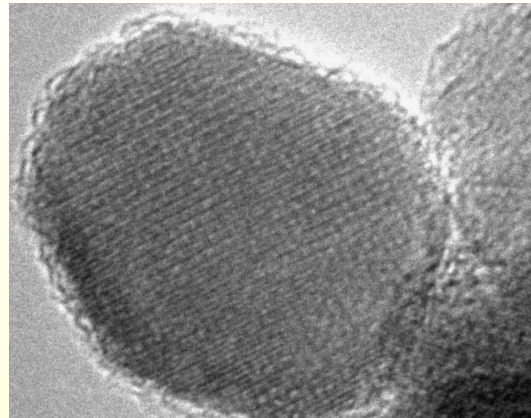
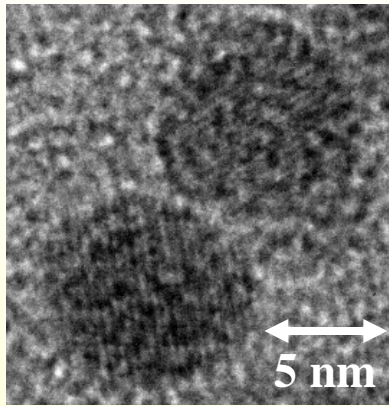


J. Cheon *Ang. Chem.* 2013

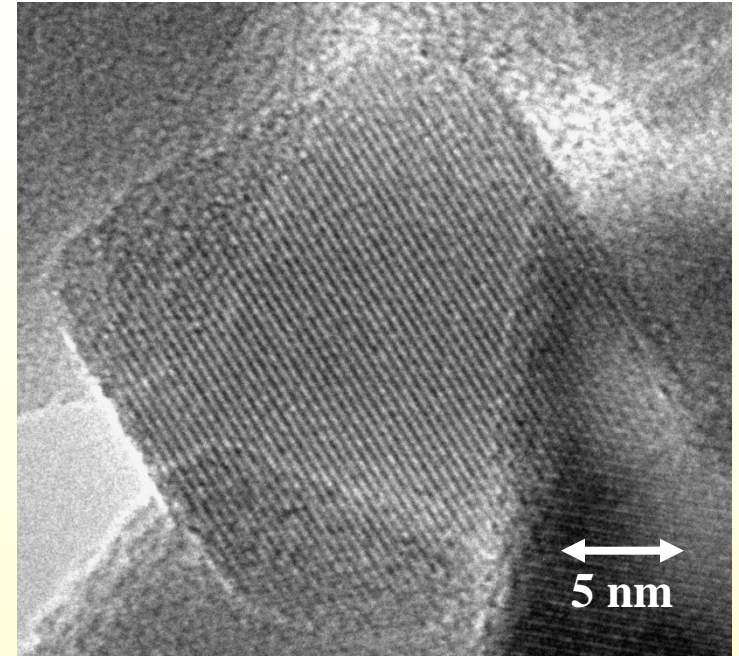


NANOPARTICLES AND NANOCRYSTALS OF IRON OXIDE

NANOPARTICLES



NANOCRYSTALS

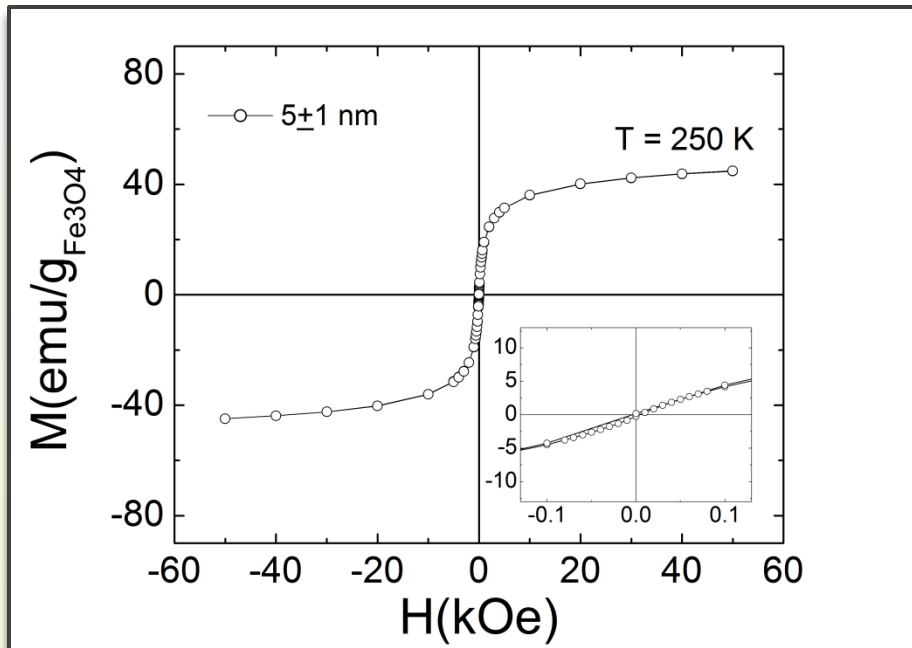


High surface energy
Round shapes

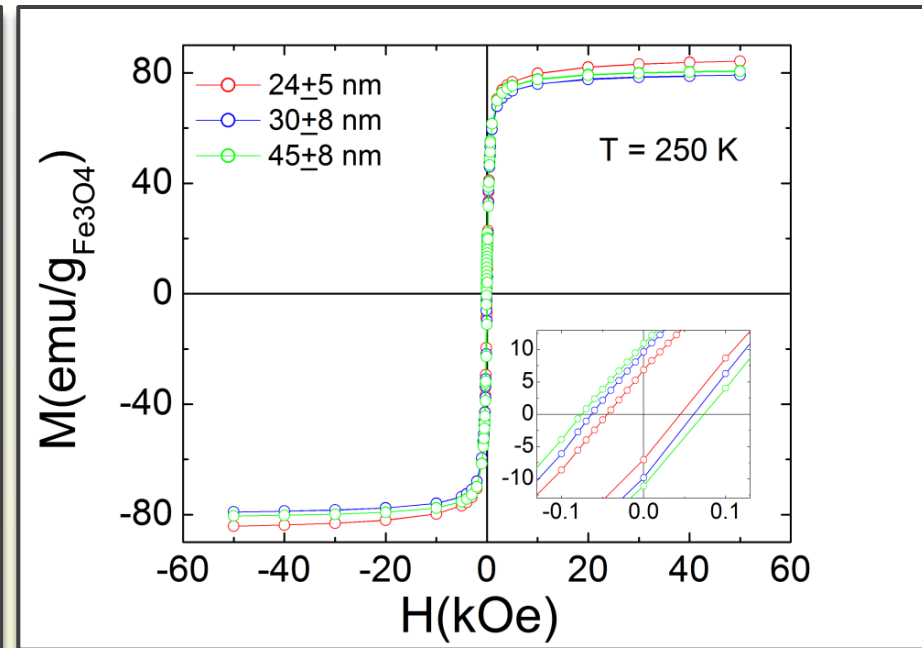
**MORE
ORDERED**

Lower surface energy
Less rounded shapes

NANOPARTICLES AND NANOCRYSTALS OF IRON OXIDE



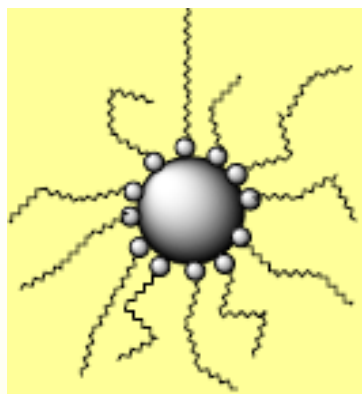
Nanoparticles



Nanocrystals

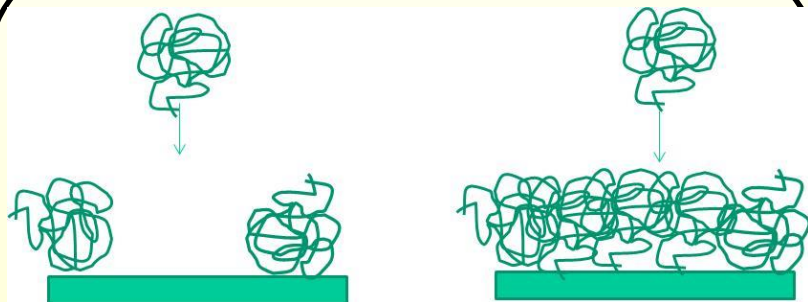
BETTER MAGNETIC RESPONSE
Maximum Heating efficiency and NMR contrast

LONG CIRCULATING AGENTS = POLYMERS = PEG

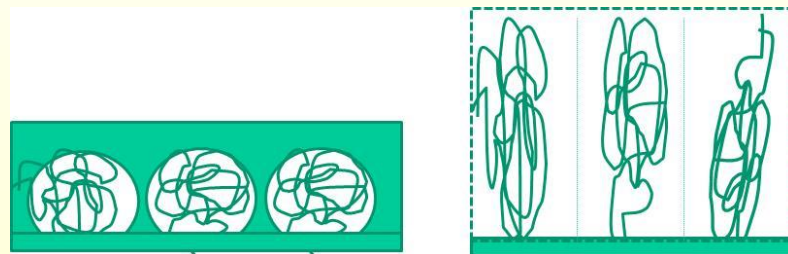


PROBLEMS

Polymerizability
End-group reactivity
Aggregation/Stability



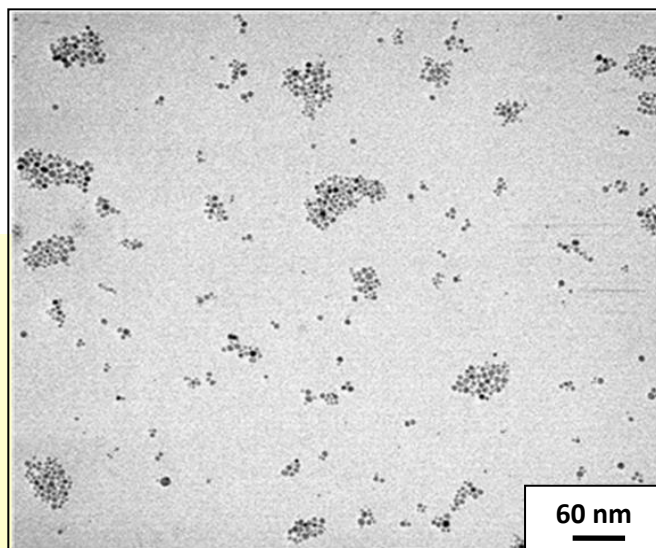
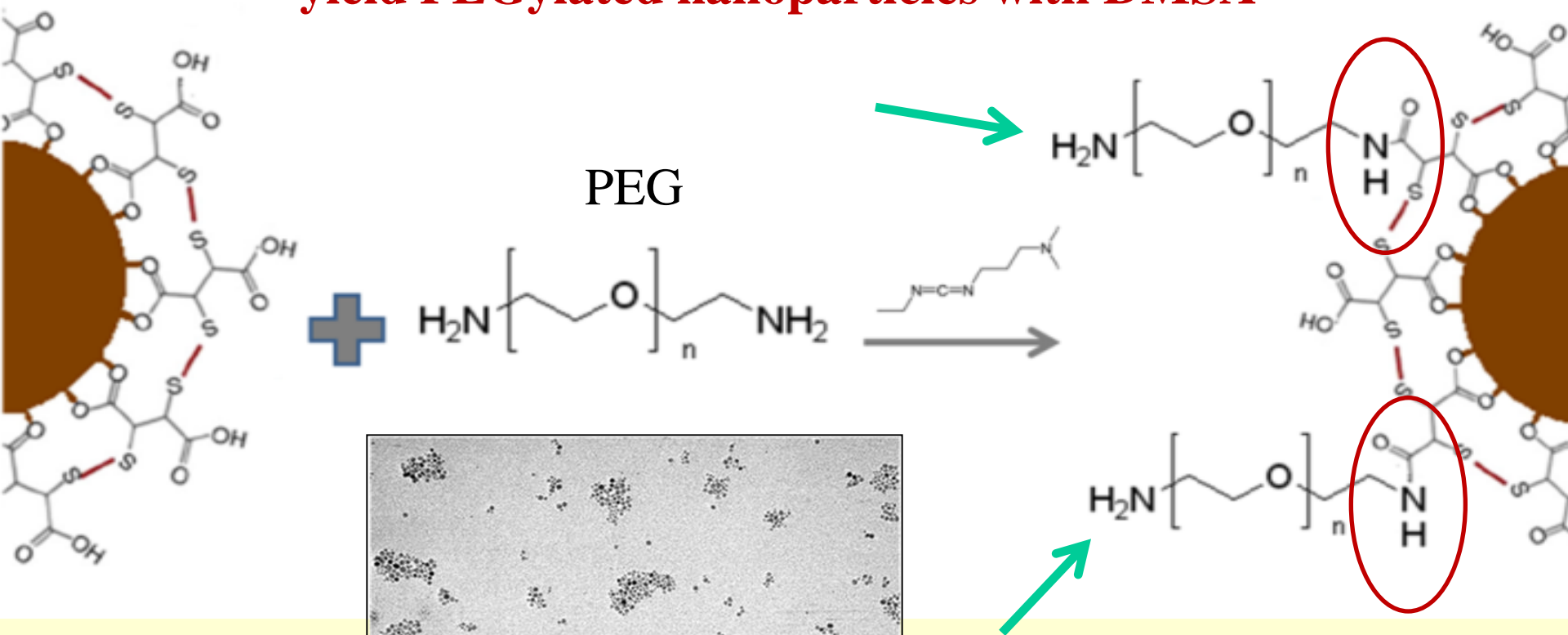
Grafting Density
(in the case of NPs
depend on geometry)



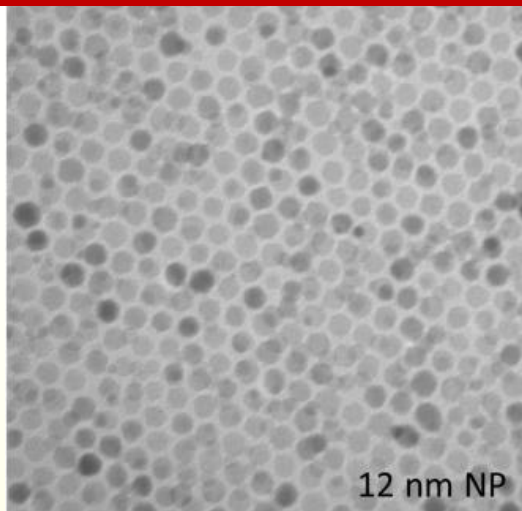
**Conformations of
surface-attached polymers**

LONG CIRCULATING AGENTS = POLYMERS = PEG

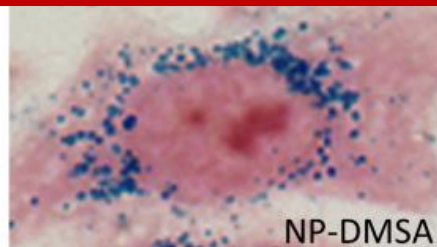
The different amine functionalized PEGs were attached to NP(Fe)-DMSA via EDC-mediated coupling reaction to yield PEGylated nanoparticles with DMSA



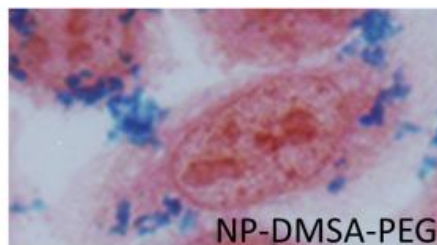
LONG CIRCULATING AGENTS



12 nm NP



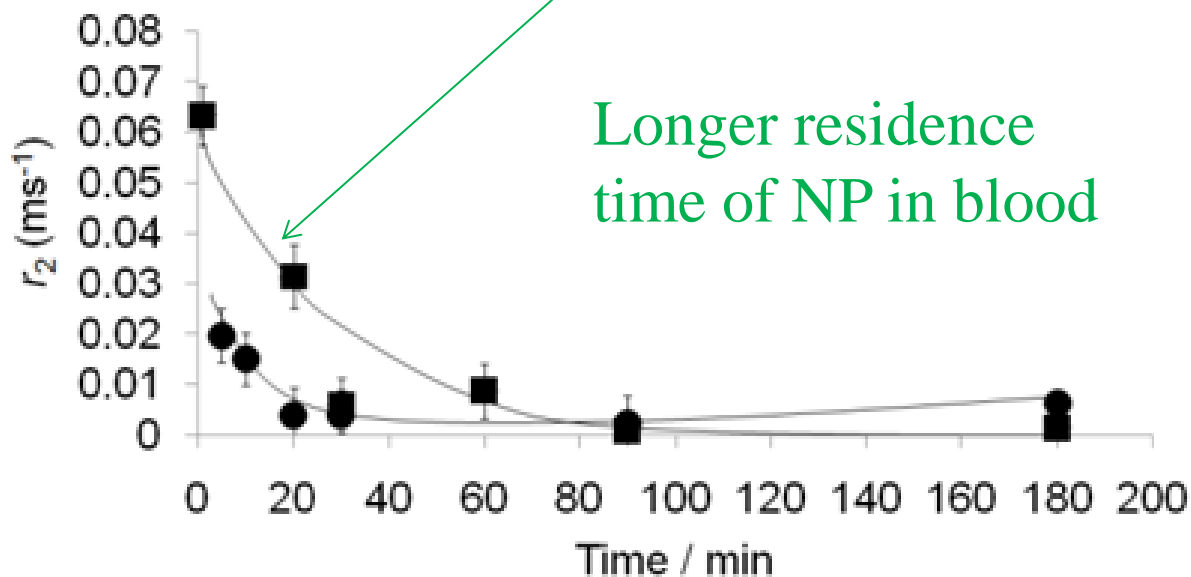
NP-DMSA



NP-DMSA-PEG

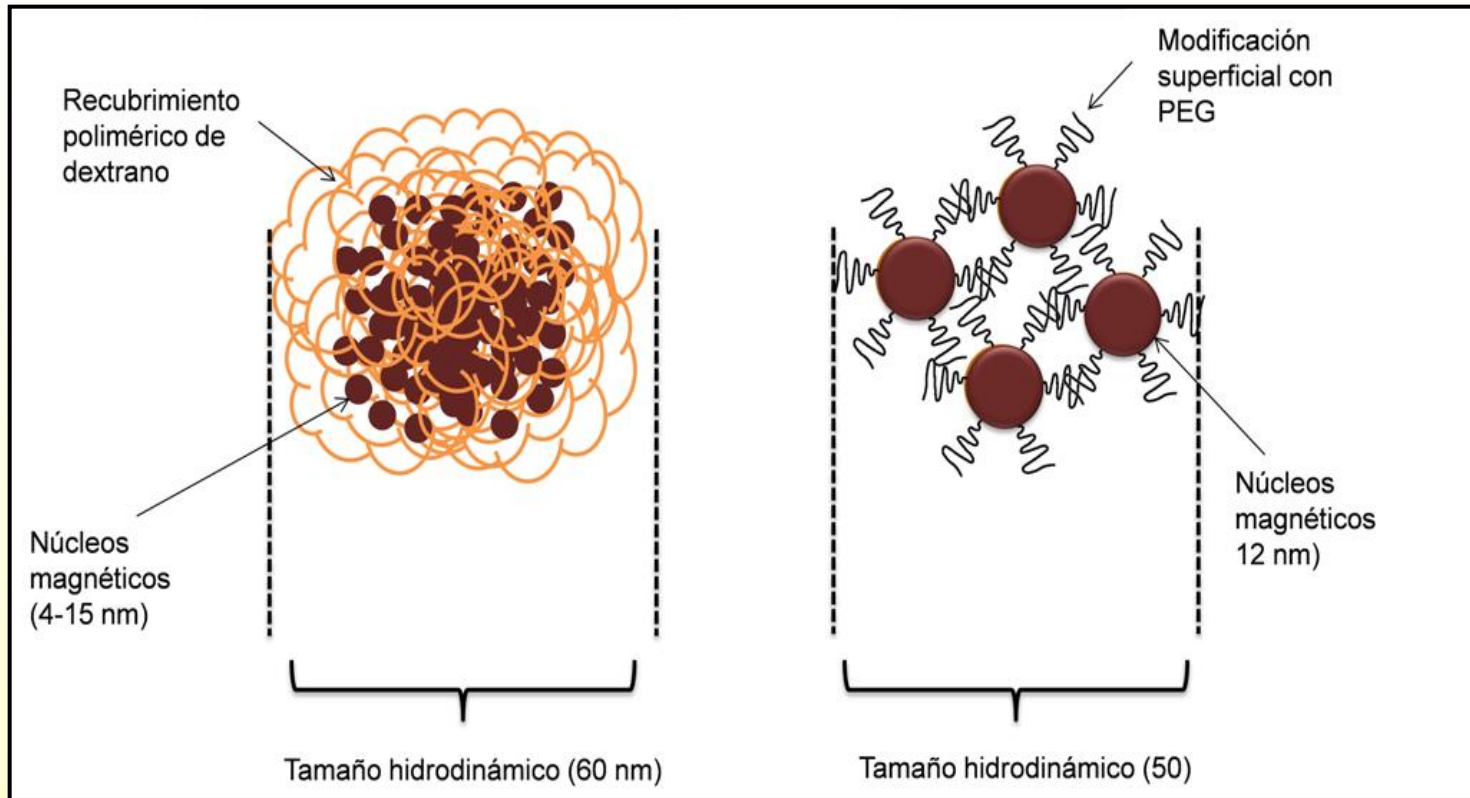
No cell uptake

NP-DMSA-PEG-(NH₂)₂



NanoMag:

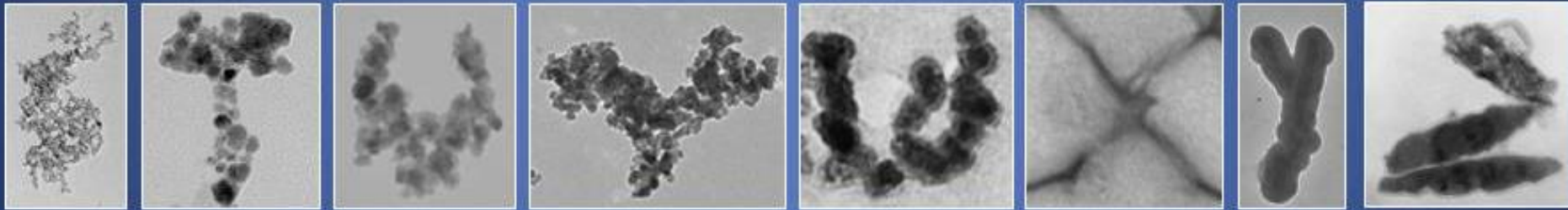
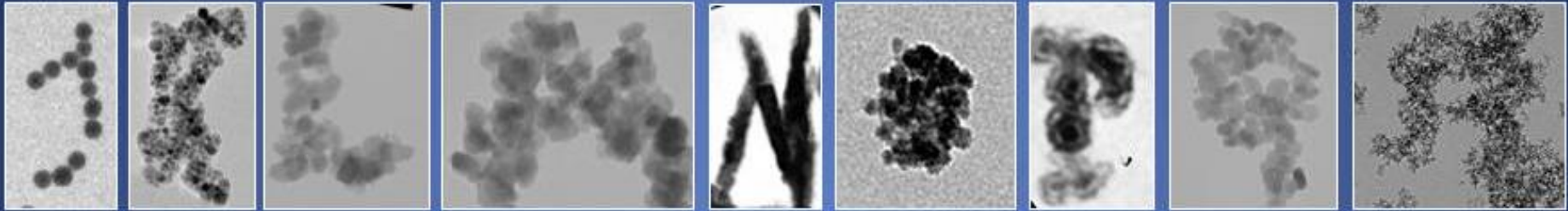
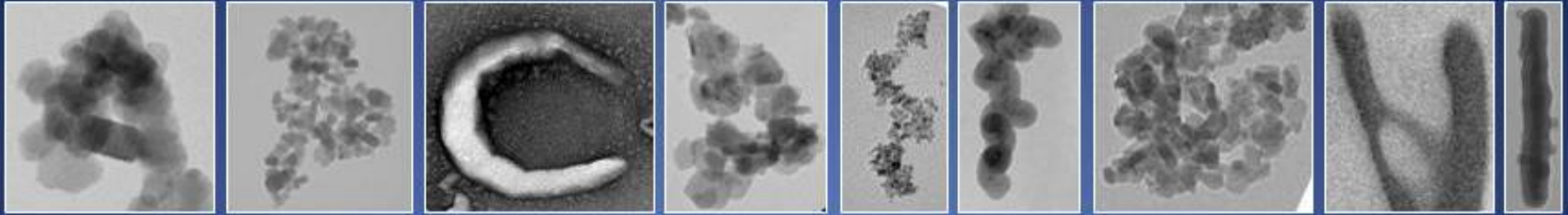
Nanometrology Standardization Methods for Magnetic Nanoparticles (Nov 2013-2017)



The NanoMag project is to improve and redefine existing analyzing methods and in some cases, to develop new analyzing methods for magnetic nanostructures.

CONCLUSIONS

- **Magnetic nanoparticles could help to improve clinical practice in the treatment of cancer**, most probably in synergy with other conventional treatments. Significant advances in the field have been made.
- There already exist methods to obtain magnetic nanoparticles with the appropriate properties, bearing in mind that these **properties must be optimized** to suit the magnetic field and application frequency that will be used.
- We have to developed not only magnetic nanoparticles with **good heating capacities**, but also with good colloidal properties, **long blood circulation time** and grafted ligands able to facilitate their specific internalization in tumor cells.
- More systemic and **long-term toxicological studies** are required before the translation of any nanoprobe to clinical adaptation.
- **Other applications of magnetic nanoparticles** are in gene therapy and cell labelling for tissue regeneration.



Gracias por vuestra atención

Pictures by: M. P. Morales¹, A. G. Roca², M. Ibrahim³, © L. Gutiérrez^{1,3}

¹Instituto de Ciencia de Materiales de Madrid ICMM-CSIC, Spain, ²The University of York, UK, ³The University of Western Australia, Australia, 2012